

Biologically Guided Radiation Therapy (BGRT)

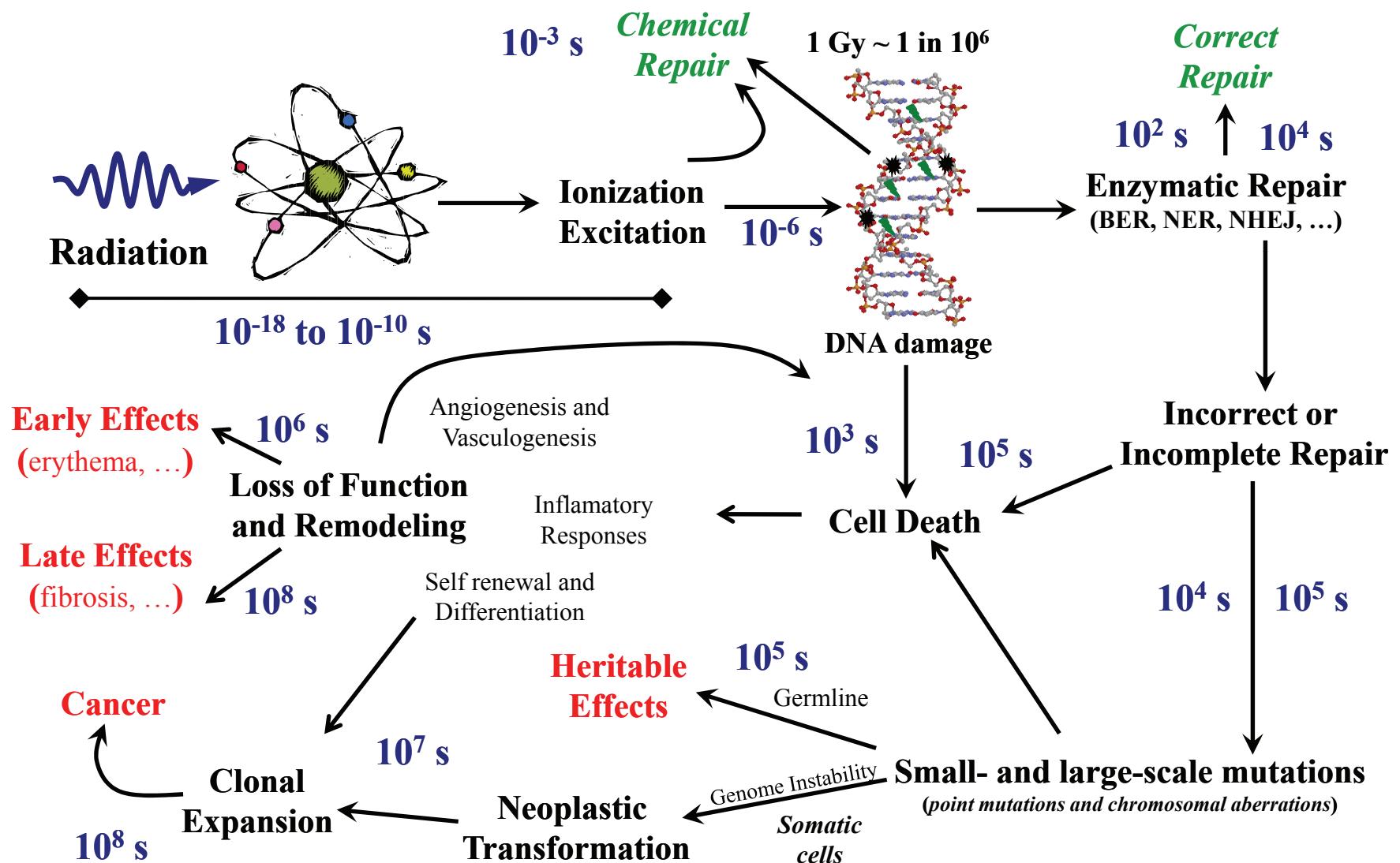
Effects Inter-Patient and Intra-Tumor Heterogeneity

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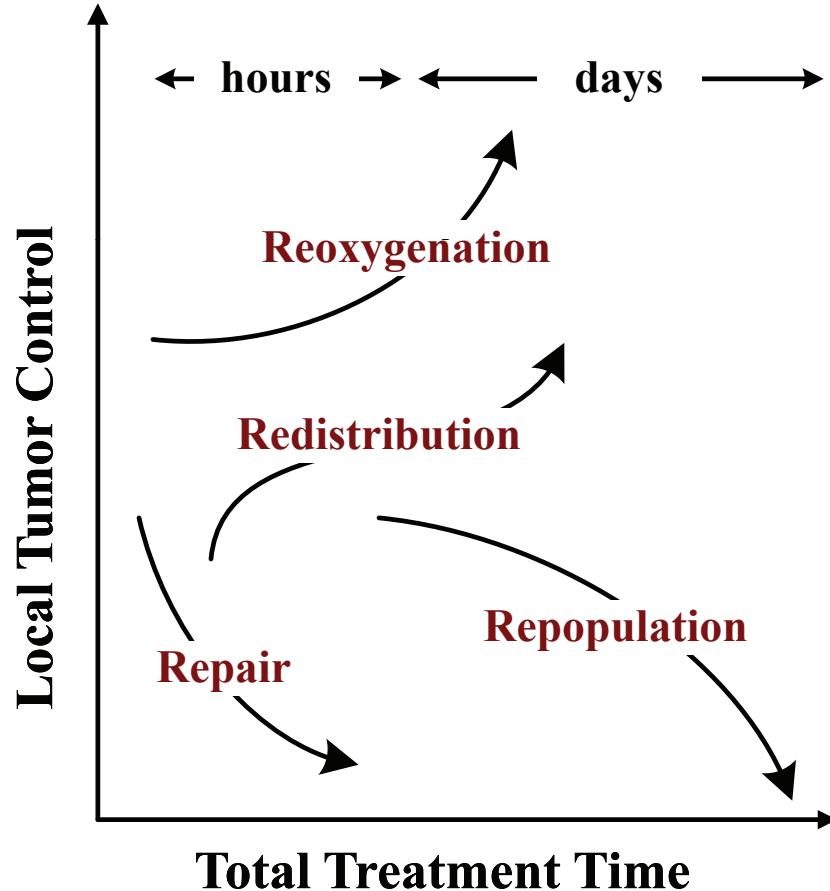
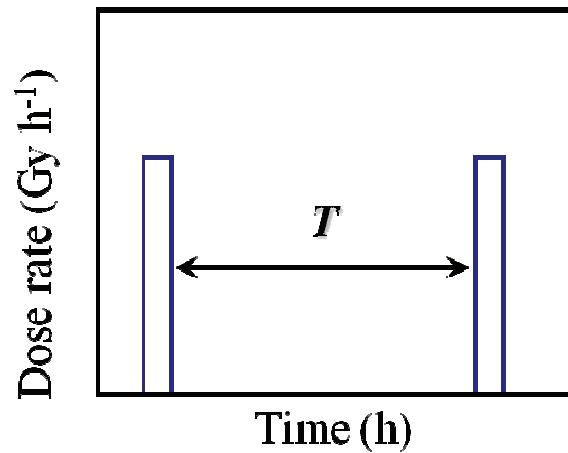
**University of Washington
Department of Radiation Oncology
Thursday April 22, 2010**

Physics → Chemistry → Biology → Clinic



Four R's of Radiobiology in RT

- Repair (\downarrow)
- Repopulation (\downarrow)
- Redistribution (\uparrow)
- Reoxygenation (\uparrow)



Outline

- **Local tumor control**
 - Models, methods and issues
 - Feasibility of predicting outcomes for individual patients
 - Feasibility of predicting outcomes for patient populations
- **Strategies to guide the design alternate and refined treatments**
 - Fractionated external beam radiation therapy (EBRT)
 - Brachytherapy

RD Stewart, JH Park, DJ Carlson, Isoeffect Calculations in Adaptive Radiation Therapy and Treatment Individualization, In *Adaptive Radiation Therapy*, X.A. Li, Editor. Taylor and Francis Group, *in press* (2010)

The LQ in Radiation Therapy

Inaccurate and too simplistic (*compared to known biology*)

$$S(D) = \exp(-\alpha D - \beta GD^2)$$

one-hit damage pairwise damage interaction Dose-rate and dose-fractionation effects (“dose protraction factor”)

Parameters (e.g., α and β) derived from analysis of clinical outcomes are uncertain and averaged over a heterogeneous patient population

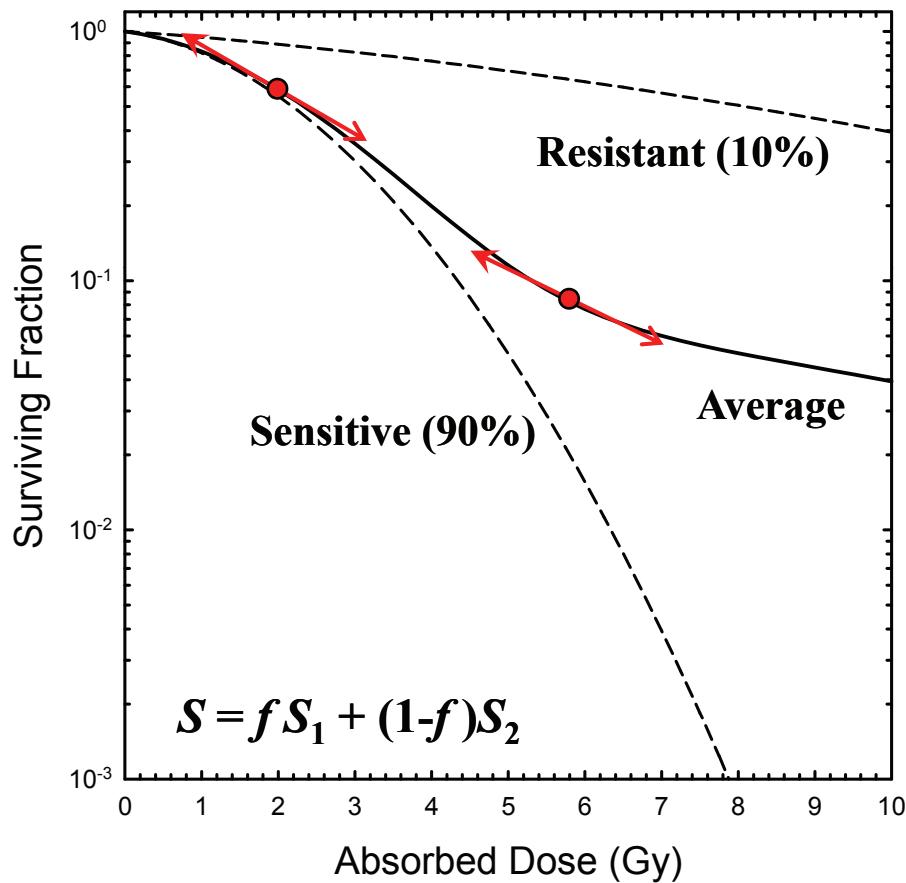
JF Fowler, R Chappell, M Ritter,
IJROBP **50**, 1021-1031 (2001)

$$\begin{aligned}\alpha &= 0.039 \text{ Gy}^{-1} \\ \alpha/\beta &= 1.49 \text{ Gy} \\ S &= 1.159 \times 10^{-3} (37 \times 2 \text{ Gy})\end{aligned}$$

JZ Wang, M Guerrero, XA Li,
IJROBP **55**, 194-203 (2003)

$$\begin{aligned}\alpha &= 0.15 \text{ Gy}^{-1} \quad (4X \text{ higher}) \\ \alpha/\beta &= 3.1 \text{ Gy} \quad (2X \text{ higher}) \\ S &= 2.677 \times 10^{-8} \quad (10^4 \text{ smaller})\end{aligned}$$

SF for a Heterogeneous Cell Population

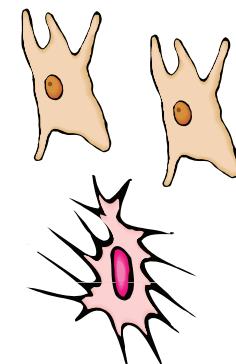


Can't use a single (*average*) set of LQ radiation sensitivity parameters (α , α/β) to predict overall shape of dose-response curve

$$S \neq \exp(-\alpha D - \beta GD^2)$$

Five Reasons (*many others possible*)

- Genomic Instability
- Repair
- Repopulation
- Reassortment
- Reoxygenation



But maybe we could extrapolate from a known point?

