

Models and Mechanisms Connecting Physics and Biology at Multiple Scales in the Biological Hierarchy

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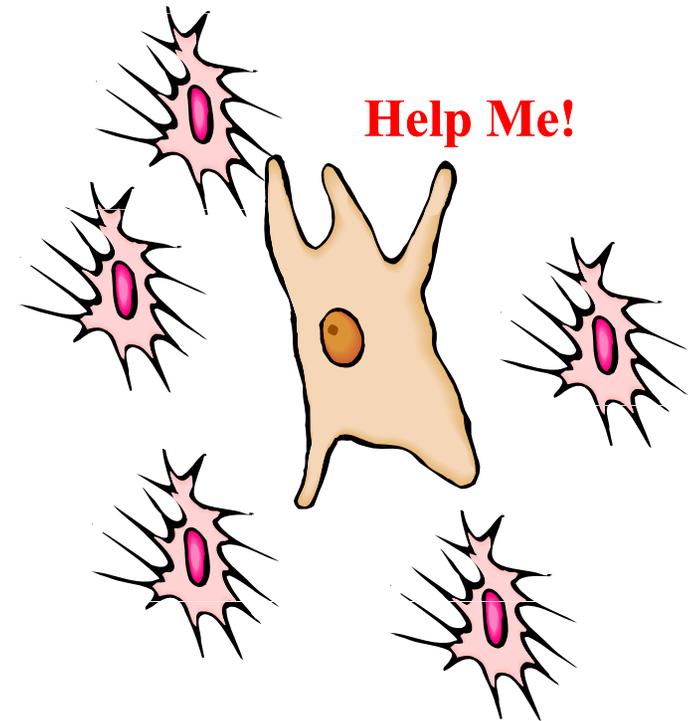
Presented at 2014 AAPM Meeting, Austin, TX

Session: TU-A-BRE-3 (*last number indicates order within session*)

Date and Time: Tuesday July 22, 2014 from 7:30 to 9:30 am

Location: Ballroom E

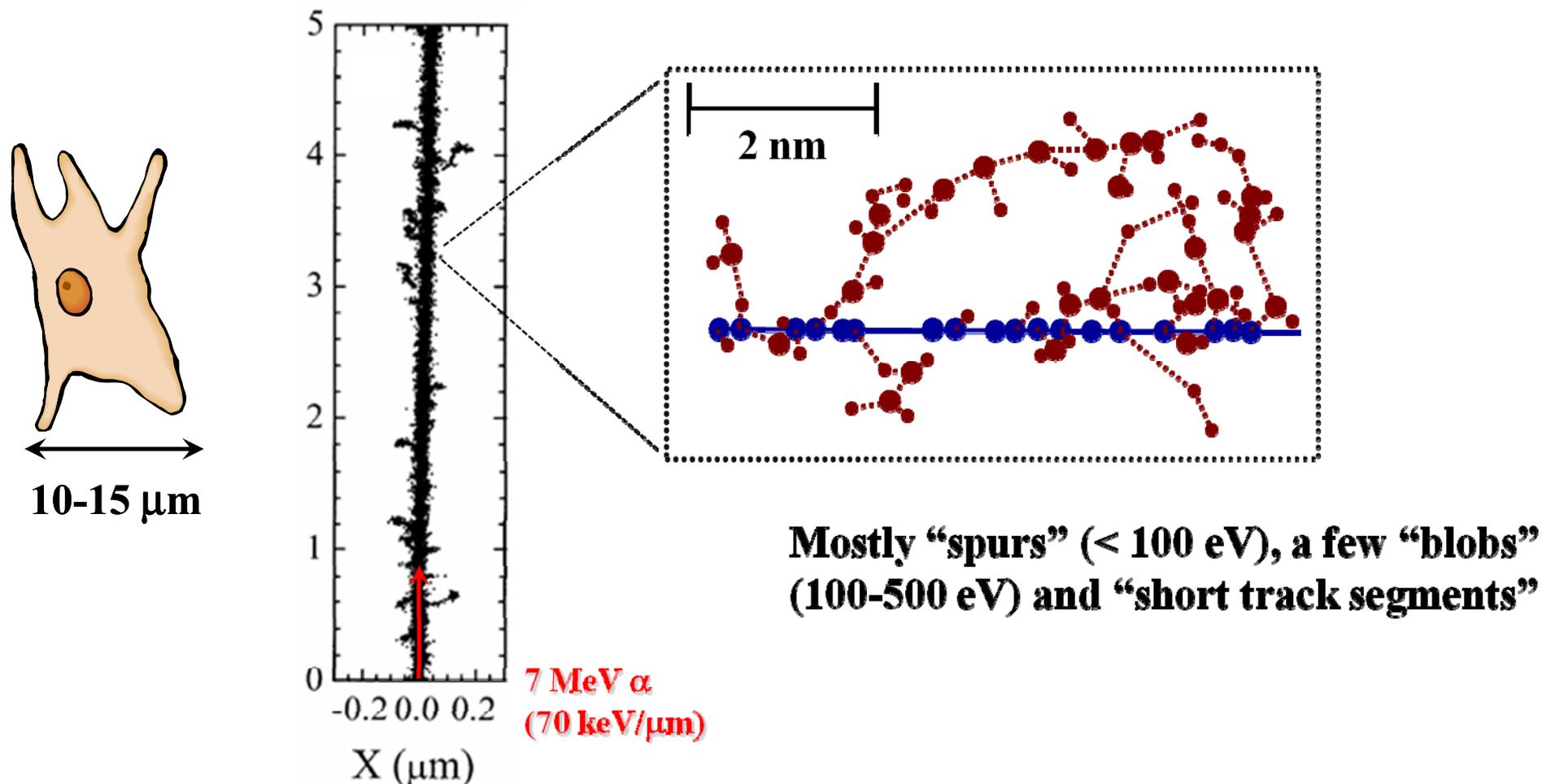
Abstract #23482



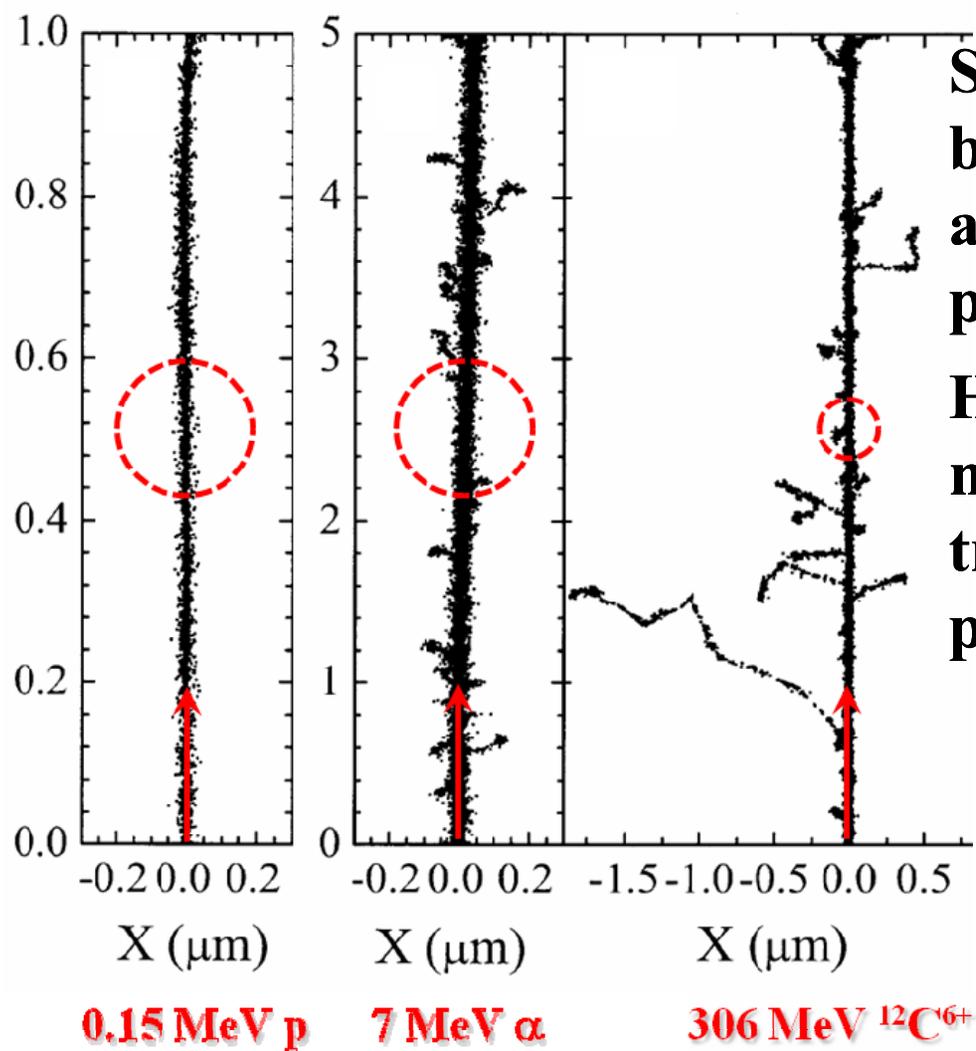
Learning Objectives

- **Review models and mechanisms connecting radiation biology at the molecular and cellular levels to radiation biology at the tumor and tissue level**
 - Focus on effects of particle linear energy transfer (LET)
- **Is the RBE for DNA damage useful for predicting cell survival?**
- **Is the RBE for cell survival useful for predicting the RBE for *clinical endpoints*?**

Spatial Pattern of Energy Deposits on the Molecular and Cellular Levels (“Track Structure”)



Tracks formed by ions in water (**70 keV/ μm**)

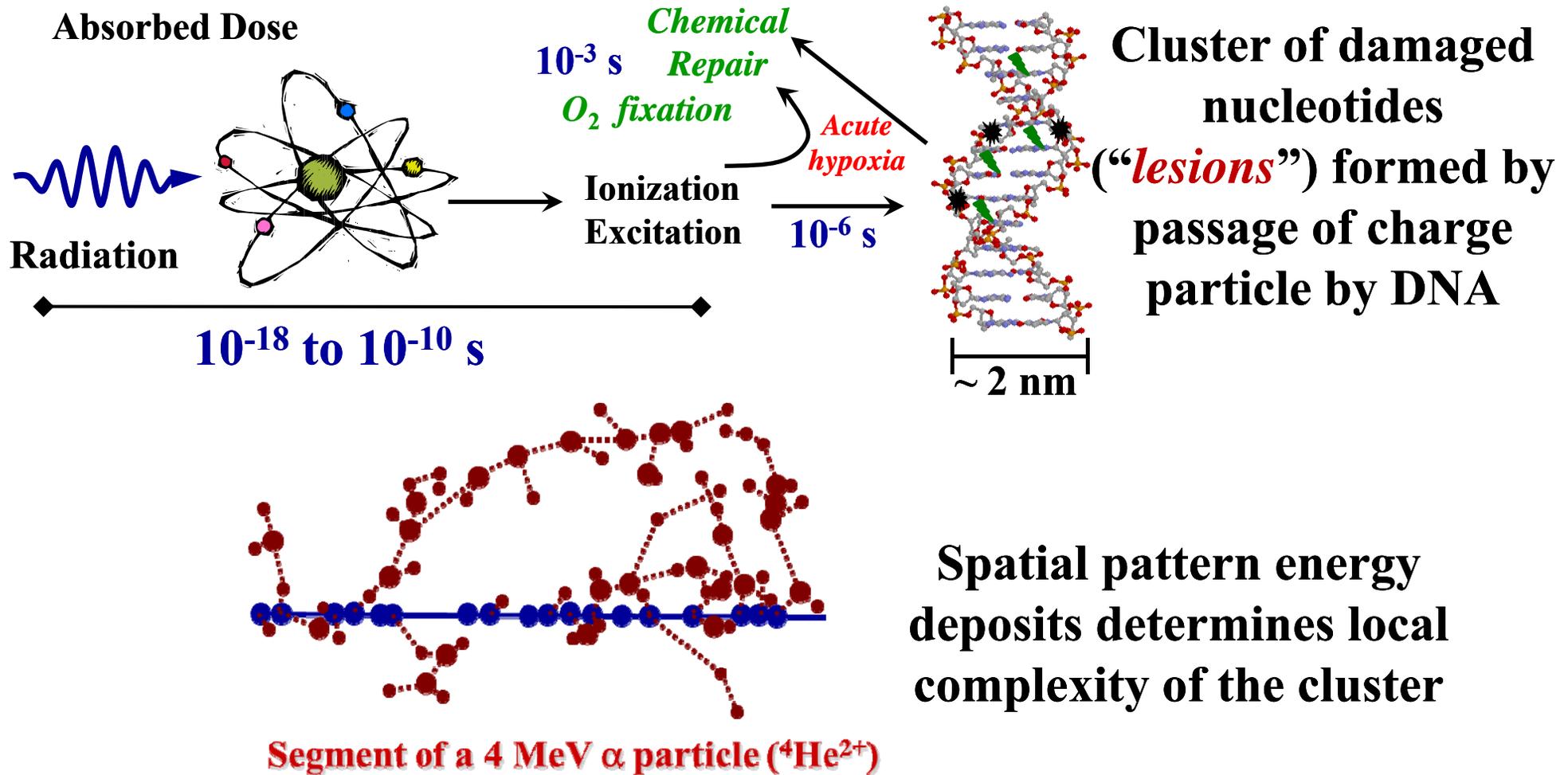


Structure of the tracks produced by particles with the same LET are not quite the same and can produce different biological effects

However if we “zoom out” to the macroscale (**> 0.1 to 1 mm**), the tracks of even very high LET particles look quite similar