Poisson Tumor control probability (TCP)

Most widely used model assumes that the distribution of the number of tumor cells surviving a treatment is adequately described by a Poisson distribution

$$\text{TCP} = \exp\{-\rho VS(D)\}$$

Chance no tumor cells survive a treatment that delivers total dose D

ρ = number of tumor cells per unit volume ($< 10^9$ cells cm^{-3})

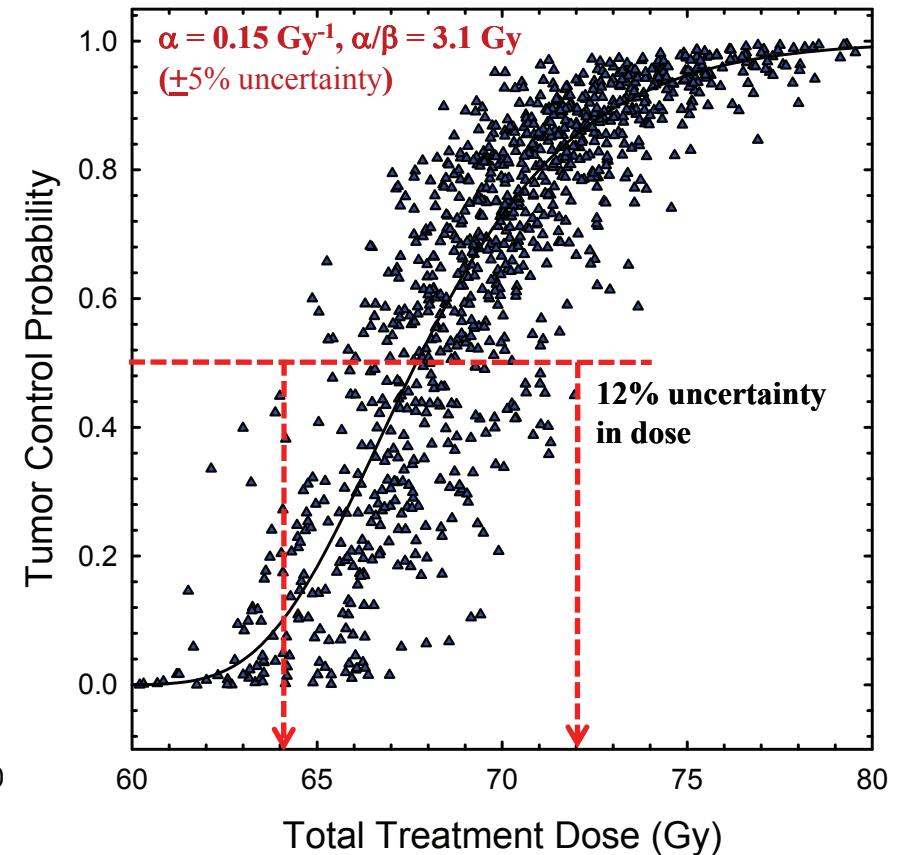
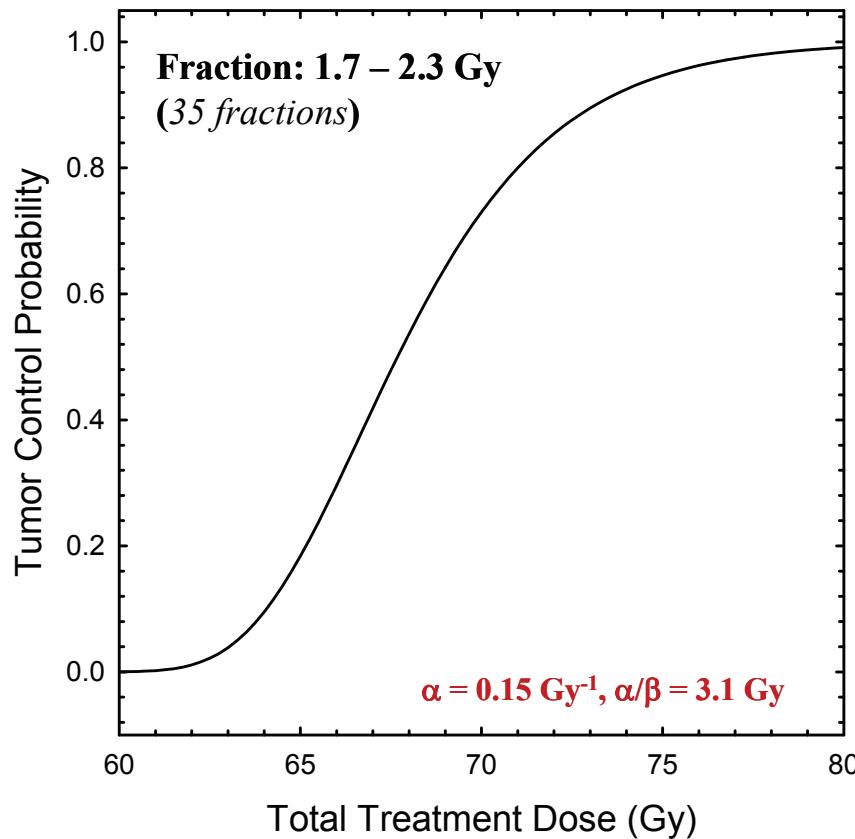
V = tumor volume (GTV? PTV?)

product ρV = pre-treatment number of tumor cells

Typical uncertainty? Factors as large as 10^3 to 10^6 !

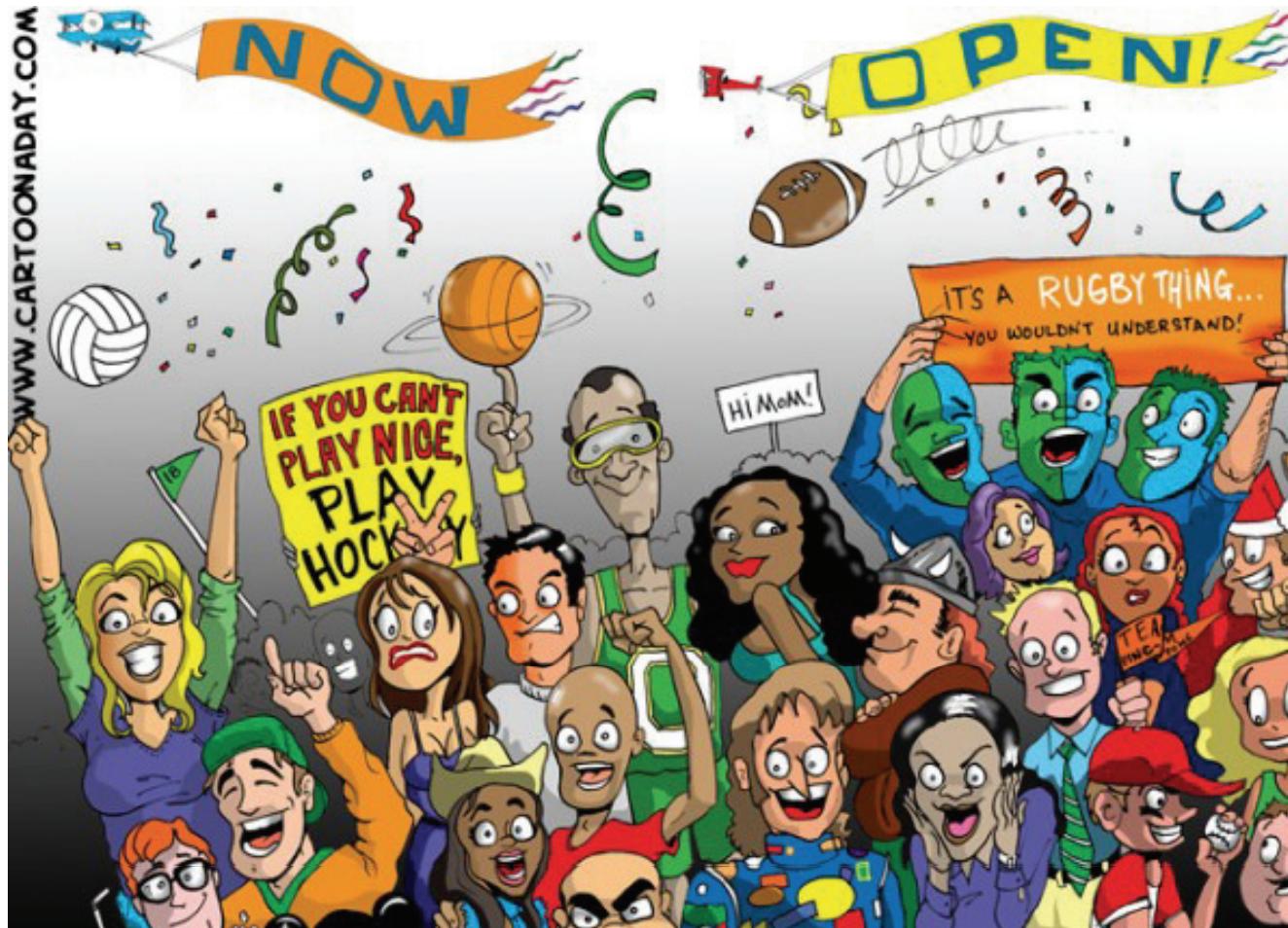
Eradication of some cells, such as cancer stem cells, may be far more important than the eradication of others (effective $\rho << 10^9$ cells cm^{-3} ?)

Prediction of Local Tumor Control



Accurate prediction of local tumor control for individual patients seems rather unlikely, no?

Outcomes for a Patient Population?



<http://www.cartoonaday.com/images/cartoons/2010/03/Crowd-of-Cartoon-Sports-FansA-598x429.jpg>

Equivalent Tumor Doses

What dose should be delivered to achieve the same level of biological damage as another treatment?

Reference Treatment Alternate Treatment

$$TCP(D_R) = TCP(D)$$

$$\exp(-\rho VS(D_R)) = \exp(-\rho VS(D)) \quad \text{Poisson TCP model}$$

$$\rho = \text{cell density } (\# \text{ cm}^{-3}) \quad V = \text{tumor volume } (\text{cm}^3)$$

When considering radiation effects in the *same patient*, ρ and V may be considered *treatment independent* constants.

$$S(D_R) = S(D) \quad \begin{array}{l} \text{Two biological parameters } (\rho \text{ and } V) \text{ eliminated from} \\ \text{modeling process } (\text{uncertainty in } \rho V \text{ doesn't matter!}) \end{array}$$

For individual patients, iso-TCP = iso-survival

Equivalent dose derived from the LQ

Reference Treatment = Alternate Treatment

$$S(D_R) = S(D)$$

$$\exp(-\alpha D_R - \beta G D_R^2) = \exp(-\alpha D - \beta G D^2)$$

α and β (or α/β) characterize
intrinsic radiation sensitivity

G is the *dose protraction factor*

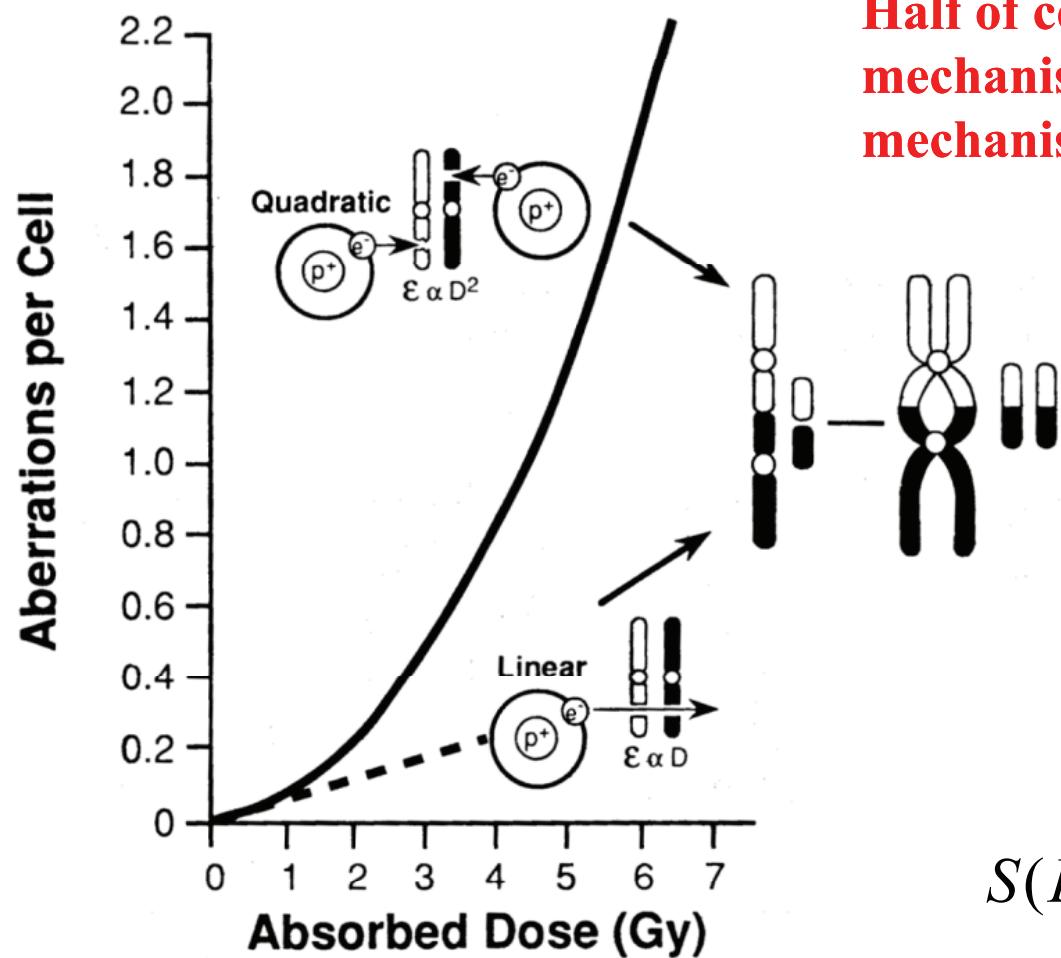
↓
Take logarithm, apply quadratic formula
and rearrange terms

$$D = \frac{\alpha / \beta}{2G} \left\{ -1 + \sqrt{1 - \frac{4G \ln S(D_R)}{\alpha(\alpha / \beta)}} \right\} = \frac{\alpha / \beta}{2G} \left\{ -1 + \sqrt{1 + \frac{4GD_R}{(\alpha / \beta)} \left(1 + \frac{G_R D_R}{\alpha / \beta} \right)} \right\}$$

D is the total treatment dose needed to achieve same biological effect as a reference treatment that delivers total dose D_R

Determined by the value of α/β and the dose protraction factor for the reference and alternate treatments (G_R and G)

One-Hit and Two-Hit Damage?



Half of cell killing due to one-track mechanism and half due to two-track mechanism

$$D = \frac{\alpha}{\beta}$$

\cong lethal aberrations

$$S(D) = \exp \left\{ - \left(\alpha D + \beta G D^2 \right) \right\}$$

($G = 1$ for an acute dose)

Conceptual Basis for G (*protraction factor*)?

Instantaneous absorbed dose rate
(e.g., Gy/h) at time t

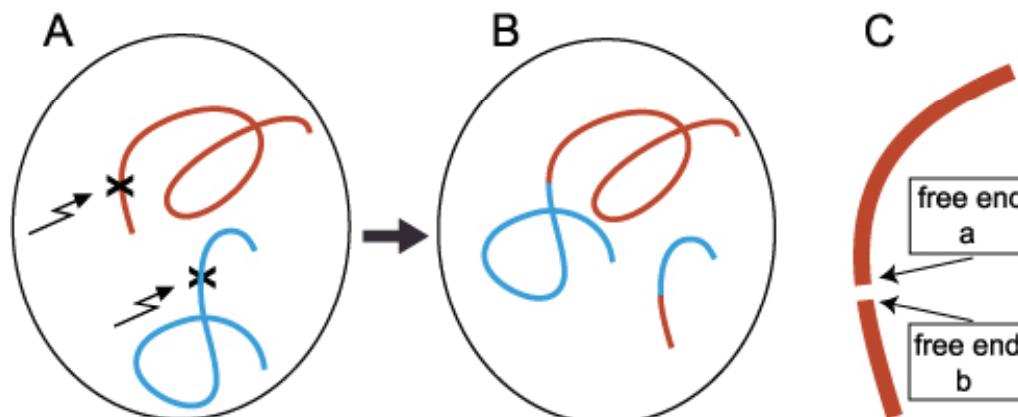
$$G = \frac{2}{D^2} \int_{-\infty}^{\infty} dt \dot{D}(t) \int_{-\infty}^t dt' \dot{D}(t') \exp\{-\lambda(t-t')\}$$

Absorbed dose (Gy)

Probability per unit time sub-lethal damage (= DSB) is rejoined

$\lambda = \frac{\ln 2}{\tau}$ ← Repair half-time

$$S(D) = \exp\{-(\alpha D + \beta GD^2)\}$$



Protraction Factor – n daily fractions

Series of n daily fractions

$$G = \frac{g}{n} \simeq \frac{1}{n} \quad \text{if } \Delta t \ll \tau$$

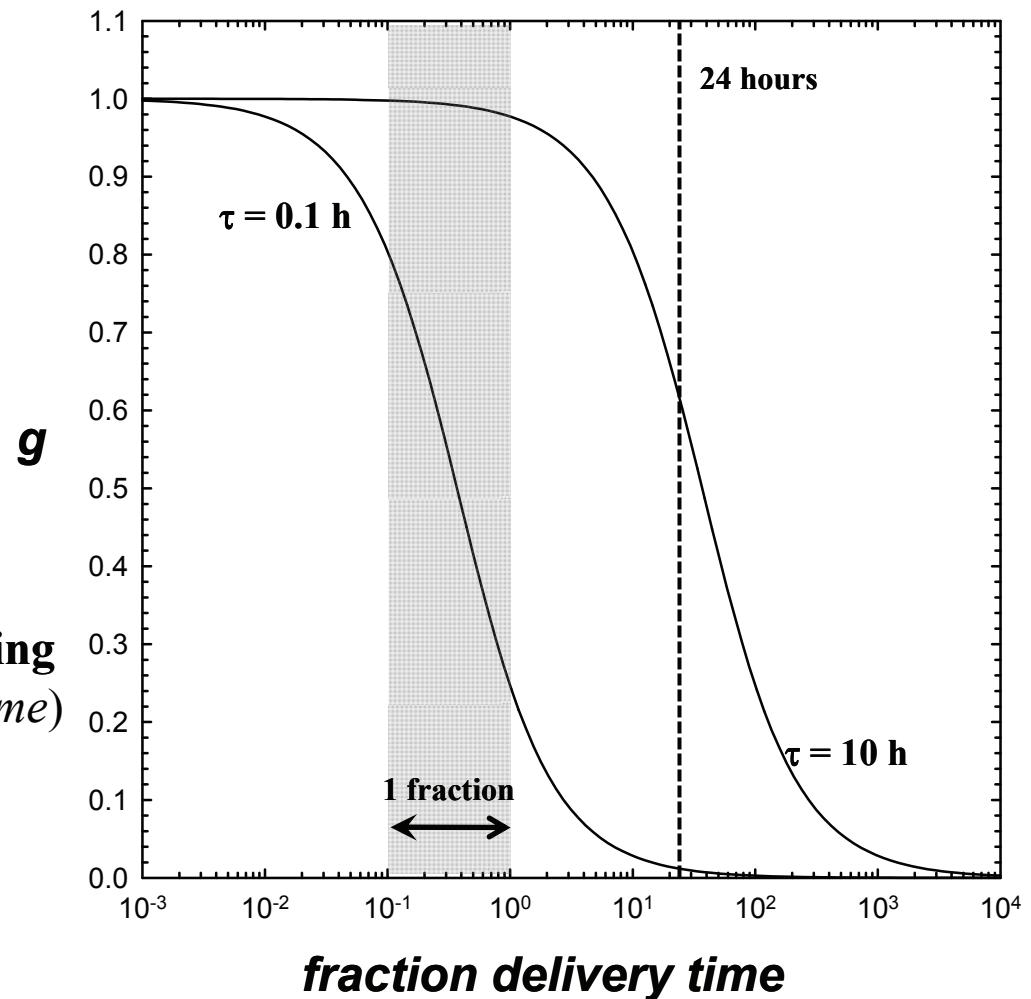
(assumes repair complete between fractions)

$$S(D) = \exp \left\{ - \left(\alpha D + \beta G D^2 \right) \right\}$$

Dose d (fraction size) delivered during time interval Δt (fraction delivery time)

$$g = 2(e^{-x} + x - 1) / x^2$$

$$x \equiv \lambda \Delta t = \Delta t \ln 2 / \tau$$



g is always between 0 (large delivery time) and 1 (short delivery times)

Equivalent Fractionation Schedules?

$$D = \frac{\alpha / \beta}{2G} \left\{ -1 + \sqrt{1 + \frac{4GD_R}{(\alpha / \beta)} \left(1 + \frac{G_R D_R}{\alpha / \beta} \right)} \right\}$$

$G \cong 1/n$
 $G \cong 1/n_R$

Determine biologically equivalent dose D by adjusting the physical parameter n

$$D = \frac{n}{2} (\alpha / \beta) \left\{ -1 + \sqrt{1 + \frac{4D_R}{n(\alpha / \beta)} \left(1 + \frac{D_R}{n_R(\alpha / \beta)} \right)} \right\}$$

Reference Treatment
("clinical experience")