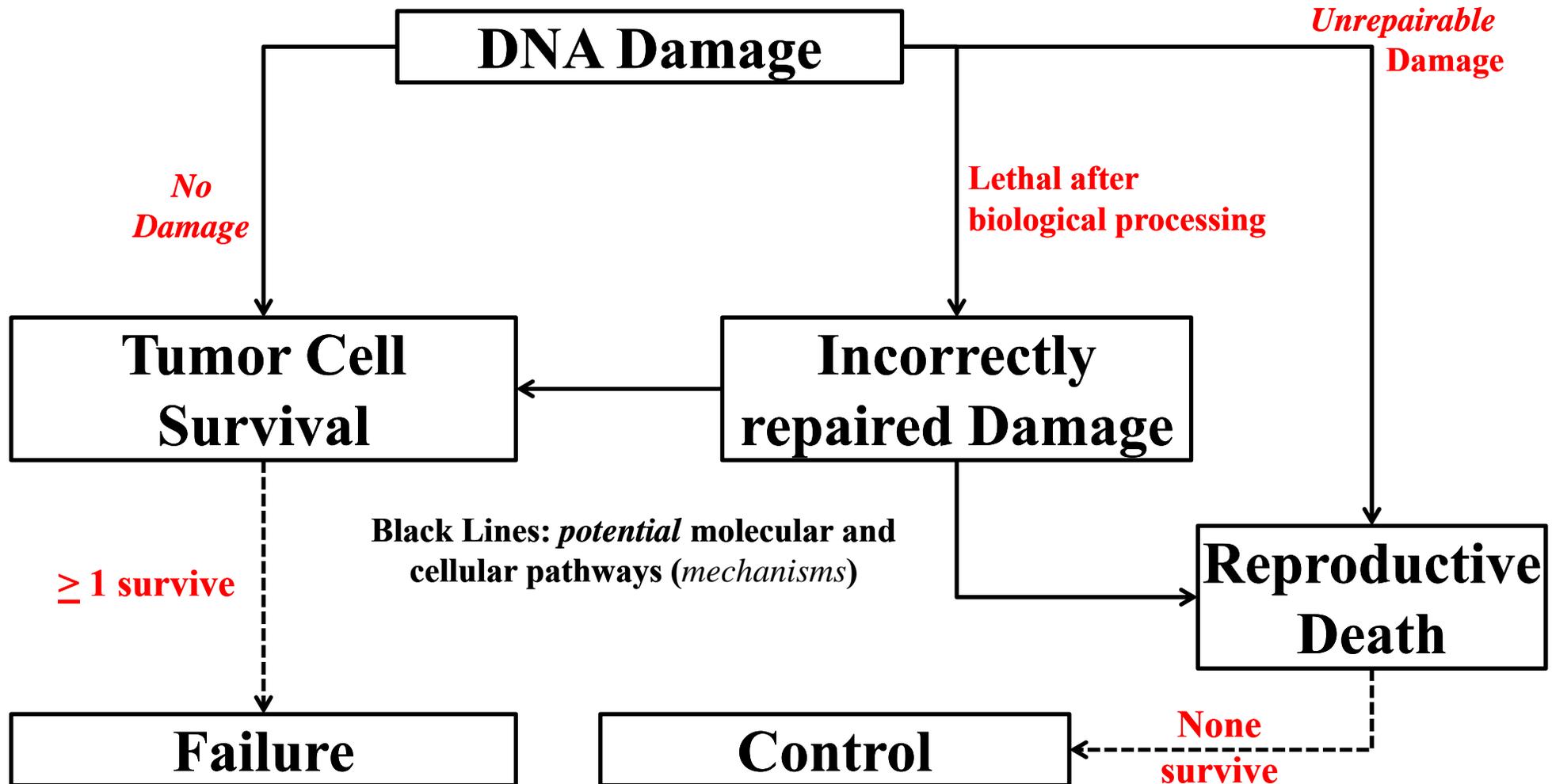
RBE effects must arise from the cellular and subcellular features of tracks – even for clinical endpoints!

Initial Damage to a Critical Molecule



Overall, a 1 Gy dose damages about 1 in 10^6 nucleotides.

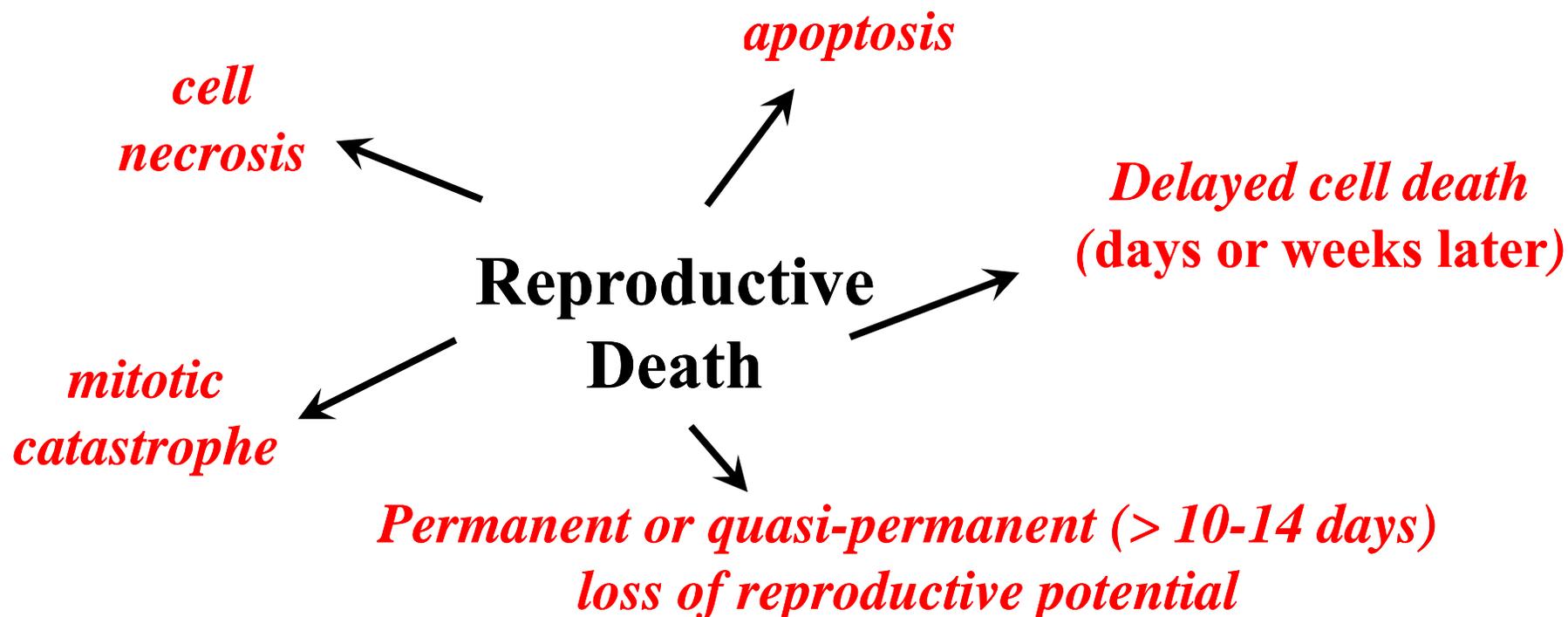
A Paradigm to Connect DNA Damage to Local Tumor Control



Black Dashed Lines: transition from cell to tissue-level biology

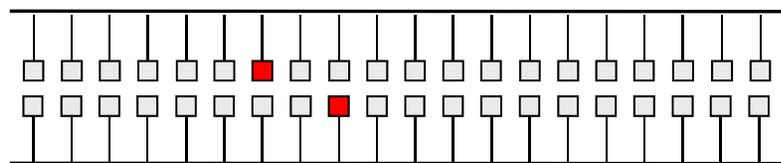
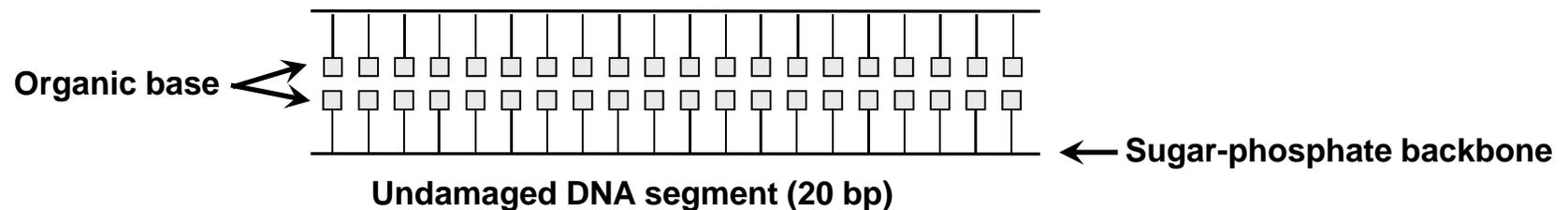
Reproductive Death?

Reproductive death is a general term that encompasses all modes of cell death, *including cells that remain metabolically active and intact but unable to divide...*

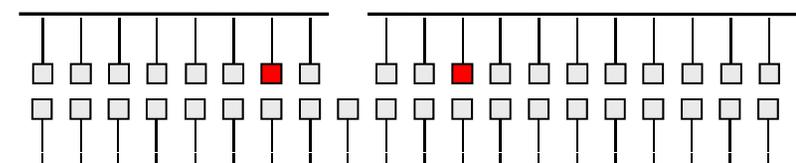


Clusters of DNA lesions

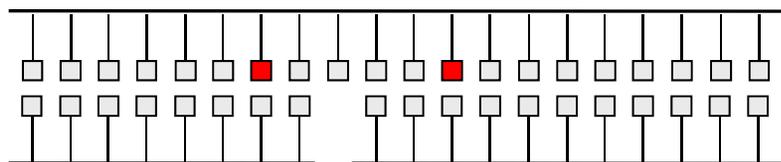
Groups of several DNA lesions within one or two turns of the DNA are termed a *cluster* or *multiply damaged site (MDS)**



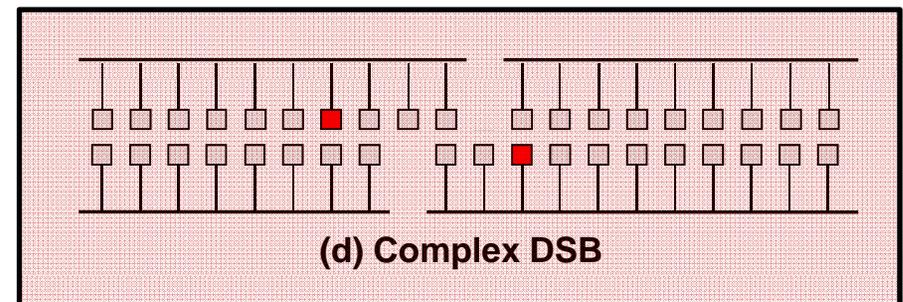
(a) Base damage in opposed strands



(c) complex SSB with adjacent base damage



(b) complex SSB with opposed base damage



(d) Complex DSB

Most critical category of DNA Damage

* Clustered lesions are also referred to as *locally multiply damaged sites (LMDS)*

Are all DSB Lethal? What about SSB?

After 1 Gy dose of low LET radiation, a typical human cell sustains **45 ± 10 DSB Gy⁻¹ cell⁻¹** and **1000 ± 200 SSB Gy⁻¹ cell⁻¹**. If all DSB are lethal, the fraction of cells that will survive a 2 Gy dose is

$$S = \exp(-45 \text{ DSB Gy}^{-1} \cdot 2 \text{ Gy}) \sim 10^{-40} \text{ (} 10^{-31}, 10^{-48} \text{)}$$

Only those cells that do not sustain a radiation-induced DSB survive
(Poisson distribution of DSB among irradiated cells)

For comparisons, many published studies indicate a surviving fraction of 0.1 (repair compromised) to 0.9 (*repair proficient*) cells after a 2 Gy dose of radiation. Only way to reconcile observations is

**< 2% of initial DSB formed
in a cell are lethal**

and/or

**< 0.1% of initial SSB formed
in a cell are lethal**

Cells are really good at repairing DNA damage, even DSB!