D_R = total dose (Gy)

n_R = number fractions

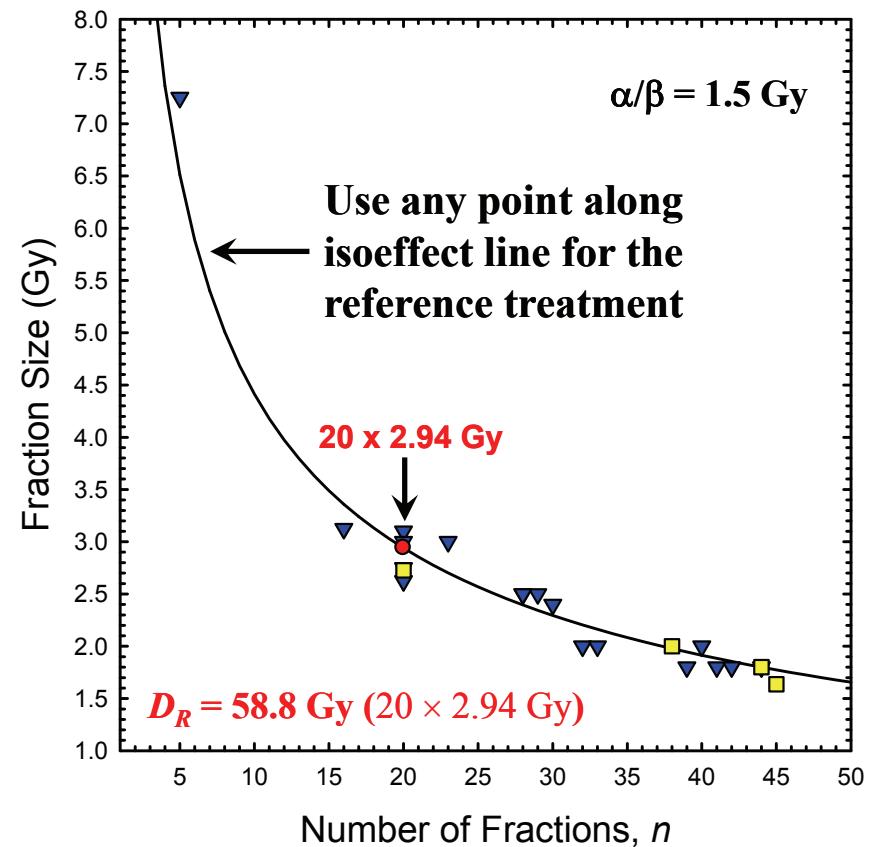
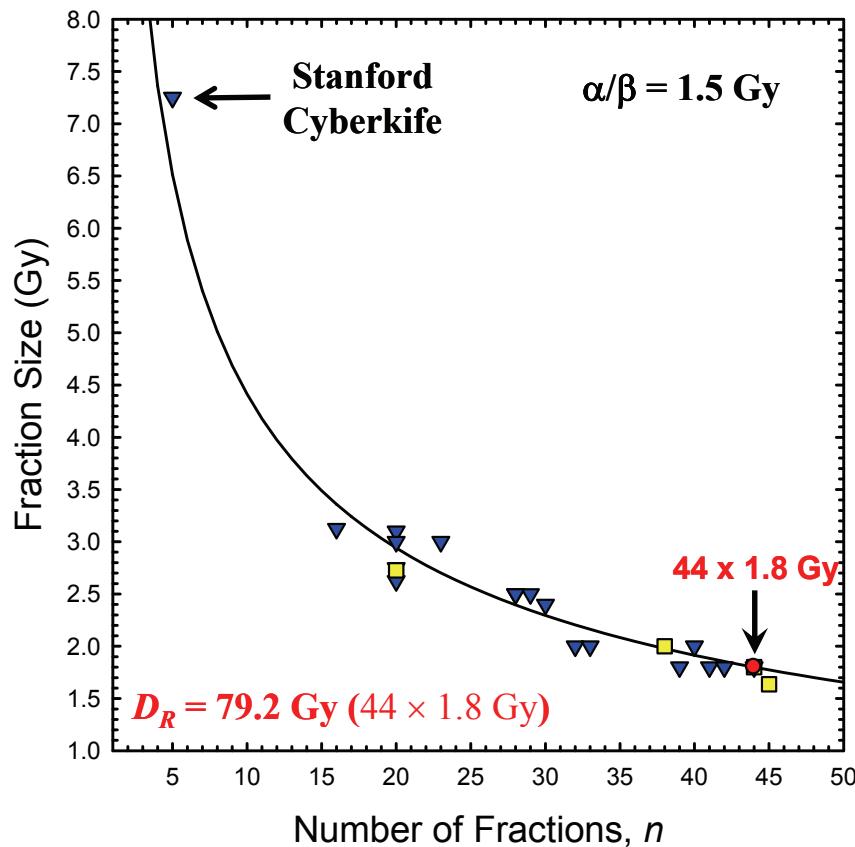
$d_R = D_R/n_r$ (fraction size)

New (alternate) Treatment

n = desired number fractions

Uncertainty in D mainly arises from uncertainties associated with α/β .

Equivalent Treatments (*prostate cancer*)



$$D = \frac{n}{2}(\alpha / \beta) \left\{ -1 + \sqrt{1 + \frac{4D_R}{n(\alpha / \beta)} \left(1 + \frac{D_R}{n_R(\alpha / \beta)} \right)} \right\}$$

Inter-Patient Heterogeneity

$$D = \frac{n}{2}(\alpha / \beta) \left\{ -1 + \sqrt{1 + \frac{4D_R}{n(\alpha / \beta)} \left(1 + \frac{D_R}{n_R(\alpha / \beta)} \right)} \right\}$$

When applied to a patient population, we are implicitly assuming that α/β is the same for *all patients* for the reference *and* alternate treatment – an assumption that is *surely* incorrect!

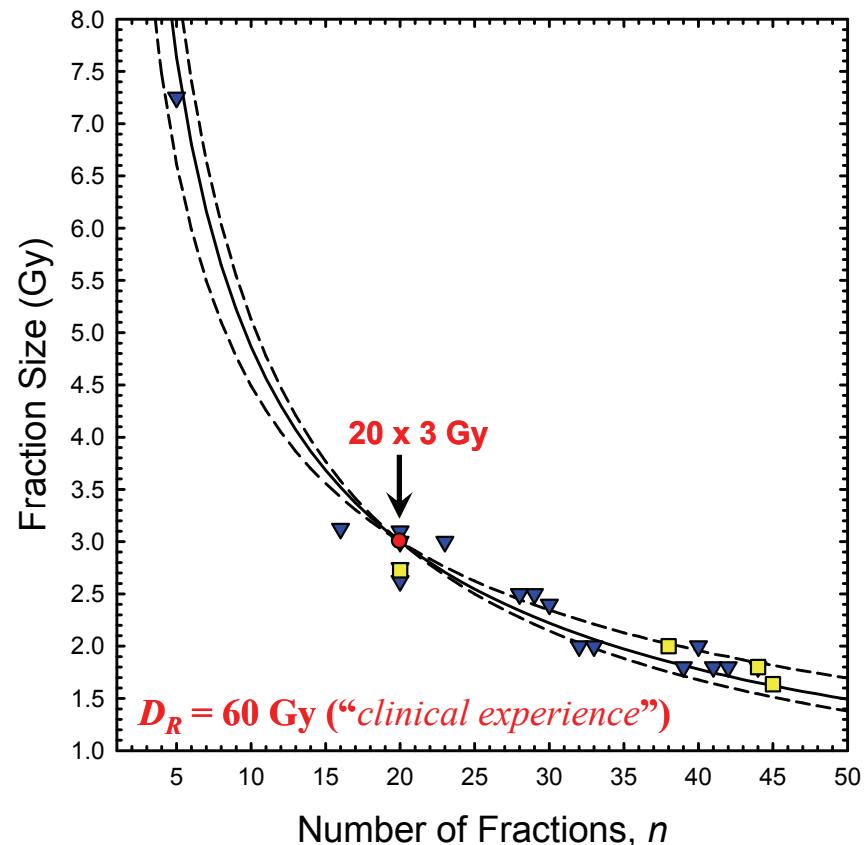
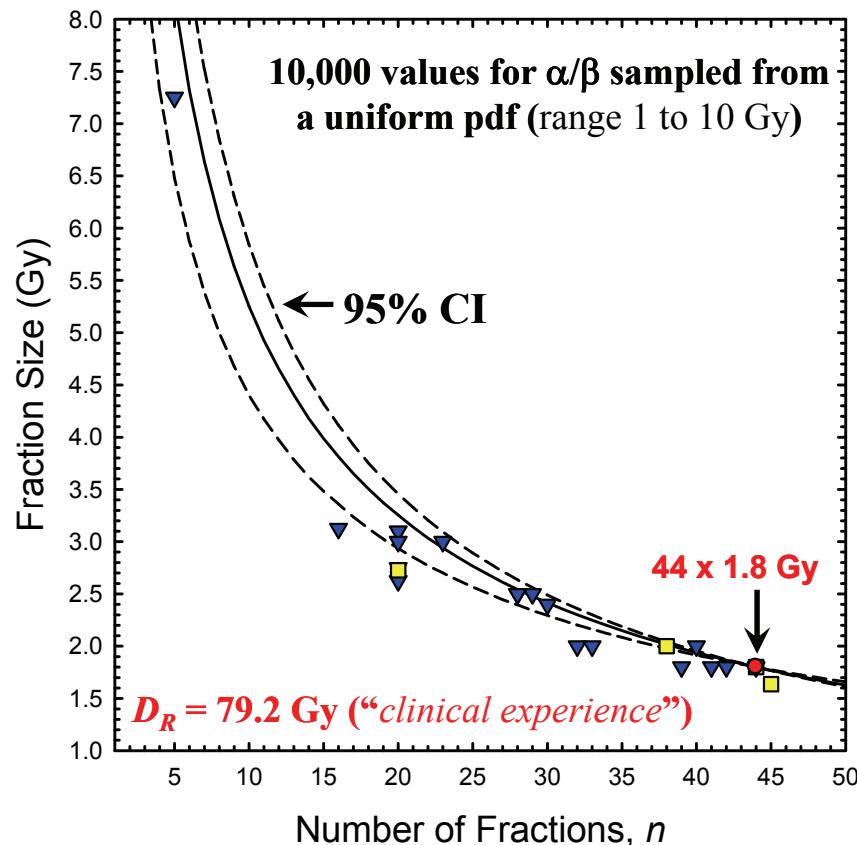
Inter-Patient Heterogeneity

Hypothesis: All patients have a different α/β (*unknown distribution*). BUT... same value of α/β is appropriate (*as a first approximation*) for all treatments in the same patient.

How does inter-patient heterogeneity influence our ability to determine equivalent prescription doses?

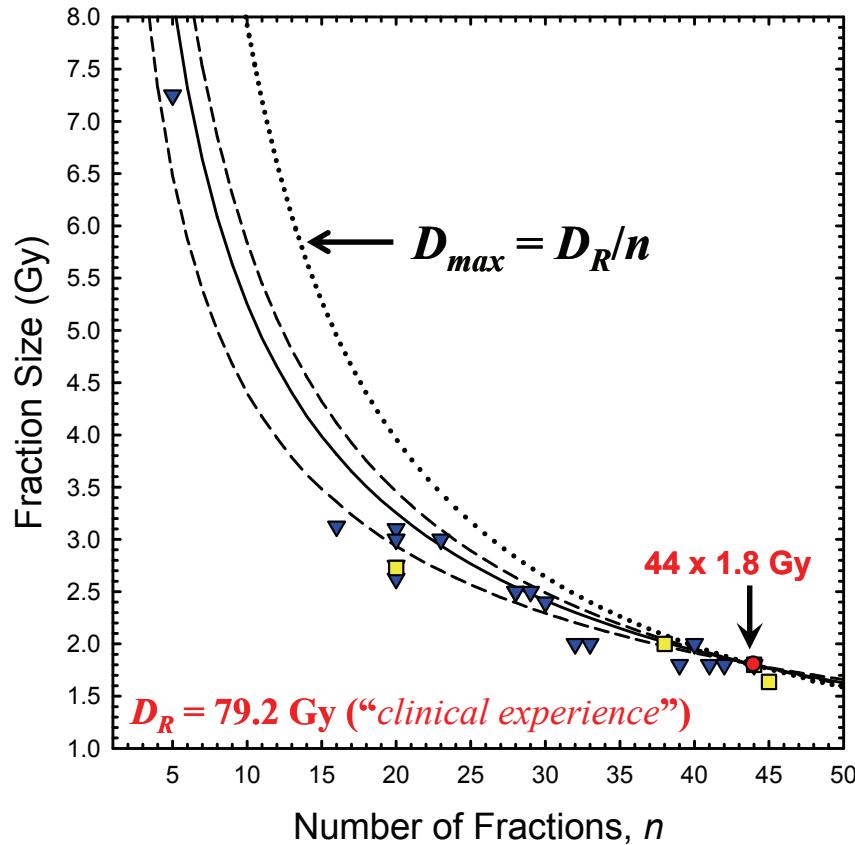
How sensitive are estimates of D to uncertainties in α/β ?