RBE for DSB induction

Σ = number of DSB Gy⁻¹ cell⁻¹
= slope of line

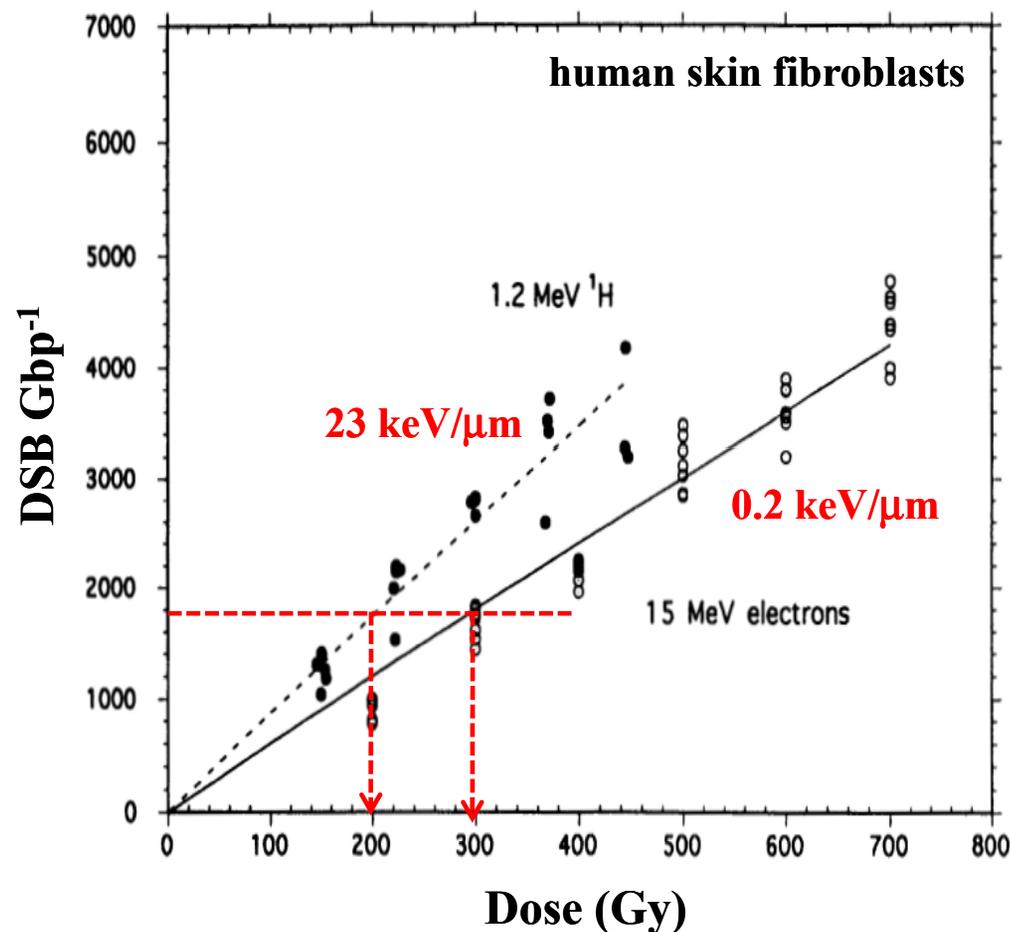
D_γ = dose of reference radiation

D_p = dose of proton

Want:

$$\text{Number DSB} = \Sigma_\gamma D_\gamma = \Sigma_p D_p$$

$$RBE_{DSB} \equiv \frac{D_\gamma}{D_p} = \frac{\Sigma_p}{\Sigma_\gamma} \cong 1.5$$



**RBE is an example of an
“isoeffect calculation”**

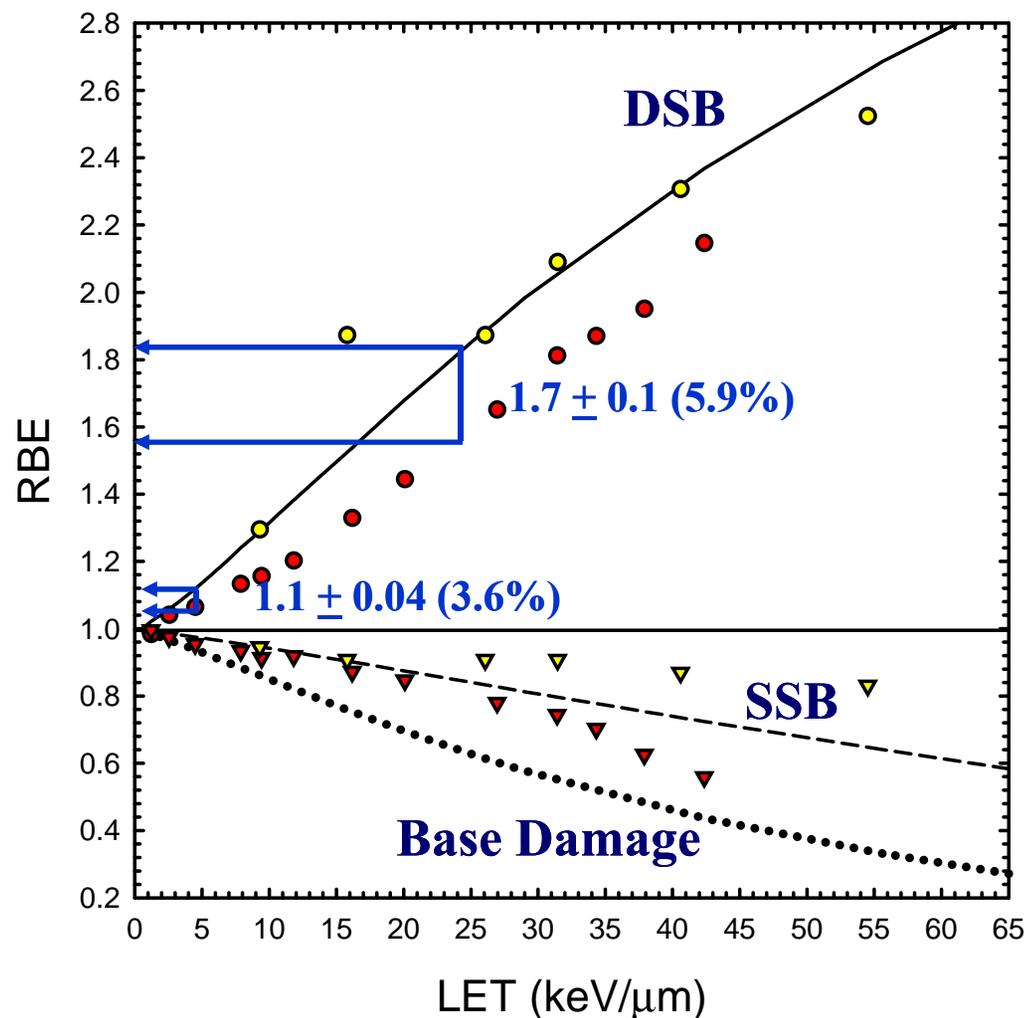
Trends in RBE_{DSB} with proton LET

Filled **Yellow** Symbols: *Track Structure Simulation* (Nikjoo *et al.* 1997, 2001, 2002)

Filled **Red** Symbols: *Track Structure Simulation* (Friedland *et al.* 2003)

Lines: *Monte Carlo Damage Simulation** (MCDS)

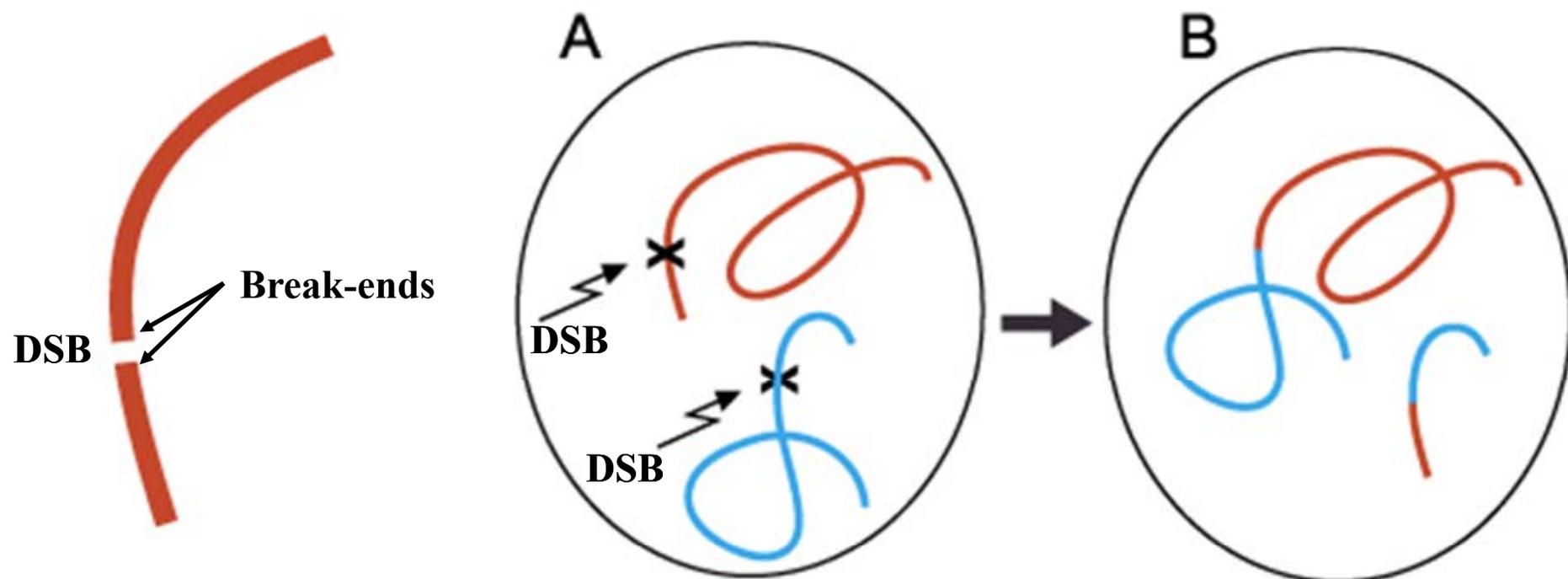
DSB are only category of DNA damage that increases with increasing particle LET (*additional evidence SSB less critical form of DNA damage than DSB*)



* Semenenko and Stewart 2004, 2006, Stewart *et al.* 2011

Why are DSB so effective at killing cells?

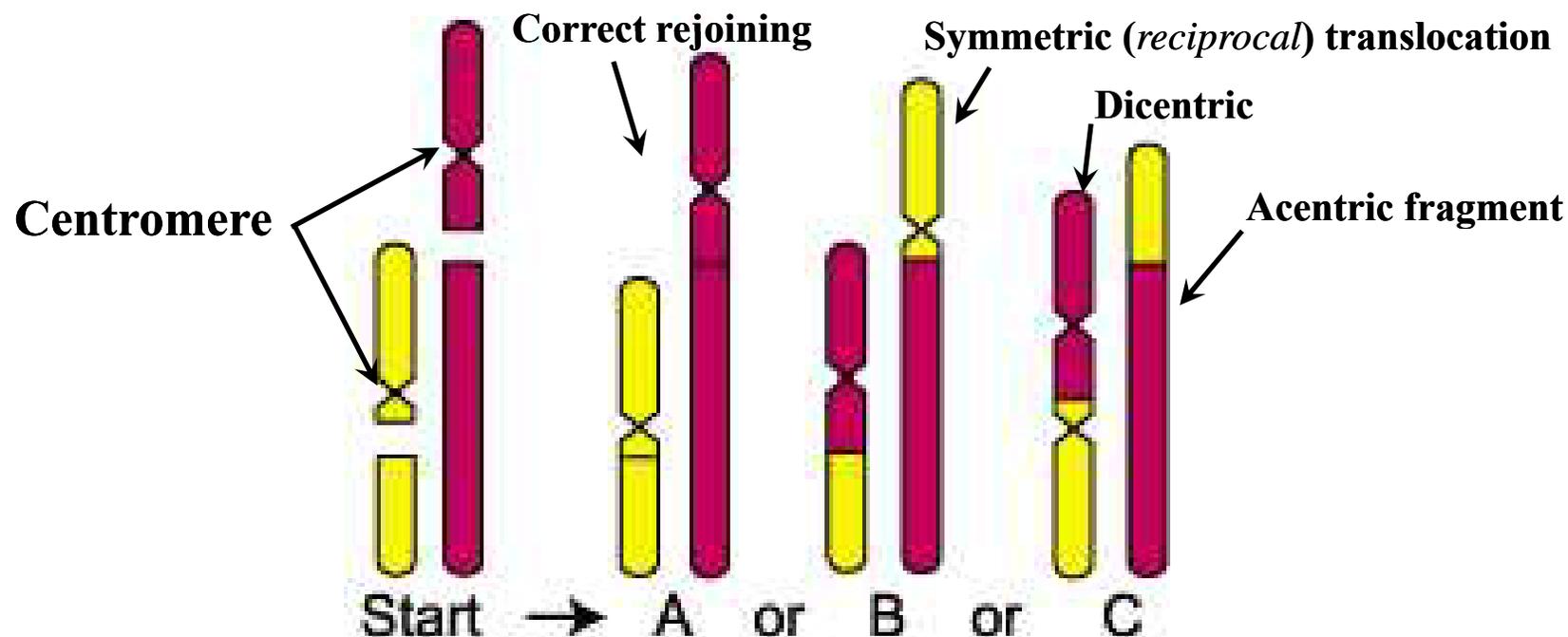
(Breakage and Rejoining Theory)



Break-ends associated with one DSB incorrectly rejoined to break-end associated with a different DSB