Effects of Inter-Patient Heterogeneity



Key Point #1: Small changes from an accepted fractionation schedule quite reasonable – even for a *very* heterogeneous patient population

Special Case – Fraction Size $d \ll \alpha/\beta$



For the special case when $d \ll \alpha/\beta$,
 $S \approx \exp(-\alpha D)$ and

$$S(D_R) = S(D)$$
$$\exp(\alpha n R d_R) \approx \exp(\alpha n d)$$

Maximum fraction size required for biological equivalence (iso-TCP)
 $d \approx D_R/n$

$$n = 44 \rightarrow 40 \text{ (3.48\%)}$$

$$n = 44 \rightarrow 35 \text{ (8.60\%)}$$

Uncertainty comparable to differences in prescription dose among institutions and to uncertainties arising from treatment delivery...

Repopulation Effects

When radiation is protracted over time intervals comparable to or longer than the doubling time (T_d) additional cell killing is required to eradicate the tumor

$$S(D) = e^{\gamma T} S(D) = e^{\gamma T} \times \exp \left[-\alpha D \left(1 + \frac{GD}{\alpha / \beta} \right) \right]$$

$$\gamma \equiv \frac{\ln 2}{T_d} \quad = \exp \left[-\alpha D \left(1 + \frac{GD}{\alpha / \beta} \right) + \gamma T \right]$$

Correction for cell division
over time interval T
(γT must be dimensionless)

$$T = (n - 1) + 2 \text{int}[(n - 1)/5]$$

Assume treatment starts on Monday

Equivalent dose – repair and repopulation

Reference Treatment = Alternate Treatment

$$S(D_R) = S(D)$$

$$\exp(-\alpha D_R - \beta G D_R^2 + \gamma T_R) = \exp(-\alpha D - \beta G D^2 + \gamma T)$$

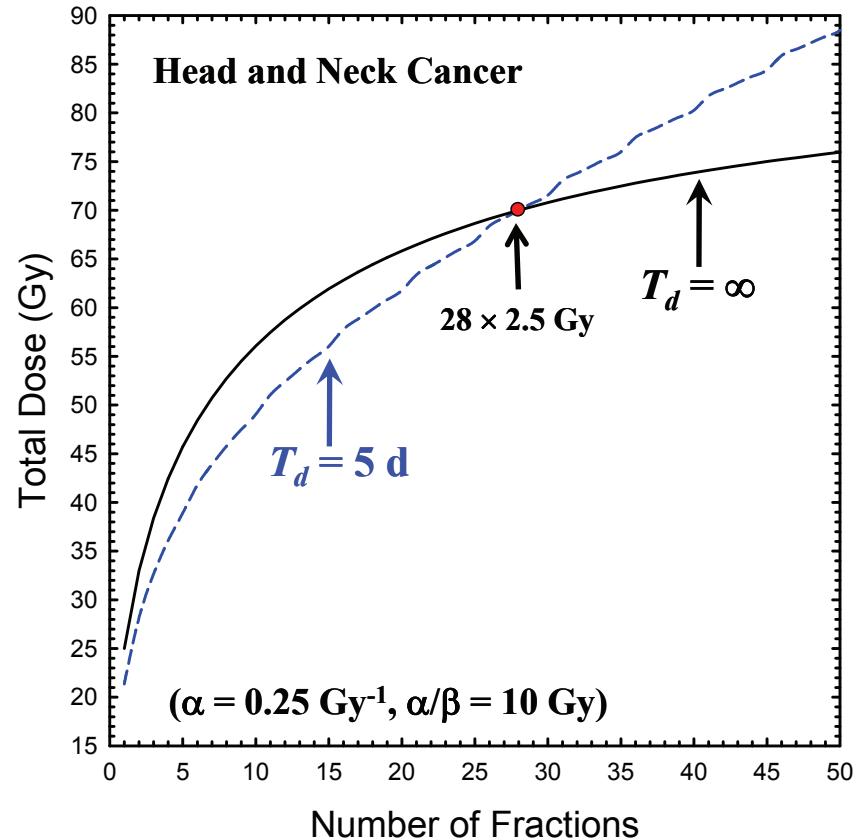
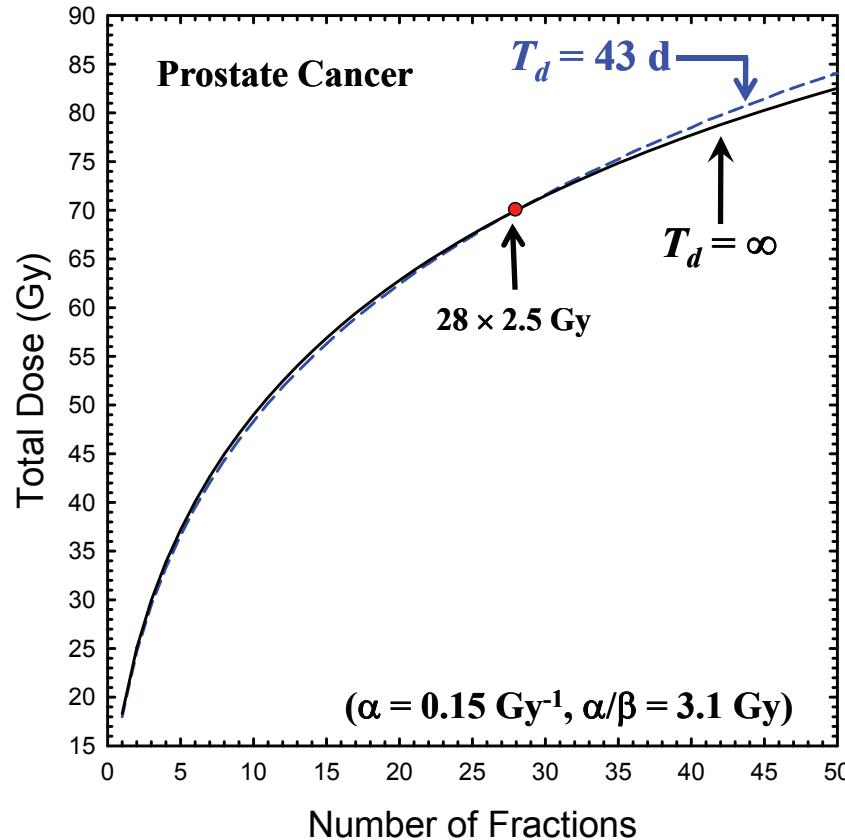
↓
Take logarithm, apply quadratic formula
and rearrange terms

$$D = \frac{\alpha / \beta}{2G} \left\{ -1 + \sqrt{1 + \frac{4GD_R}{\alpha / \beta} \left[1 + \frac{G_R D_R}{\alpha / \beta} - \frac{\gamma(T_R - T)}{\alpha D_R} \right]} \right\}$$

D is the total treatment dose needed to achieve same biological effect as a reference treatment that delivers total dose **D_R**

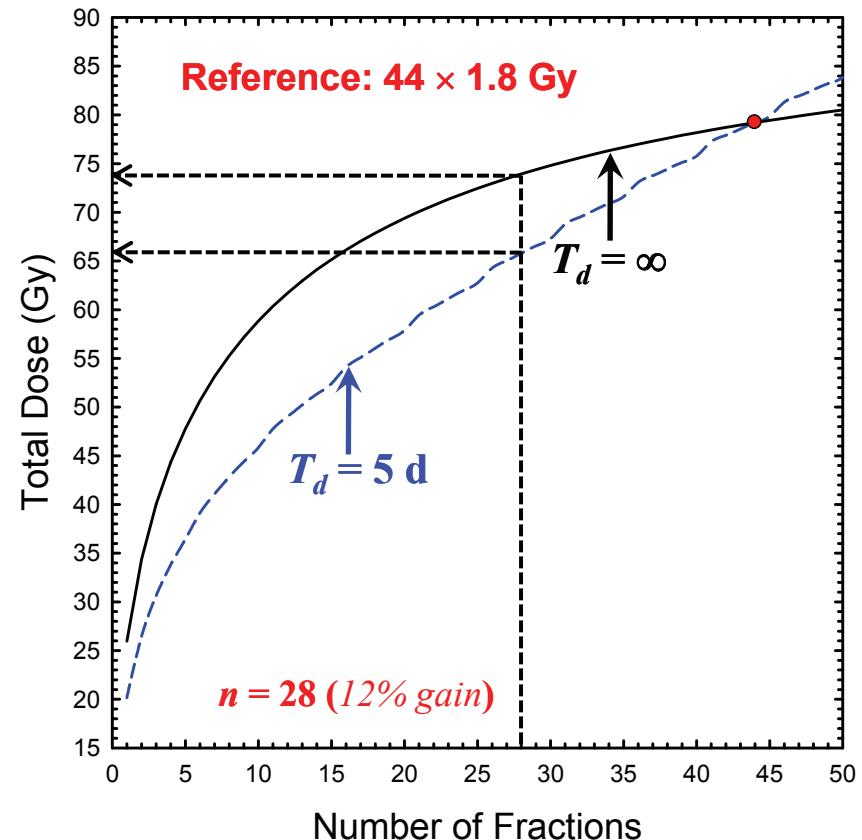
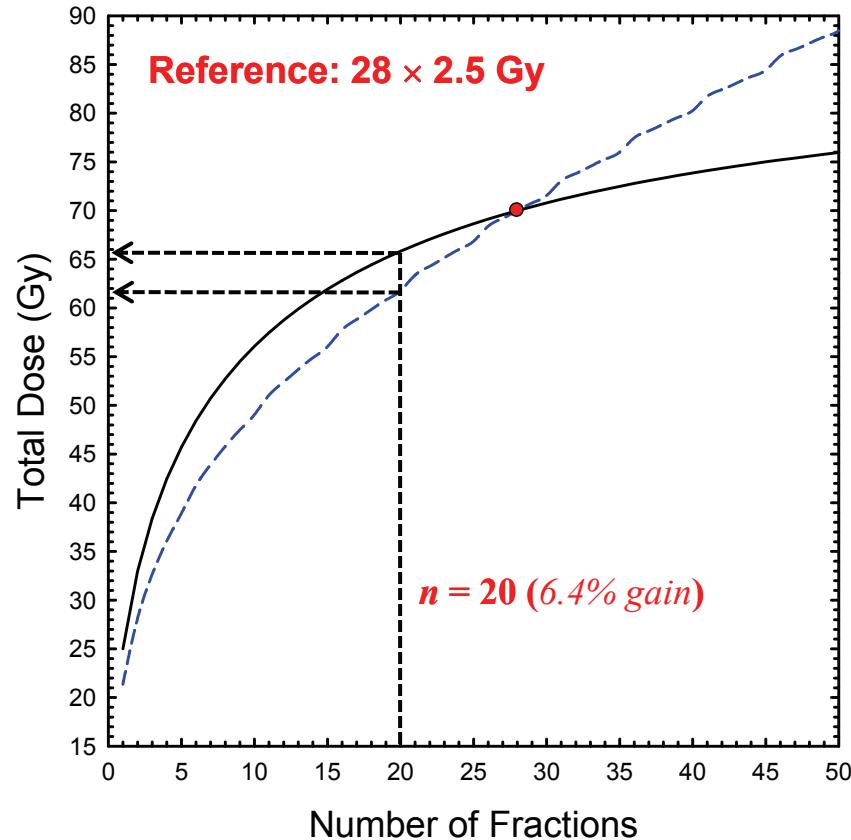
Determined by the value of α/β (in Gy), γ/α (in Gy/day) and the dose protraction factor for the reference and alternate treatments (**G** and **G_R**)

Repopulation Effects – Fast and Slow Growing Tumors



Repopulation effects are negligible for slow growing tumors but potentially very significant for fast growing tumors

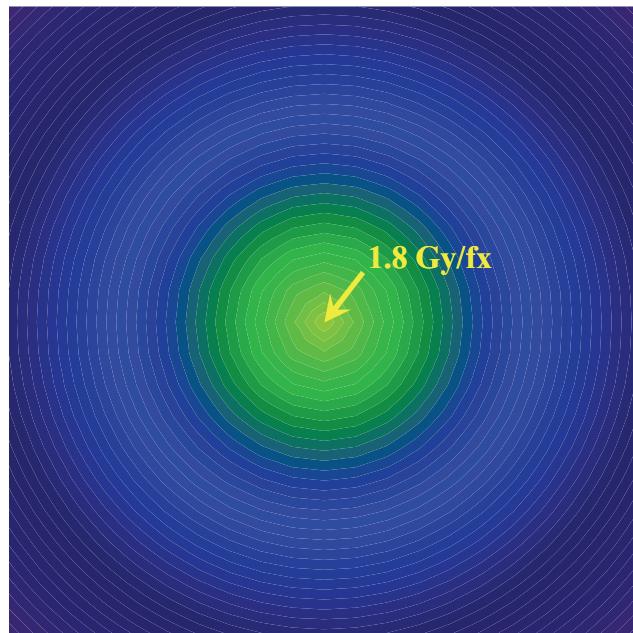
Are gains in tumor control significant?



Key Point #2: Clinical significance of potential gains (*or losses*) are easily judged when expressed in terms of physical dose.

Isoeffective Dose Distributions

Absolute dose distributions (*in Gy*) typically determined through application of a calibration factor (Gy/MU) at a reference location

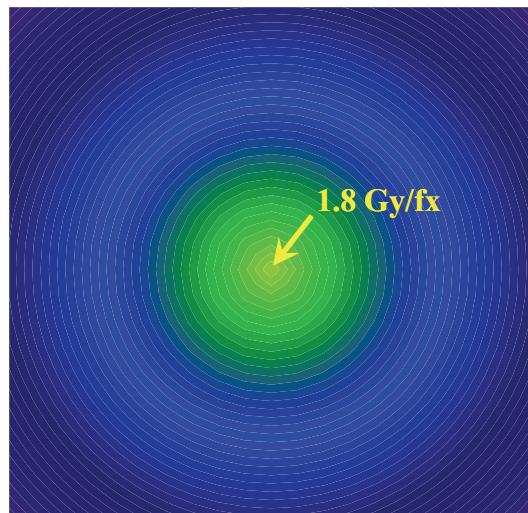


Prescription dose specified at center ($44 \times 1.8 \text{ Gy} = 79.2 \text{ Gy}$)

44 fractions

Equivalent dose distributions?

Scale the dose distribution by a ratio of biologically equivalent prescription doses ($n = 44 \rightarrow n = 20$)



44 fractions

$$D = \frac{n}{2}(\alpha / \beta) \left\{ -1 + \sqrt{1 + \frac{4D_R}{n(\alpha / \beta)} \left(1 + \frac{D_R}{n_R(\alpha / \beta)} \right)} \right\}$$

$$\alpha/\beta = 1.5 \text{ Gy}$$

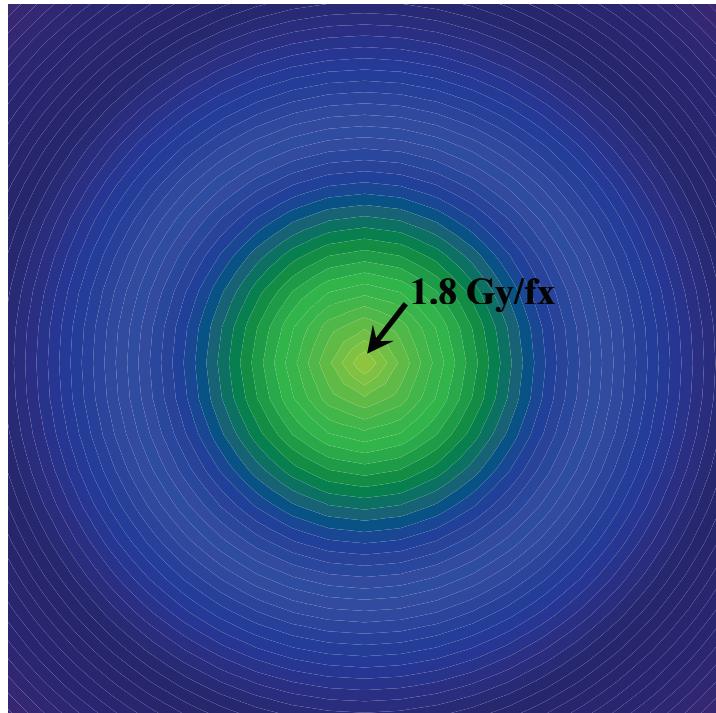
$$n_R = 44 \quad D_R = 79.2 \text{ Gy} \quad (d_R = 1.8 \text{ Gy})$$

$$n = 20 \text{ (new)} \quad D = 58.8 \text{ Gy} \quad (d_R = 2.94 \text{ Gy})$$

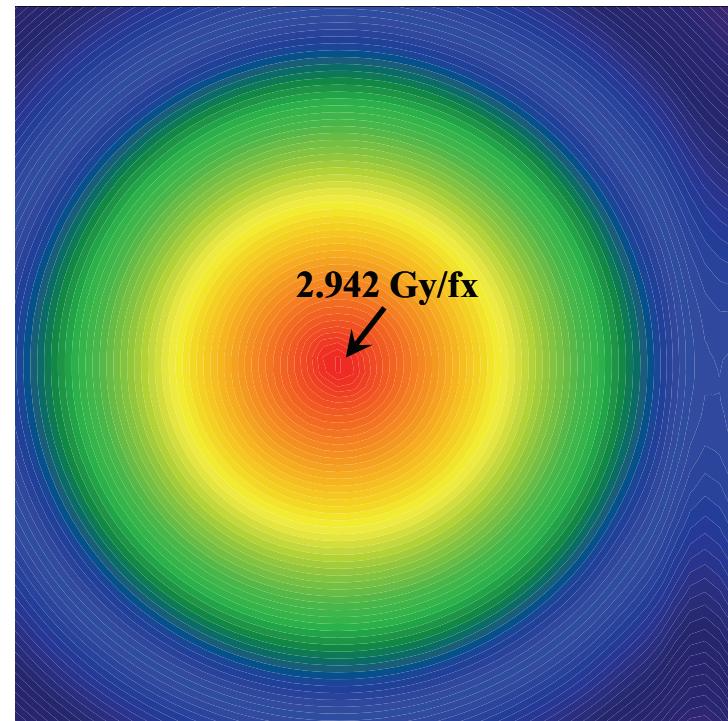
Dose to i^{th} voxel in new treatment

$$d^i = \frac{d}{d_R} d_{R,i} = \frac{2.94 \text{ Gy}}{1.8 \text{ Gy}} d_R^i = 1.6333 d_R^i$$

Dose Distribution ($n = 44 \rightarrow 20$) – MU scaling



44 fractions



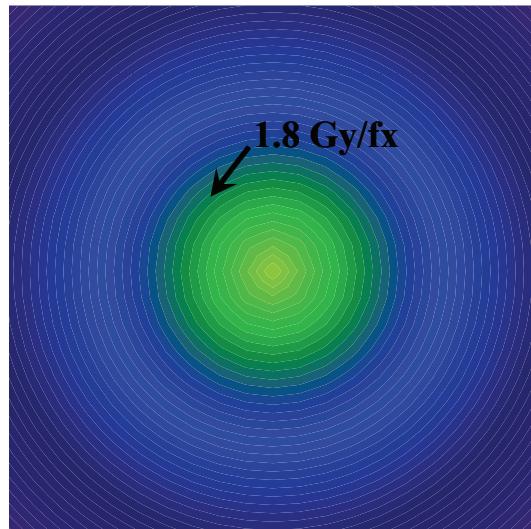
20 fractions

Same biological effect at center ($n = 44$ and 20).
But same biological effect at other locations??

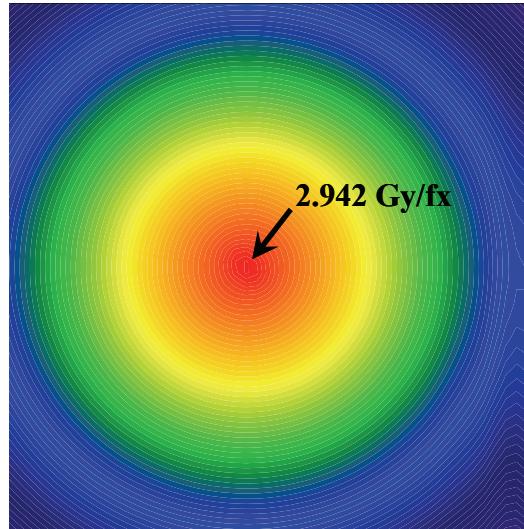
Biologically Equivalent Dose Distributions

dose to
 i^{th} voxel

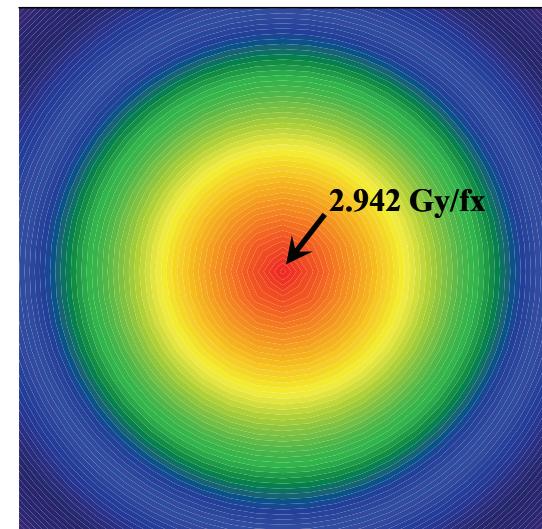
$$D^i = \frac{n}{2}(\alpha / \beta) \left\{ -1 + \sqrt{1 + \frac{4D_R^i}{n(\alpha / \beta)} \left(1 + \frac{D_R^i}{n_R(\alpha / \beta)} \right)} \right\} \quad \alpha/\beta = 1.5 \text{ Gy}$$



44 fractions
(original)



20 fractions
(scaled using dose at center)