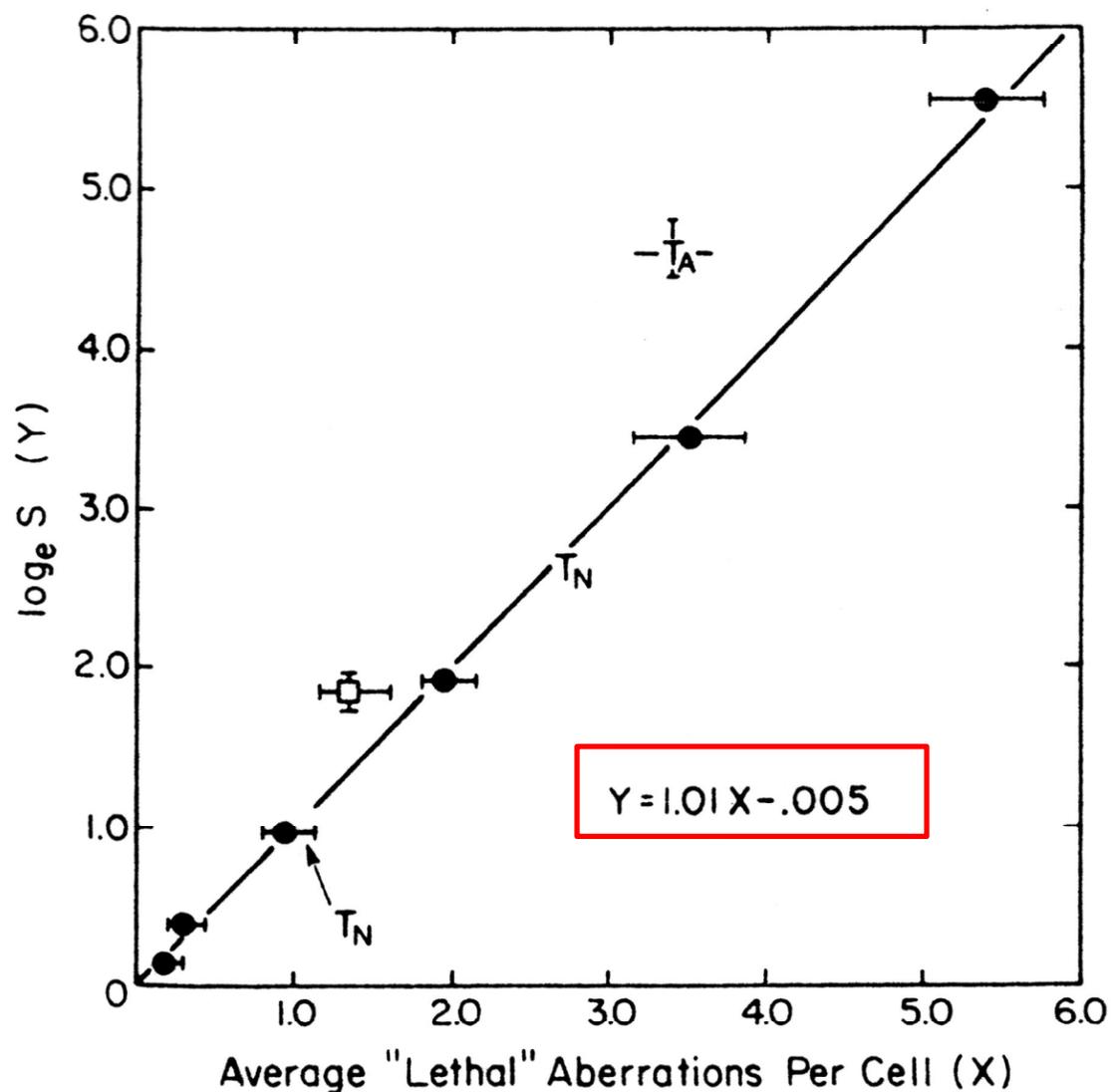
Proximity Effects: pairs of DSB formed in close spatial *and* temporal proximity are more likely to rejoin incorrectly than pairs of DSB separated in time and/or space (*dose rate and LET effects*)

Lethal and Non-Lethal Aberrations



Dicentrics and acentric fragments are usually lethal in the reproductive sense because segregation of chromosomes at mitosis is disturbed. In contrast, correct DSB rejoining and symmetric (*reciprocal*) translocations are consistent with continued cell division

Is there a 1:1 relationship?



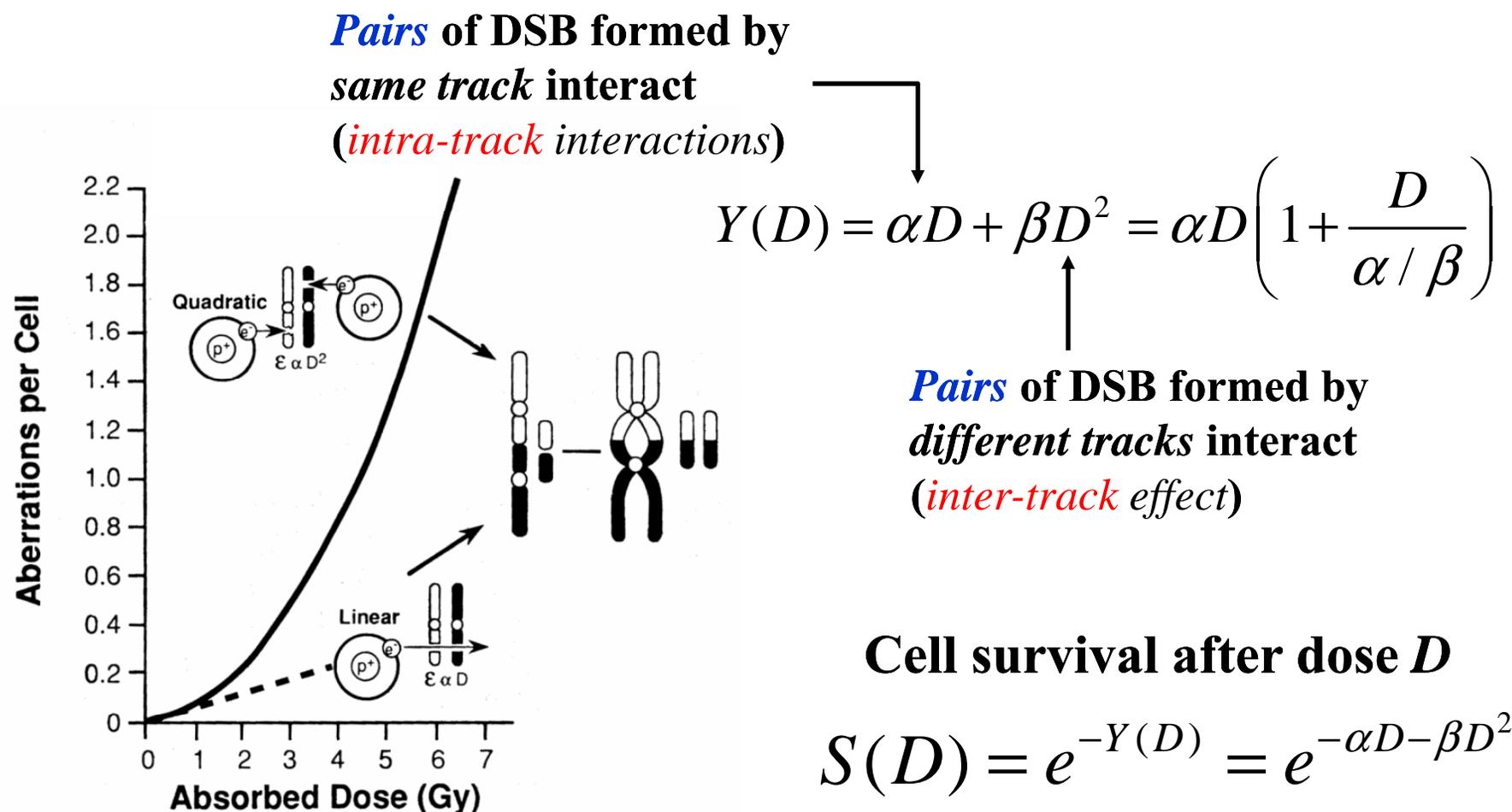
AC 1522 normal human fibroblasts irradiated by x-rays

$$S = e^{-Y}$$

S = fraction that survive

Y = avg number of lethal aberrations per cell

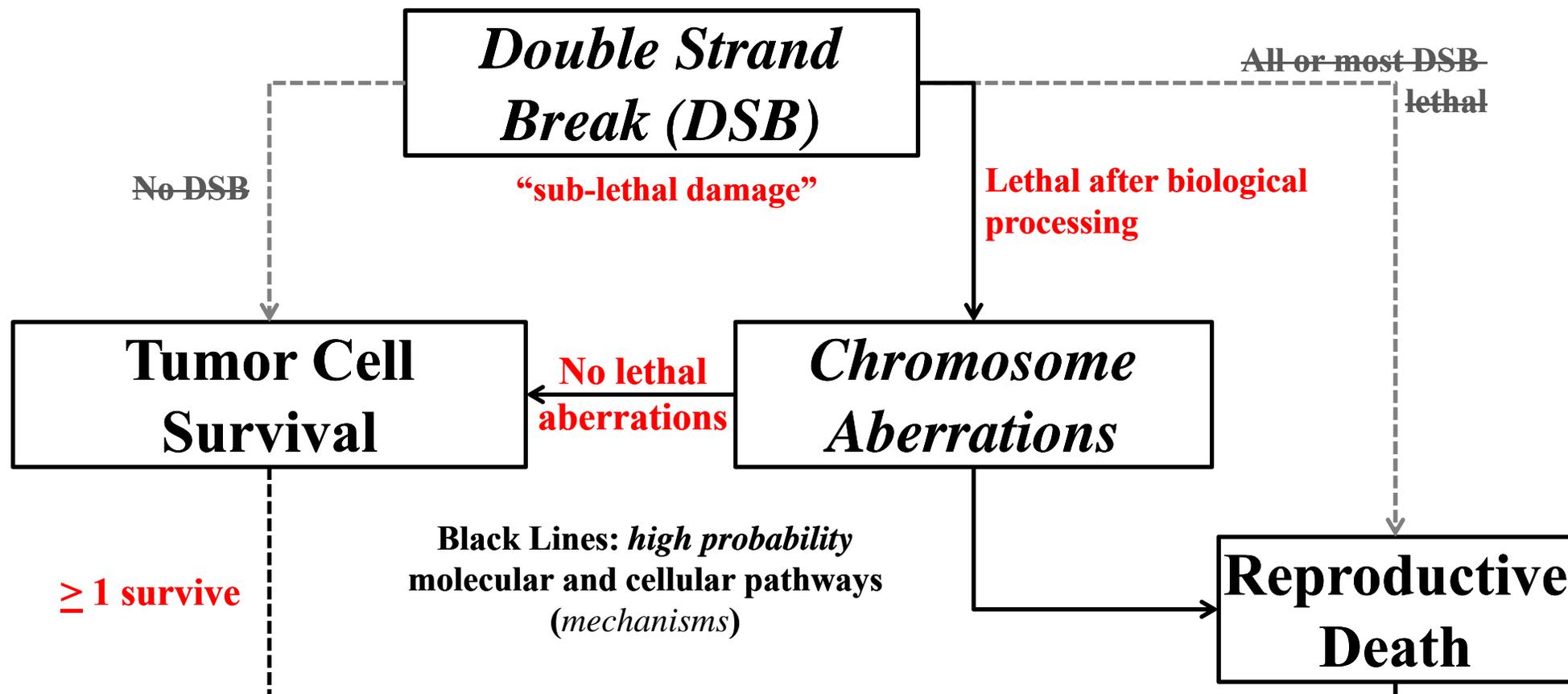
Linear-Quadratic (LQ) Model for Cell Survival



Only those cells without a lethal aberration in their DNA retain the ability to divide and produce viable progeny (“reproductive survival”).

Connecting DSB to Local Tumor Control

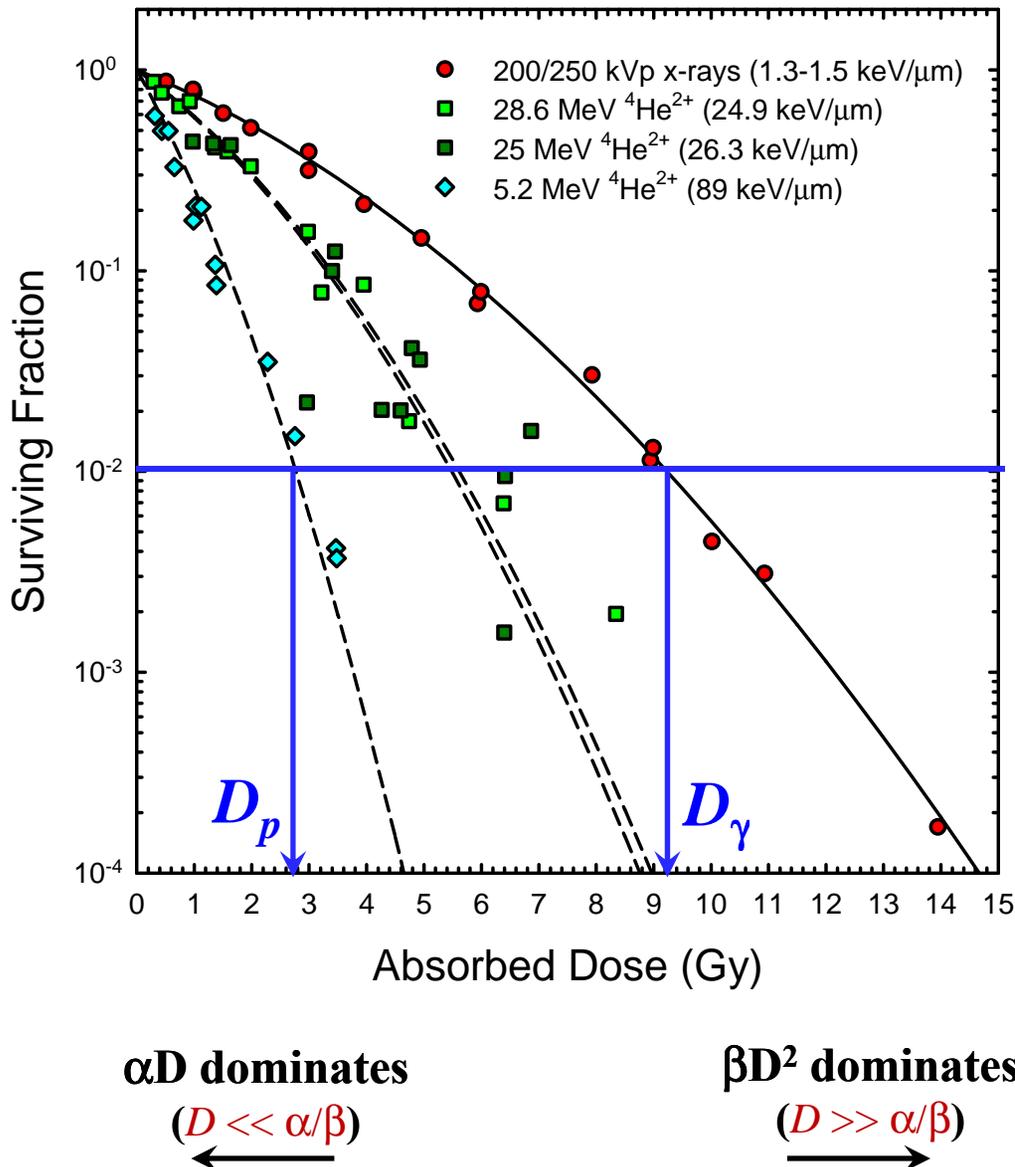
Grey Dashed Lines: *low probability* molecular and cellular pathways (*mechanisms*)



Are trends in the RBE for DSB induction qualitatively and quantitatively similar to the RBE for cell survival?