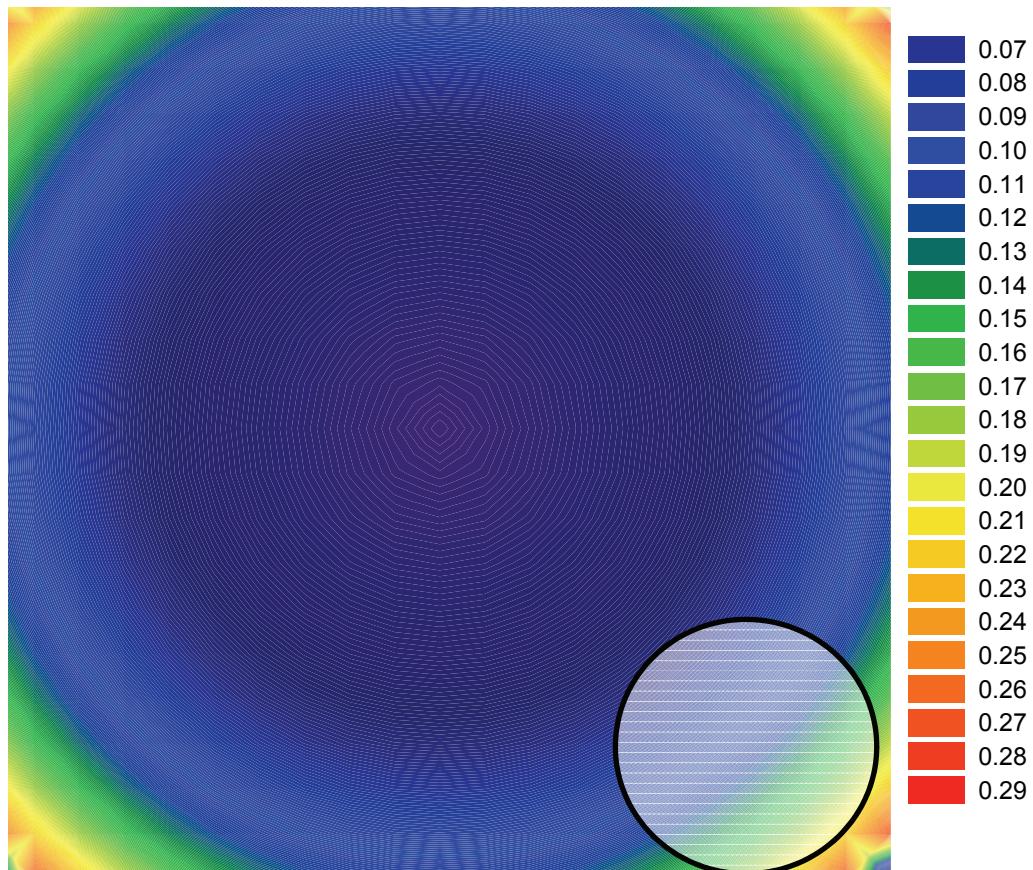


20 fractions (isoeffect)



Isoeffect dose is up to 27% larger than the distribution scaled by dose (or MU or fluence)

Dose Distribution Difference ($n = 20$)

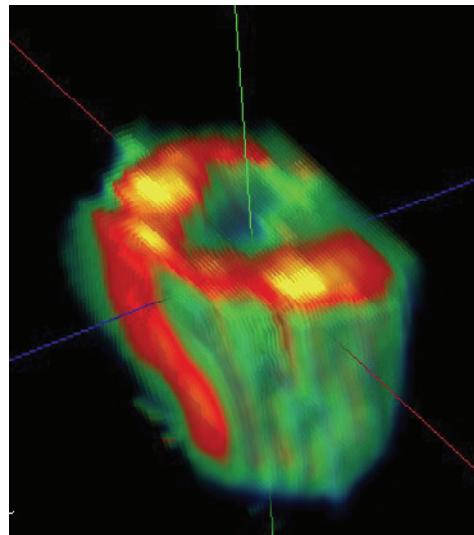


**Scaling by physical quantities
underestimates isoeffect dose
by up to 27% ($n = 44 \rightarrow 20$)**

**Dose “scaling” effects
become more important as
fraction size increases
(because of βD^2 term)**

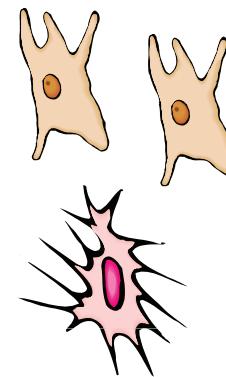
Key Point #3: Scaling dose distributions by maximum dose (or fluence or monitor units) at a point may *underestimate* tolerance dose for normal tissues

Intra-Tumor Heterogeneity



Representative DCE-CT image of a tumor
(Courtesy Minsong Cao, IUSM)

- Genomic Instability
- Repair
- Repopulation
- Reassortment
- Reoxygenation



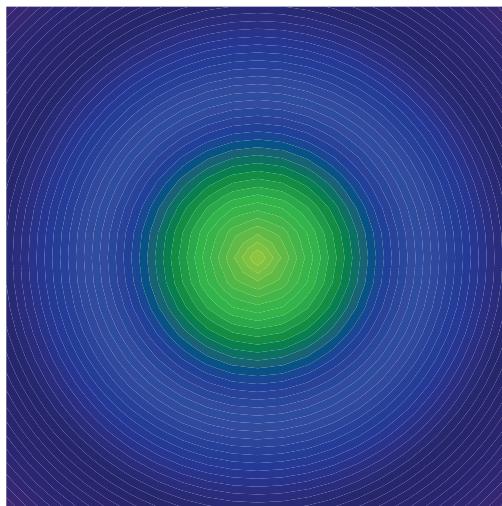
How does intra-tumor heterogeneity influence our ability to determine biologically equivalent *dose distributions*?

Imagine that...

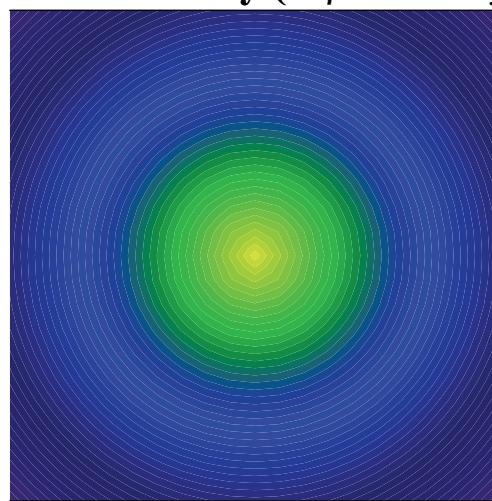
Individual cells have different values of α/β (*unknown distribution*). But, again, same for all treatments as a *first approximation*

Effect of intra-tumor heterogeneity

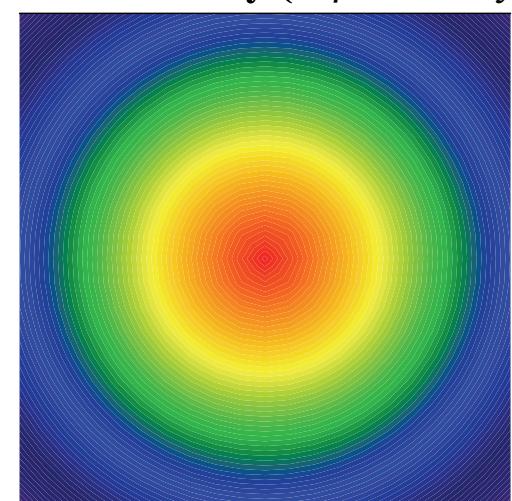
44×1.80 Gy (original)



39×1.95 Gy ($\alpha/\beta = 1.5$ Gy)

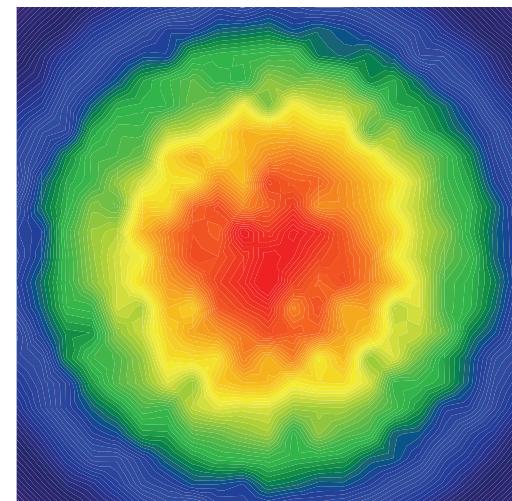
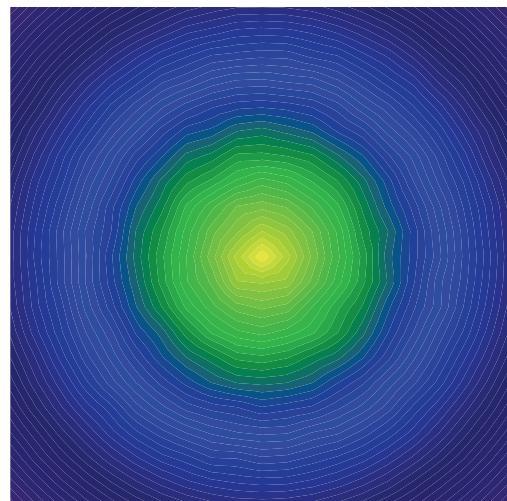


20×2.94 Gy ($\alpha/\beta = 1.5$ Gy)



0.0
0.2
0.4
0.6
0.8
1.0
1.2
1.4
1.6
1.8
2.0
2.2
2.4
2.6
2.8
3.0

α/β sampled from a uniform pdf (range 1 to 10 Gy) on a voxel by voxel basis



Fractionated EBRT → Brachytherapy

Dose for a brachytherapy procedure (*again*) determined by

$$D = \frac{\alpha / \beta}{2G} \left\{ -1 + \sqrt{1 + \frac{4GD_R}{\alpha / \beta} \left[1 + \frac{G_R D_R}{\alpha / \beta} - \frac{\gamma(T_R - T)}{\alpha D_R} \right]} \right\}$$

Reference Treatment
("clinical experience")

D_R = total dose (Gy)

n_R = number fractions

d_R = D_R/n_r (fraction size)

T_R = $(n_R - 1) + 2\text{int}[(n_R - 1)/5]$

Brachytherapy Procedure

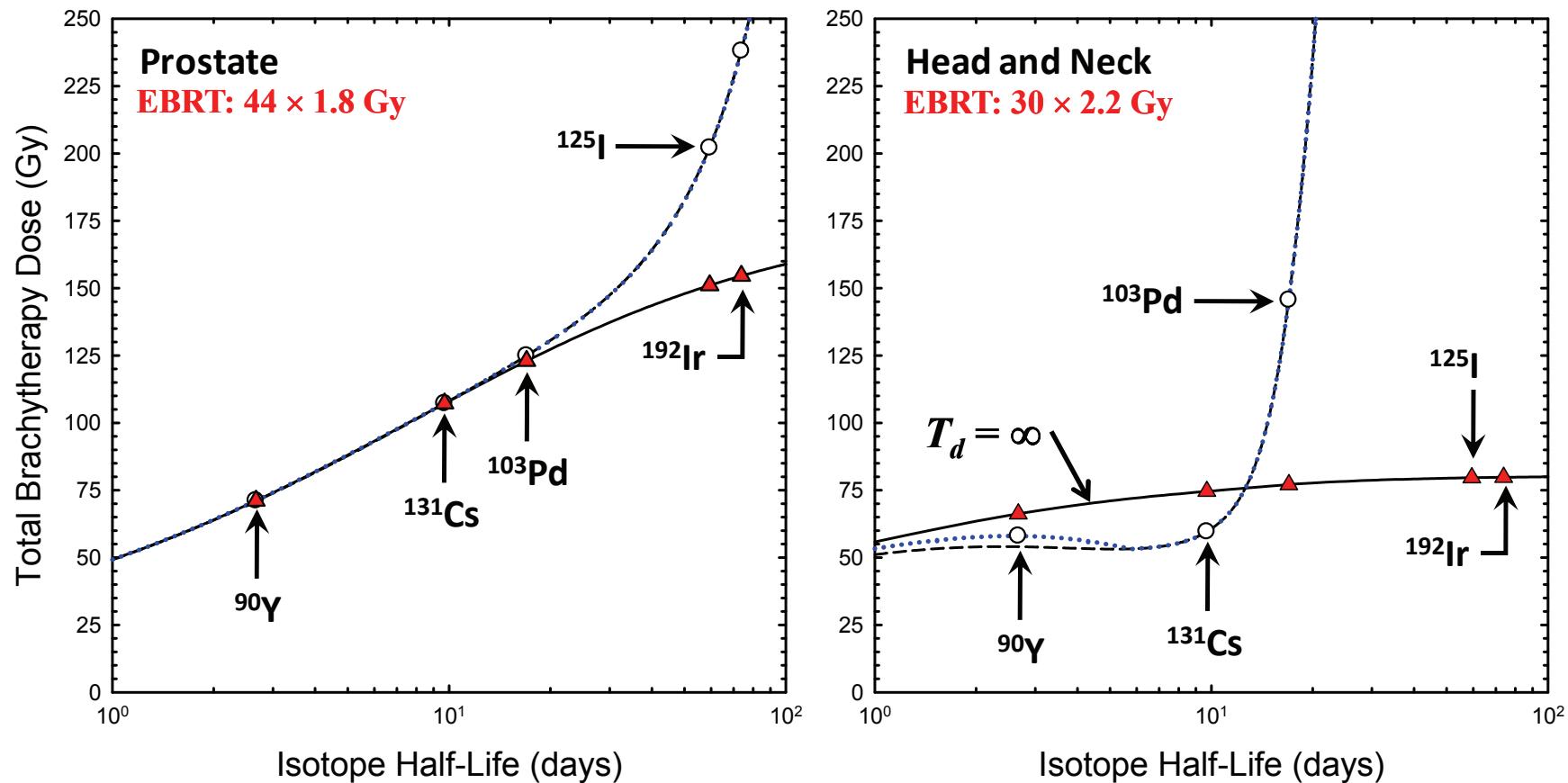
$$G = G_\infty \left\{ \frac{(1+x)}{(1-x)} - \frac{yx^2}{(1-x)^2} \left[1 - e^{-(\lambda-\mu)T} \right] \right\}$$