Black Dashed Lines: transition from cell to tissue-level biology

Low and High Dose RBE (*cell survival*)



RBE for a specific dose (*cell survival level*)

$$RBE = \frac{D_\gamma}{D_p} \cong \frac{9.2 \text{ Gy}}{2.8 \text{ Gy}} = 3.3 \text{ (1\% survival)}$$

Low Dose RBE: $-\ln S \cong (\alpha D)_\gamma = (\alpha D)_p$

$$\text{low dose } RBE_{SF} = \frac{D_\gamma}{D_p} = \frac{\alpha_p}{\alpha_\gamma}$$

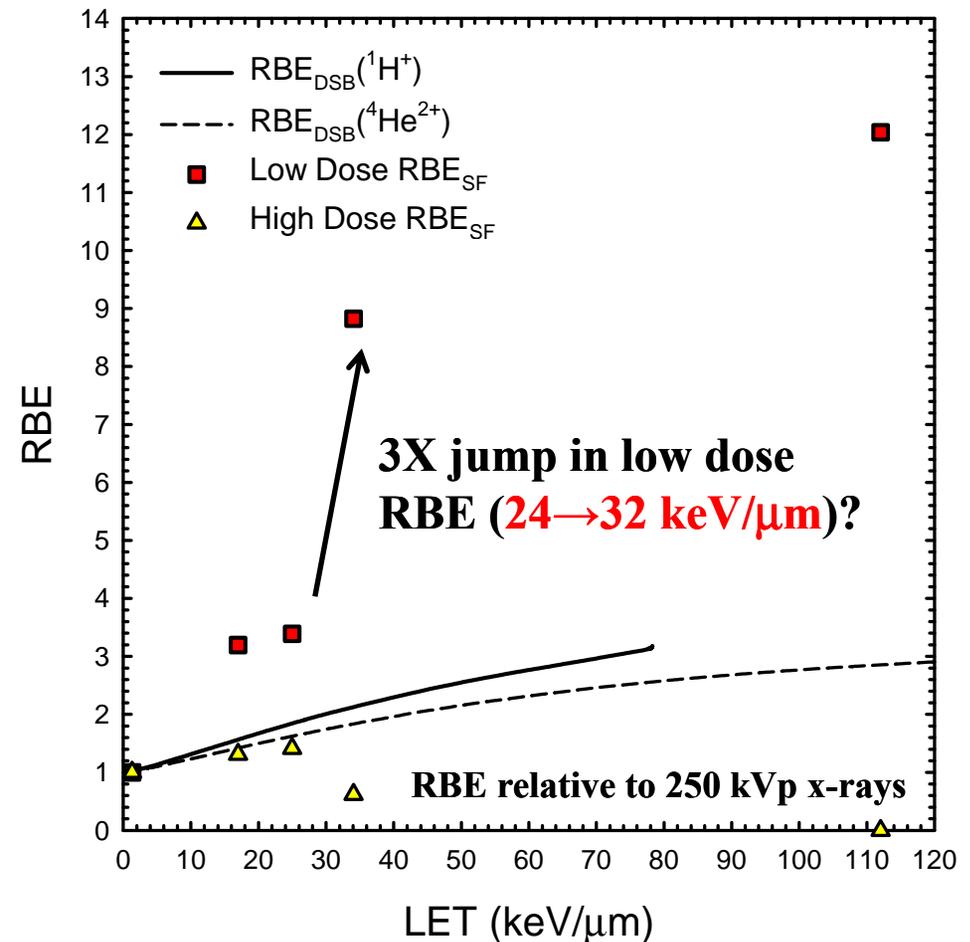
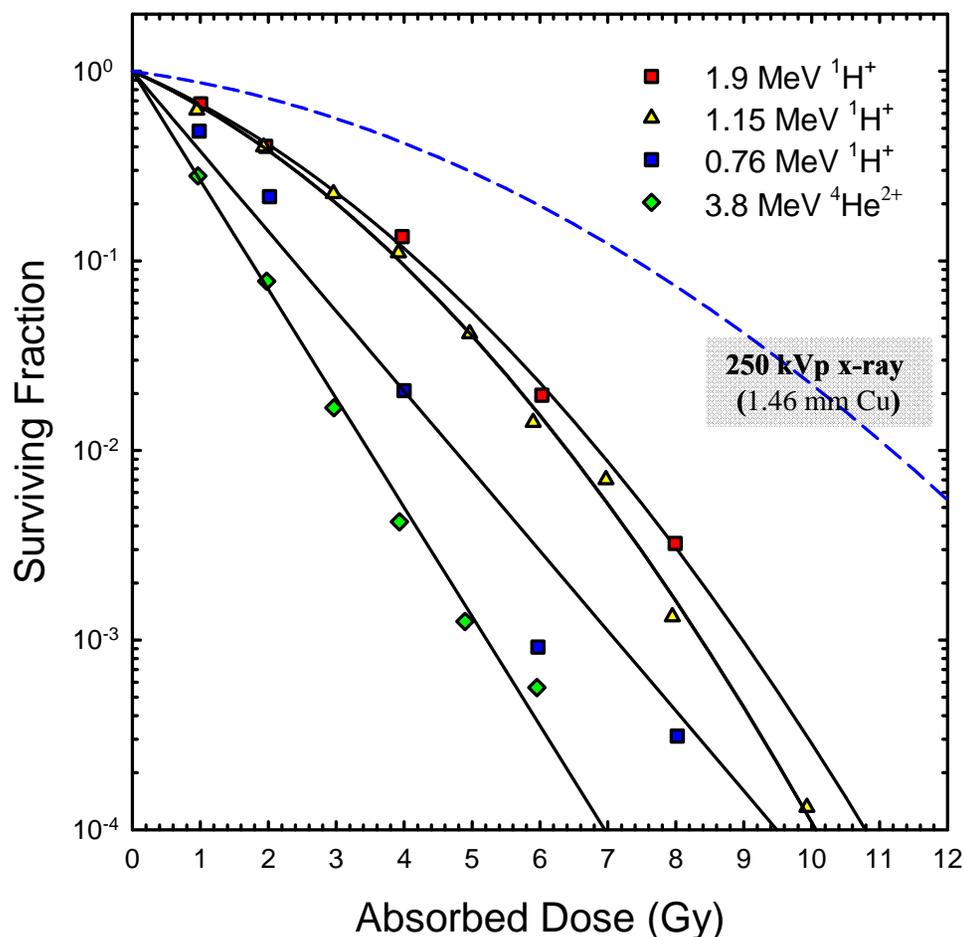
“ RBE_{\max} ”

High Dose RBE: $-\ln S \cong (\beta D^2)_\gamma = (\beta D^2)_p$

$$\text{high dose } RBE_{SF} = \frac{D_\gamma}{D_p} = \sqrt{\frac{\beta_p}{\beta_\gamma}}$$

“ RBE_{\min} ”

Is RBE_{DSB} predictive of RBE_{SF} ?



Little if any evidence RBE_{SF} ($^1\text{H}^+$ and $^4\text{He}^{2+}$) is related to RBE_{DSB} , or so it seems...

A Mechanistic Model for α and α/β

The Repair-Misrepair-Rixation (RMF) model (*Carlson et al. 2008*) predicts, in the limit when the D is small compared to α/β , that

$$\alpha = \theta \Sigma + \kappa \bar{z}_F \Sigma^2 \quad \beta = \frac{\kappa}{2} \Sigma^2 \quad \frac{\alpha}{\beta} = \frac{2}{\Sigma} (\theta / \kappa) + 2 \bar{z}_F$$

Intra-track chromosomal aberrations Inter-track aberrations

Unrepairable and misrepaired

θ , κ are *adjustable cell- or tissue-specific* parameters related to biological processing of DNA damage (*independent of LET and O_2 concentration*)

Σ is the number of DSB $\text{Gy}^{-1} \text{Gbp}^{-1}$ (or per cell); estimate using the MCDS (*strong function of LET and O_2 concentration*)

\bar{z}_F is the frequency-mean specific energy (in Gy) delivered to the cell nucleus (*strong function of LET but independent of O_2 concentration*) – estimate with the MCDS or other Monte Carlo code(s)

How is RBE_{DSB} related to RBE_{SF} ?

With the RMF-motivated formulas for α and β , the low and high dose RBE_{SF} is

$$\alpha = \theta \Sigma + \kappa \bar{z}_F \Sigma^2 \quad \beta = \frac{\kappa}{2} \Sigma^2 \quad \text{DSB Gy}^{-1} \text{ Gbp}^{-1}$$

“ RBE_{min} ” high dose $RBE_{SF} = \sqrt{\frac{\beta_p}{\beta_\gamma}} = RBE_{DSB}$

“ RBE_{max} ” low dose $RBE_{SF} = \frac{\alpha_p}{\alpha_\gamma} \cong RBE_{dsb} \left\{ 1 + RBE_{dsb} \frac{\bar{z}_F \Sigma_\gamma}{\theta / \kappa} \right\} \geq RBE_{dsb}$

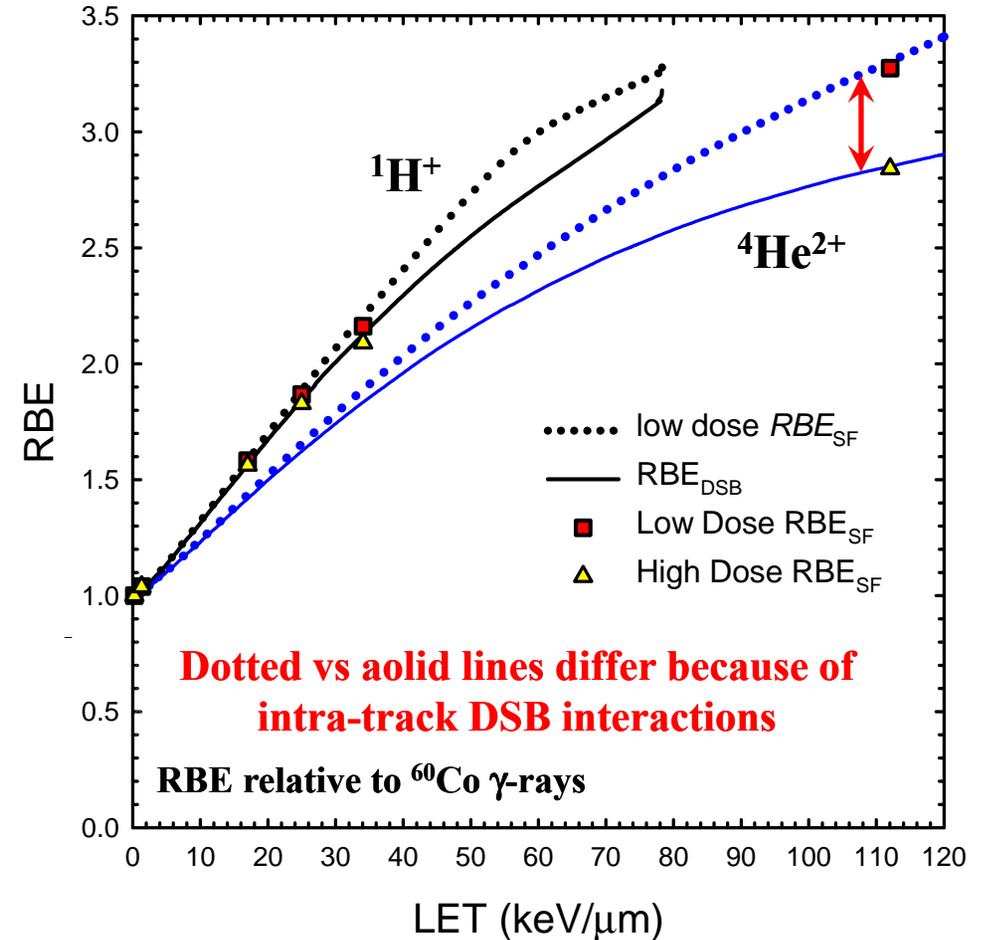
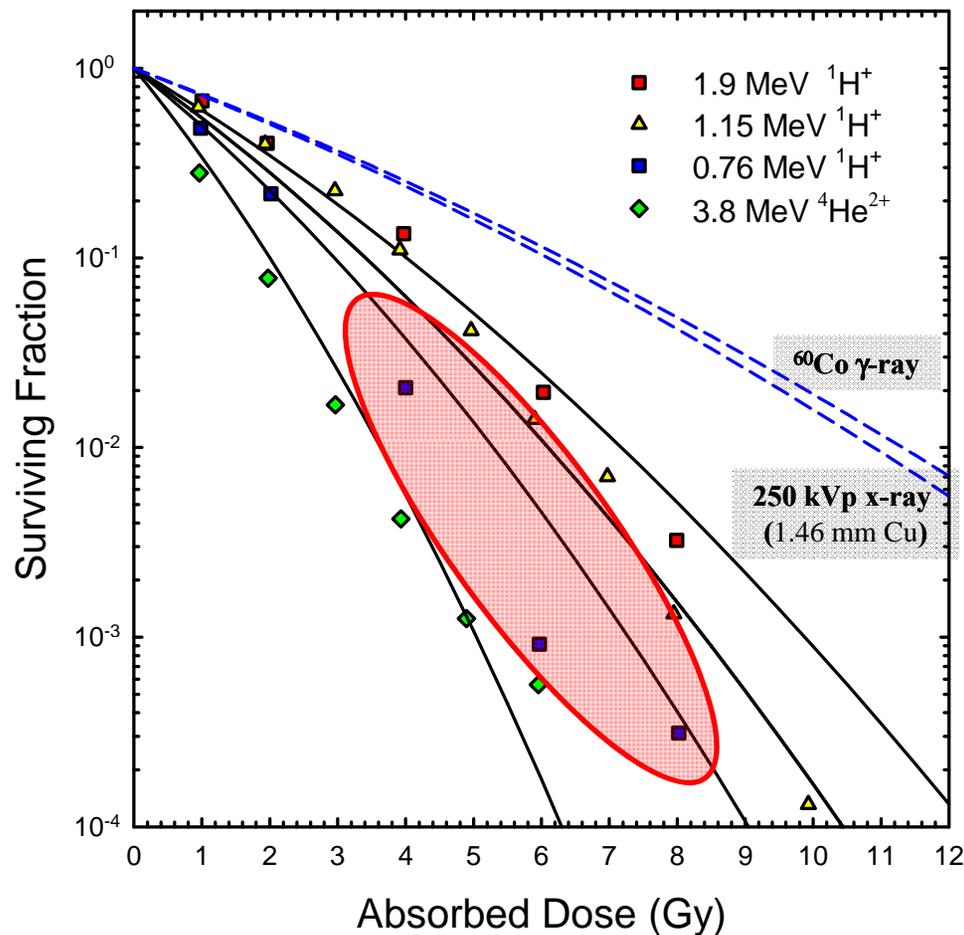
D is “small” compared to α/β

Intra-track DSB interactions increase with increasing LET because of proximity effects

$$\frac{\bar{z}_F \Sigma_\gamma}{\theta / \kappa} \propto \frac{\Sigma_\gamma}{\theta / \kappa} \cdot LET$$

DSB Gy⁻¹ Gbp⁻¹
reference radiation

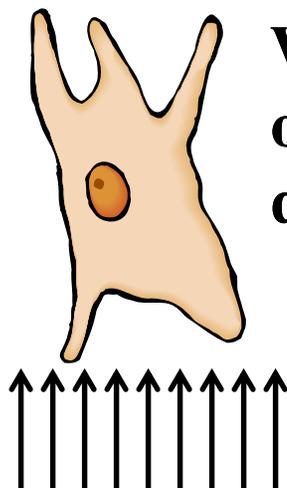
Is RBE_{DSB} predictive of RBE_{SF} ? *Version 2.0*



Reasonable fit to cell survival data for all energies.

Low dose $RBE_{SF} \geq RBE_{DSB}$

Dosimetry of Short-Range Particles is Tricky...



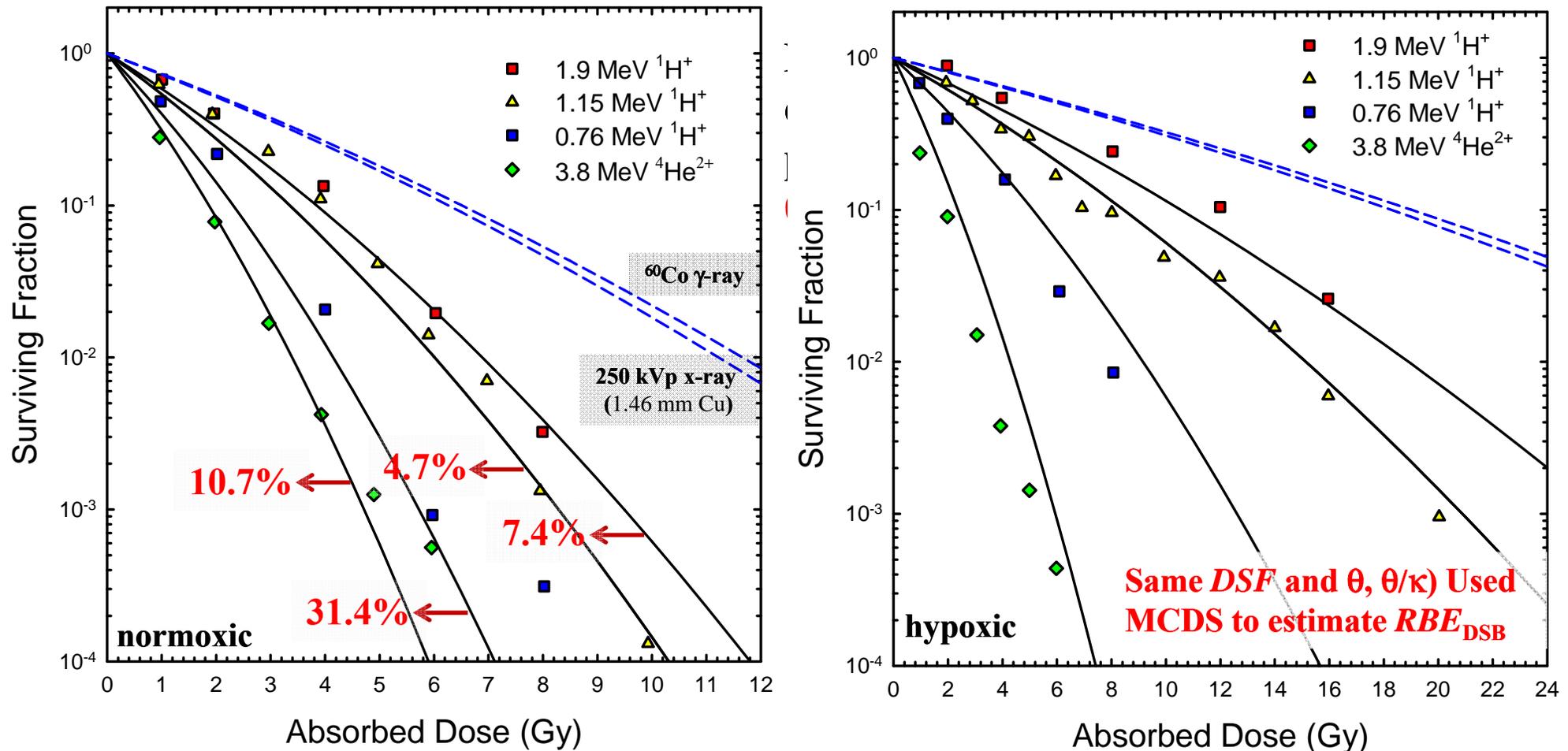
When the CSDA range of a charge particle is of the same order of magnitude as the dimensions of the biological target, dosimetry needs to be corrected for

- **Change in stopping power within target**
- **Energy and path length straggling**
- **Finite particle range (“stoppers”), energy and angular distribution of particles incident on target**

For a monoenergetic particle incident on a 5 μm target

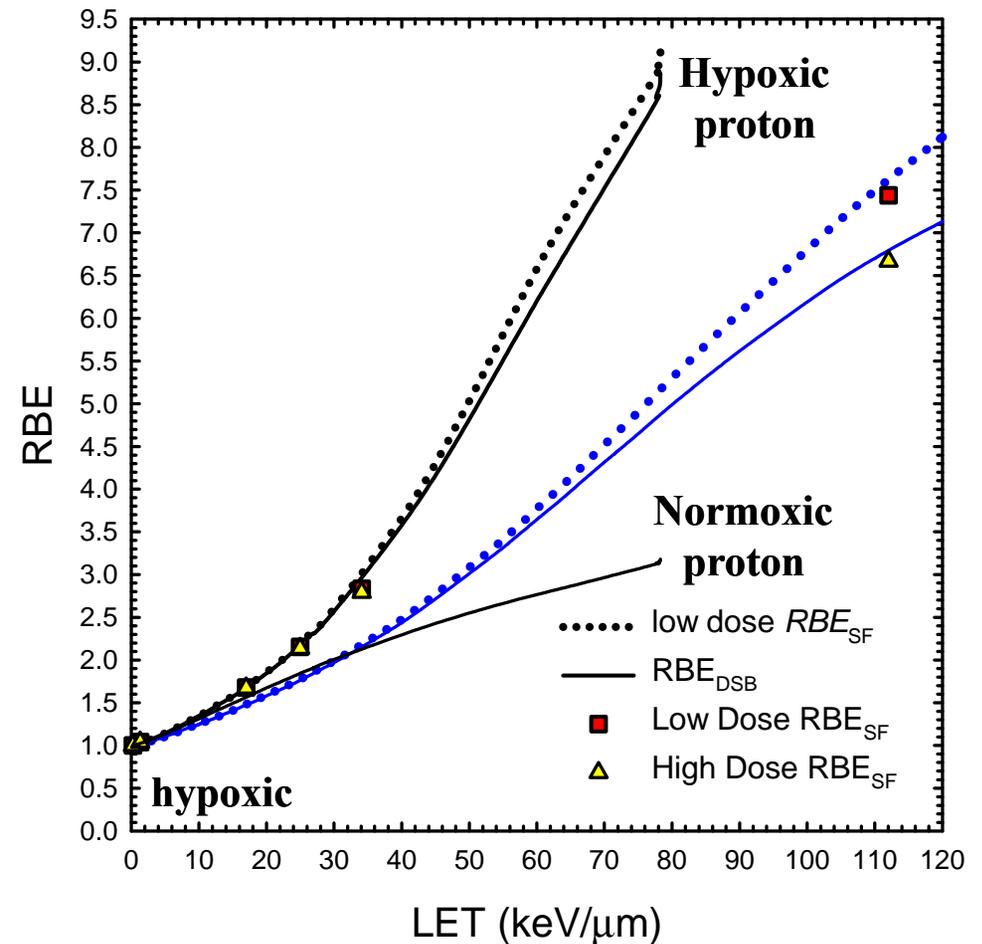
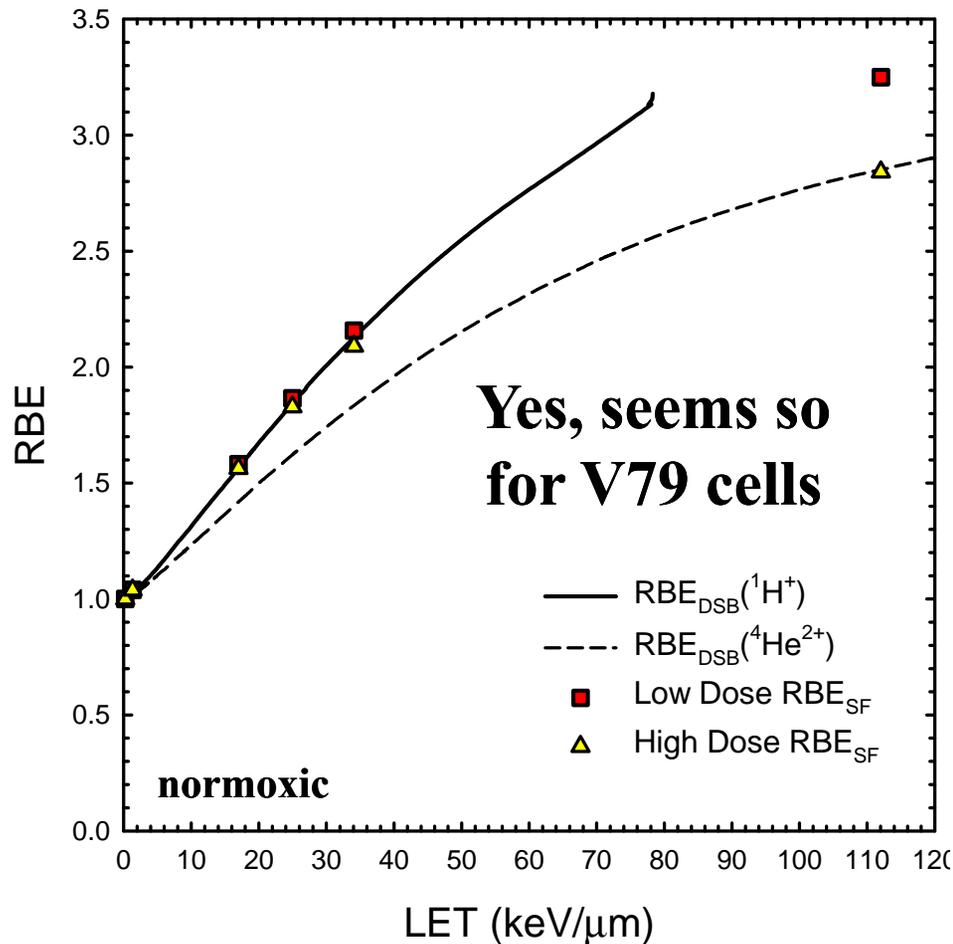
Particle	Range (μm)	LET (keV/ μm)			D/ Φ (nGy-cm ²)		
		Reported	Entrance	Exit	Entrance	Avg. over Target	% difference
1.9 MeV $^1\text{H}^+$	67.7	17.0	16.8	17.4	26.9	27.3	1.30
1.15 MeV $^1\text{H}^+$	29.9	24.0	24.4	26.5	39.1	40.3	3.06
0.76 MeV $^1\text{H}^+$	15.9	32.0	32.5	38.6	52.1	55.3	6.12
3.8 MeV $^4\text{He}^{2+}$	25.3	110.0	108.7	120.9	174.2	180.9	3.89