$$G_\infty \equiv \mu / (\mu + \lambda) \quad x \equiv \exp(-\mu T)$$

$$\begin{array}{ccc} \uparrow & \uparrow & \\ \text{relates to} & & \\ \text{Isotope} & \text{Repair} & \\ \text{Half-life} & \text{Half-time} & \\ & & \\ & & y \equiv 2\mu / (\lambda - \mu) \end{array}$$

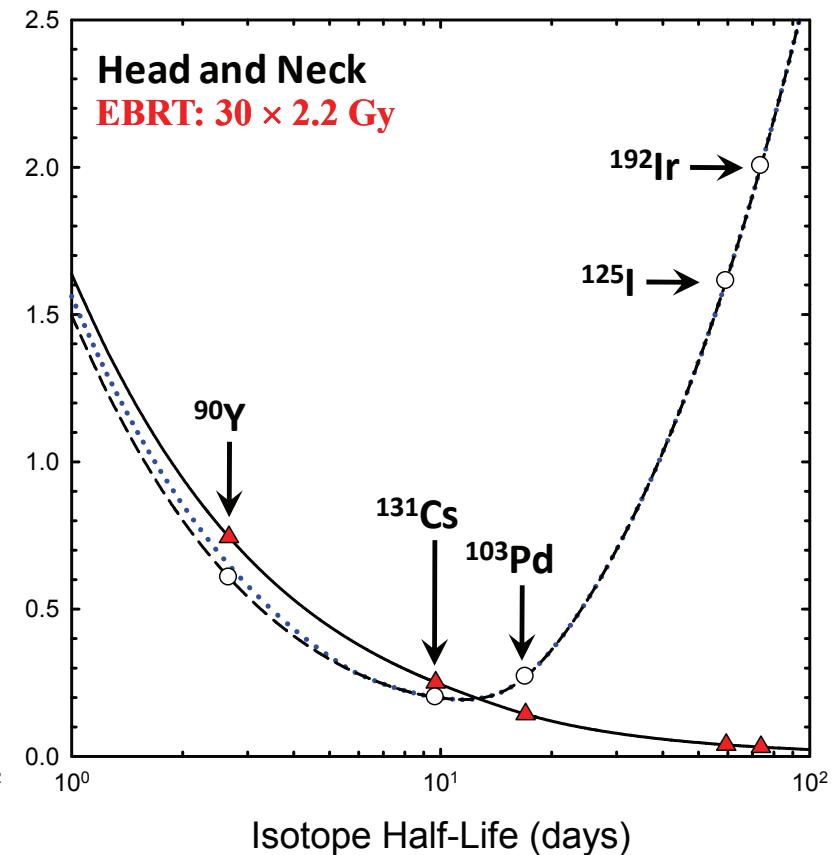
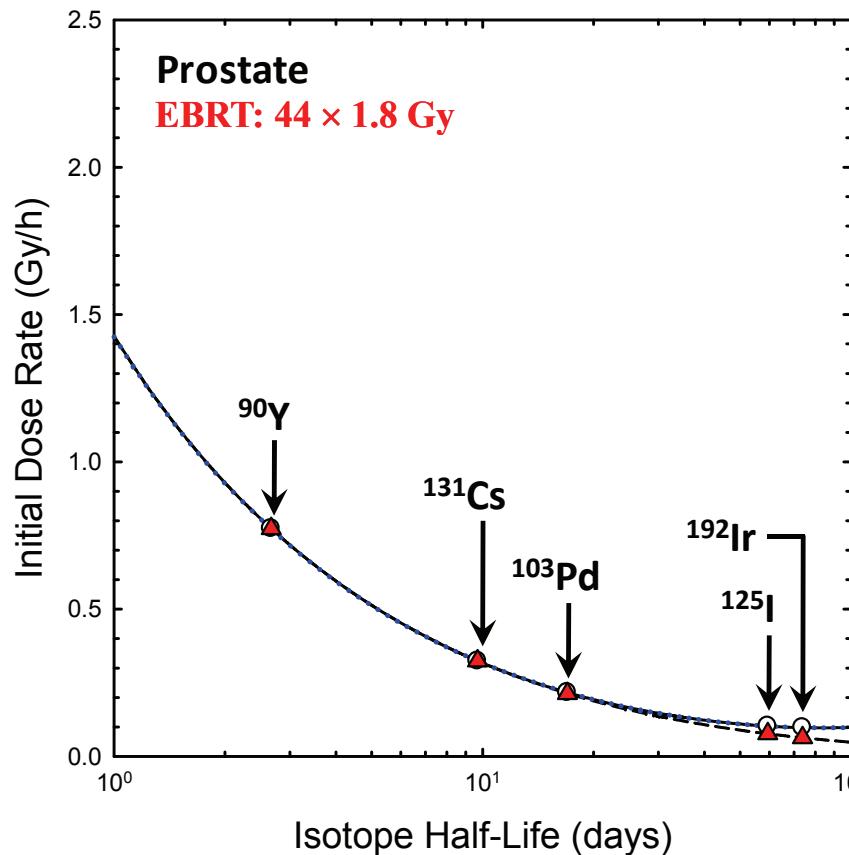
T = effective treatment time

Brachytherapy – Isotope Selection and Dose



Biologically equivalent brachytherapy doses for **prostate cancer (left panel)** and **head and neck cancer (right panel)**.
Prostate ($T_d = 43$ days): $T_k = 0$ days (**black dashed line**) or $T_k = 60$ days (**blue dotted line**). **Head and Neck** ($T_d = 5$ days): $T_k = 0$ days (**black dashed line**) or $T_k = 21$ days (**blue dotted line**). **Solid black lines:** not corrected for repopulation effects ($T_d = \infty$).

Brachytherapy – Initial Dose Rate



Initial brachytherapy dose rates for **prostate cancer** (left panel) and **head and neck cancer** (right panel). **Prostate** ($T_d = 43$ days): $T_k = 0$ days (black dashed line) or $T_k = 60$ days (blue dotted line). **Head and Neck** ($T_d = 5$ days): $T_k = 0$ days (black dashed line) or $T_k = 21$ days (blue dotted line). **Solid black lines**: not corrected for repopulation effects ($T_d = \infty$).

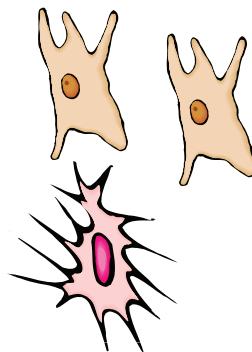
Summary and Conclusions

- **Direct application of TCP (and NTCP) modeling may result in the selection of inappropriate or suboptimal treatment parameters or modalities**
 - Too many parameters – very challenging to estimate from clinical data
 - Predictions very sensitive to parameter uncertainties
 - Prediction of individual outcomes unlikely (*foreseeable future*)
 - *But* general trends in dose-response behavior of a patient population can be predicted despite inter-patient and intra-tumor heterogeneity
- **Isoeffect calculations are a useful alternative**
 - Uncertainties and limitations mitigated through use of prior clinical experience (“*dose or dose distribution for an accepted treatment*”)
 - Focus on most important parameters, such as α/β (Gy) and γ/α (Gy/day)
 - Easy to judge potential gains and losses in treatment effectiveness in terms of *physical dose* (< 3-5% change in dose not significant)
 - Guide design of dose escalation studies, compare effectiveness of EBRT and brachytherapy, isotope selection and initial dose rate, ...

A Path to Treatment Individualization

Develop distributions of parameters for sub-populations
(biomarkers, functional imaging, ...)

- Repair
- Repopulation
- Reassortment
- Reoxygenation

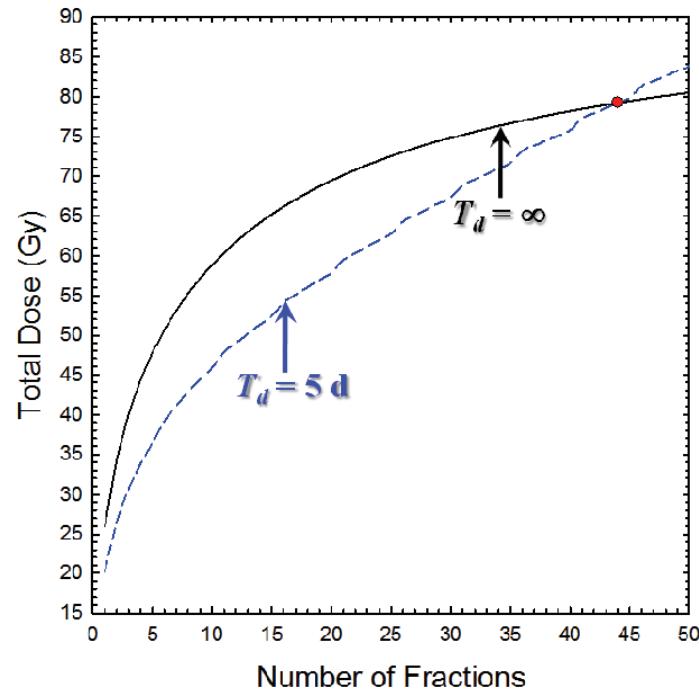


Group 1

$$\begin{aligned}\alpha/\beta &\approx 2-5 \text{ Gy} \\ \gamma/\alpha &< 10 \text{ Gy/day}\end{aligned}$$

Group 2

$$\begin{aligned}\alpha/\beta &\approx 3-8 \text{ Gy} \\ \gamma/\alpha &> 50 \text{ Gy/day}\end{aligned}$$



α/β relates to fraction-size sensitivity (*repair, oxygen effects, genetic factors, cell kinetics*)
 γ/α related to cell loss, growth fraction, hypoxia, tumor responsiveness (*shrinkage?*), ...

Estimating Parameters from Clinical Data

Don't we need TCP and NTCP models to estimate biological parameters?

Group 1

$$\alpha/\beta \approx 2-5 \text{ Gy}$$
$$\gamma/\alpha < 10 \text{ Gy/day}$$

Group 2

$$\alpha/\beta \approx 3-8 \text{ Gy}$$
$$\gamma/\alpha > 50 \text{ Gy/day}$$

If so, what about uncertainties in ρV ? Inter-patient heterogeneity? Intra-tumor heterogeneity?