Fit with “Corrected” Dosimetry



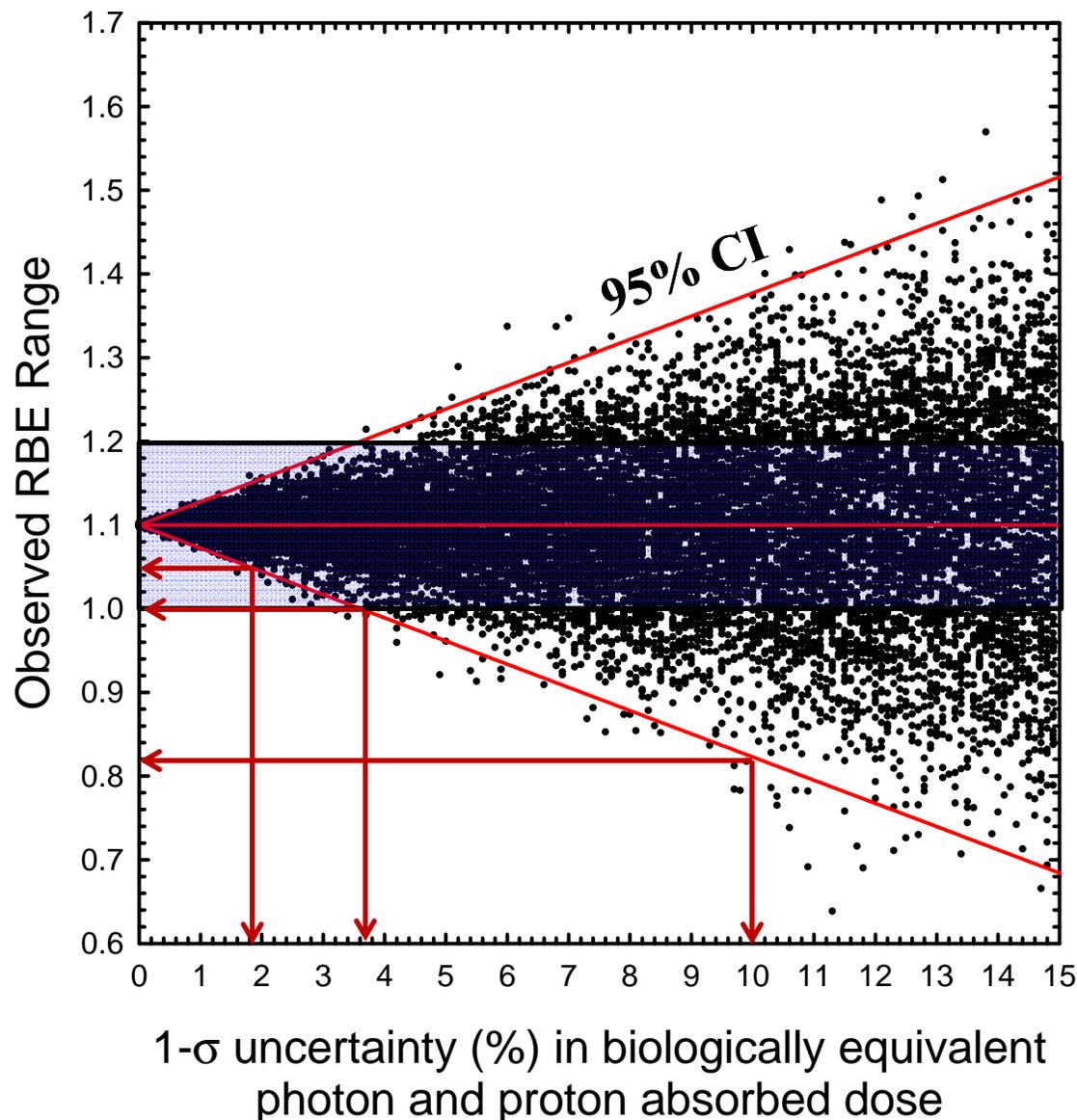
Improved fit to measured data with small (*quite plausible*) changes in the mean particle energy (**< 10 μm shift**)

Is RBE_{DSB} predictive of RBE_{SF} ? *Version 2.1*



For protons with an LET ≤ 20 keV/ μ m (≥ 2 MeV), RBE is about the same in cells irradiated under normoxic and anoxic conditions (no change in OER from ^{60}Co γ -rays).

Impact of Uncertainties on “observed” RBE



RBE is ratio of doses that produce same biological effect

$$RBE = \frac{D_{\gamma} \pm \sigma_{\gamma}}{D_p \pm \sigma_p}$$

RBE 1.1 ± 0.1 (blue shaded region)

1.8% uncertainty in equivalent physical dose: RBE = 1.1 ± 0.05

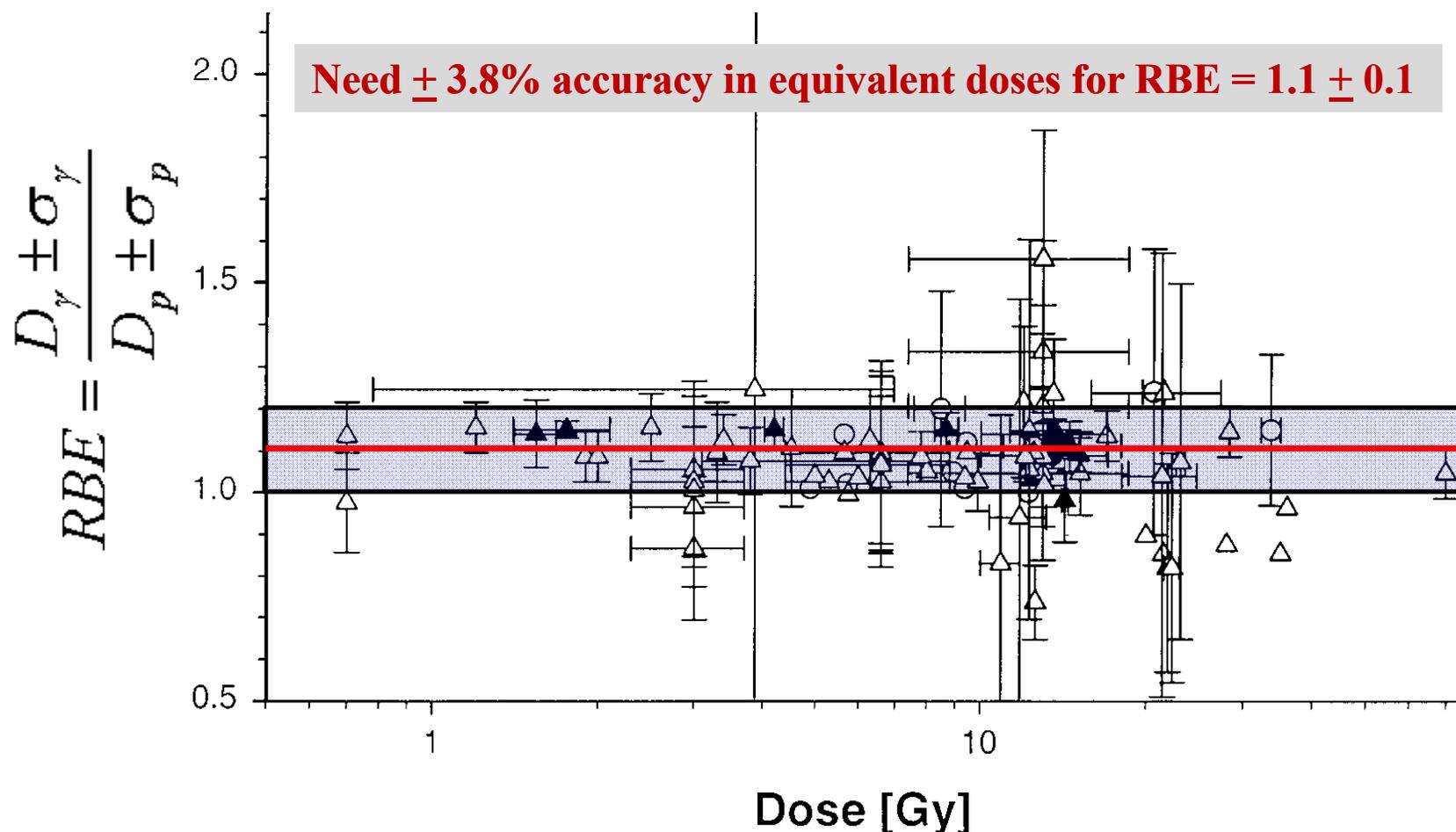
3.8% uncertainty in equivalent physical dose: RBE = 1.1 ± 0.1

10% uncertainty in equivalent physical dose: RBE = 1.1 ± 0.3

Do we just need more accurate dosimetry

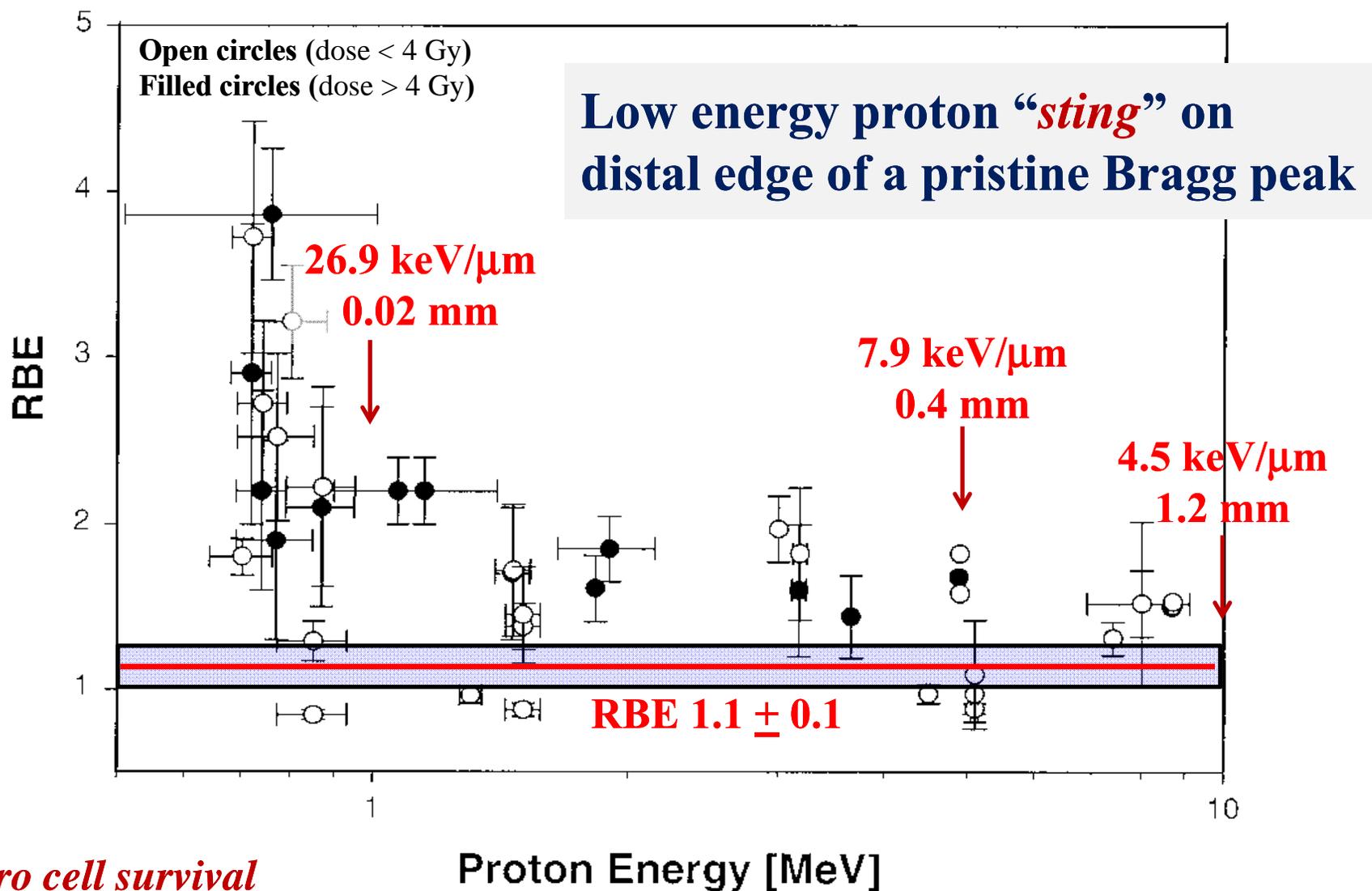
***and* better dose-response models
(e.g., RMF model)?**

in vivo studies



Adapted from Figure 2 in Paganetti, Niemierko, Ancukiewicz, Gerweck, Goitein, Loeffler, and Suit, Relative Biological Effectiveness (RBE) Values for Proton Beam Therapy, IJROBP 53(2) 407-421 (2002).

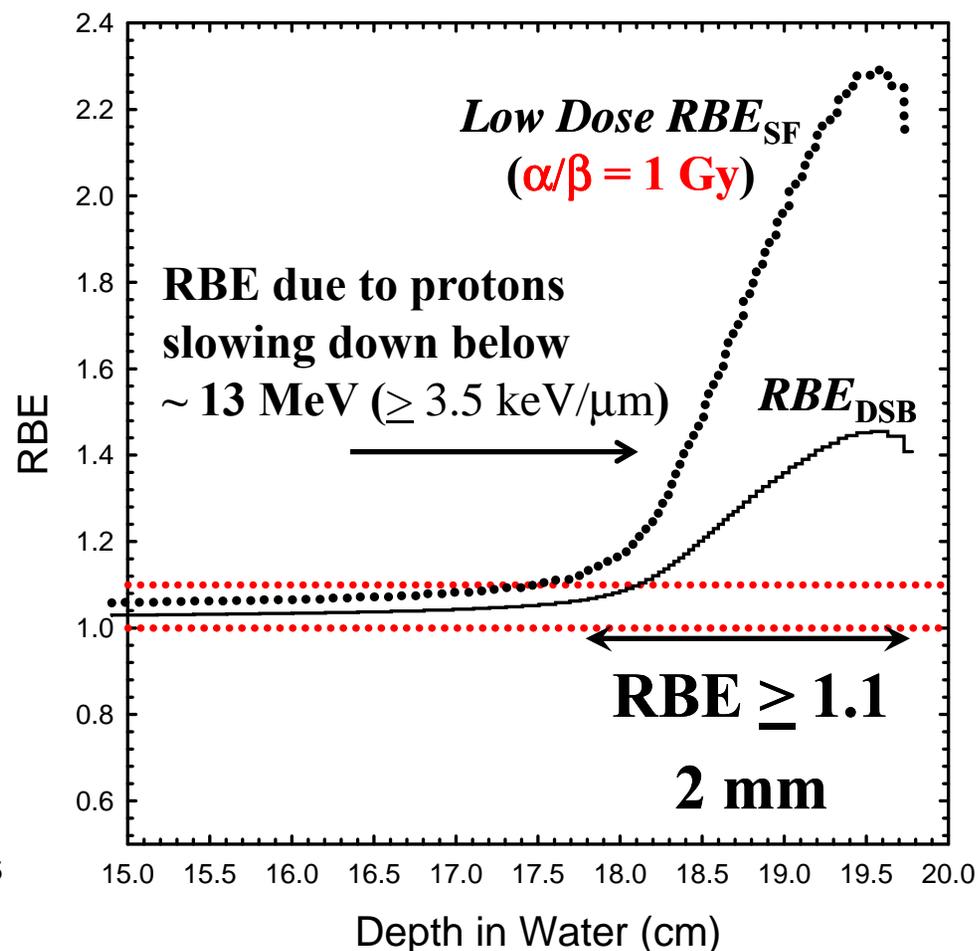
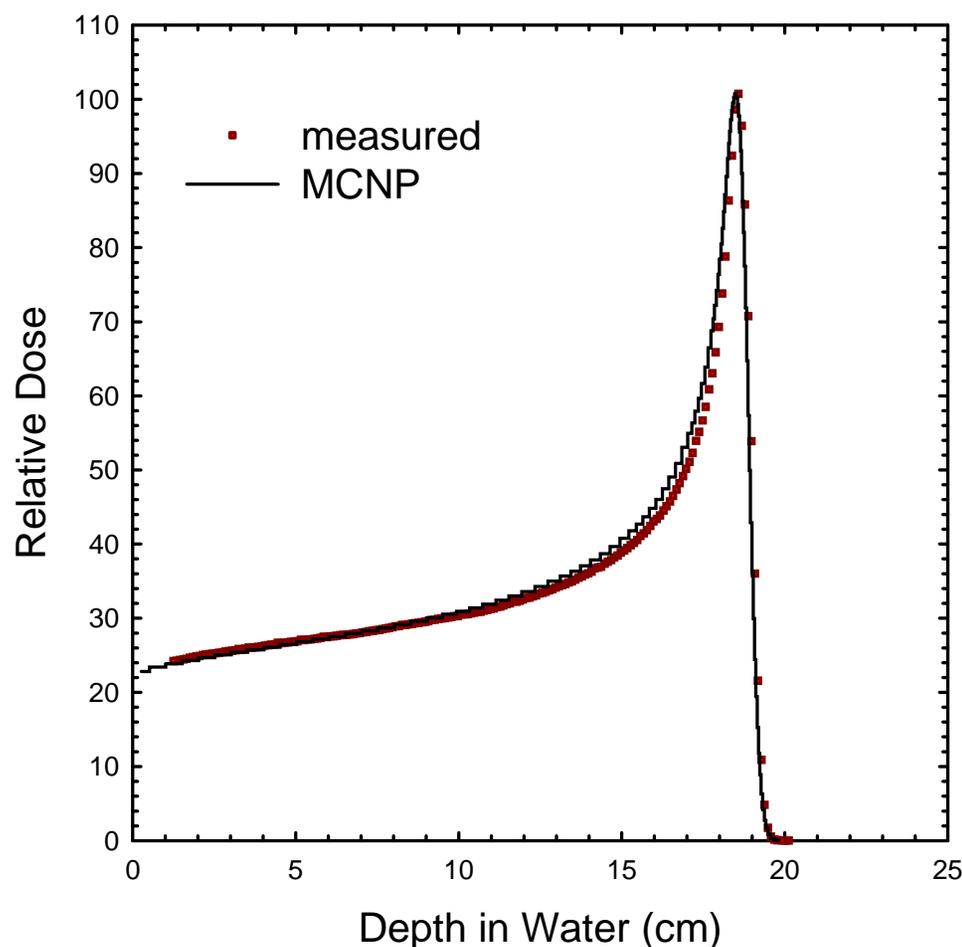
Strong evidence for spatial (*and LET*) variations in proton RBE despite uncertainties ...



Adapted from Figure 3 in Paganetti, Niemierko, Ancukiewicz, Gerweck, Goitein, Loeffler, and Suit, Relative Biological Effectiveness (RBE) Values for Proton Beam Therapy, IJROBP 53(2) 407-421 (2002).

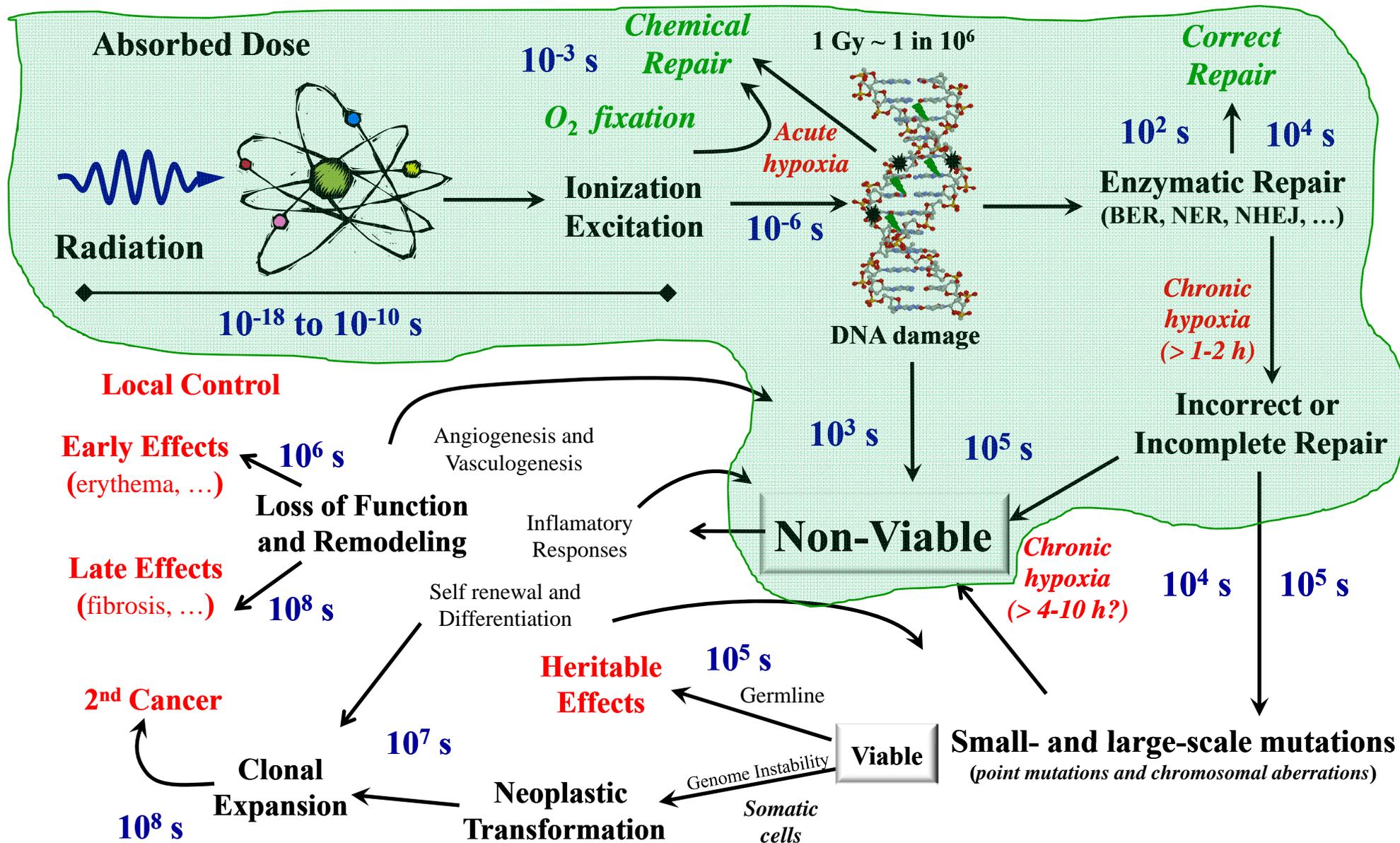
RBE effects in a 163 MeV pencil beam

Tuned MCNP 6.1 model of 163.25 MeV pencil beam to match measured depth-dose profile (SCCA proton facility, Seattle, WA).

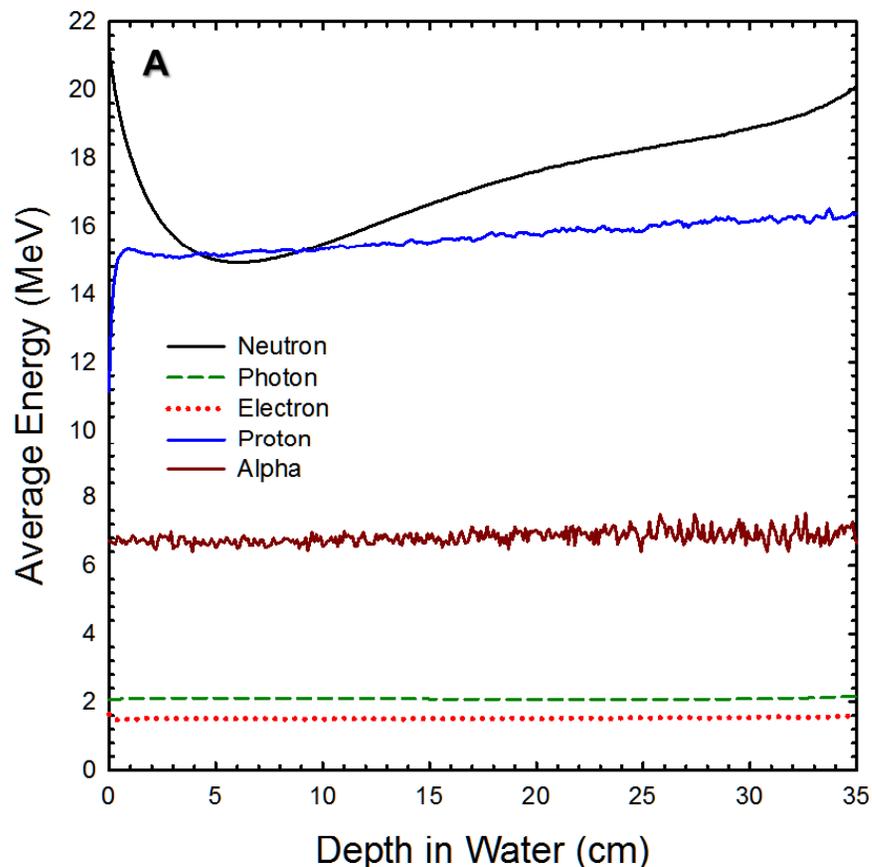


* Really easy way to generate dose-averaged RBE in MCNP. See supplemental slides.

Proton RBE for Healthy Organs and Tissues?



UW Experience with Fast Neutrons



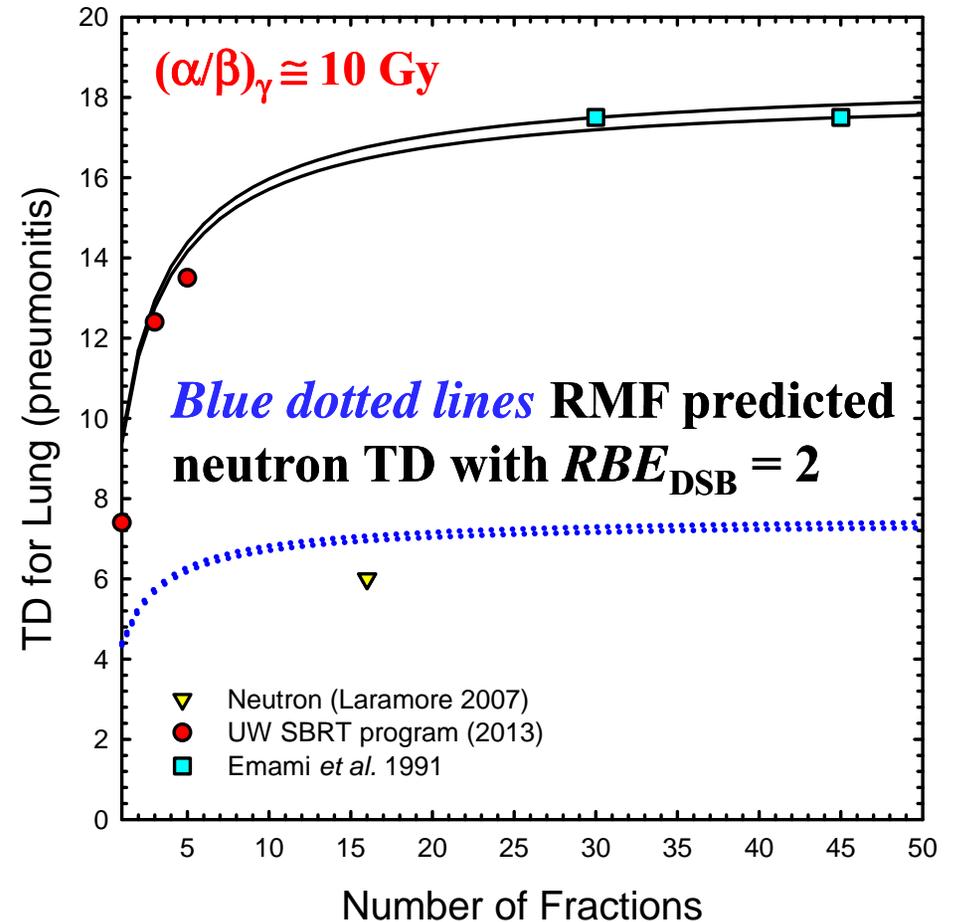
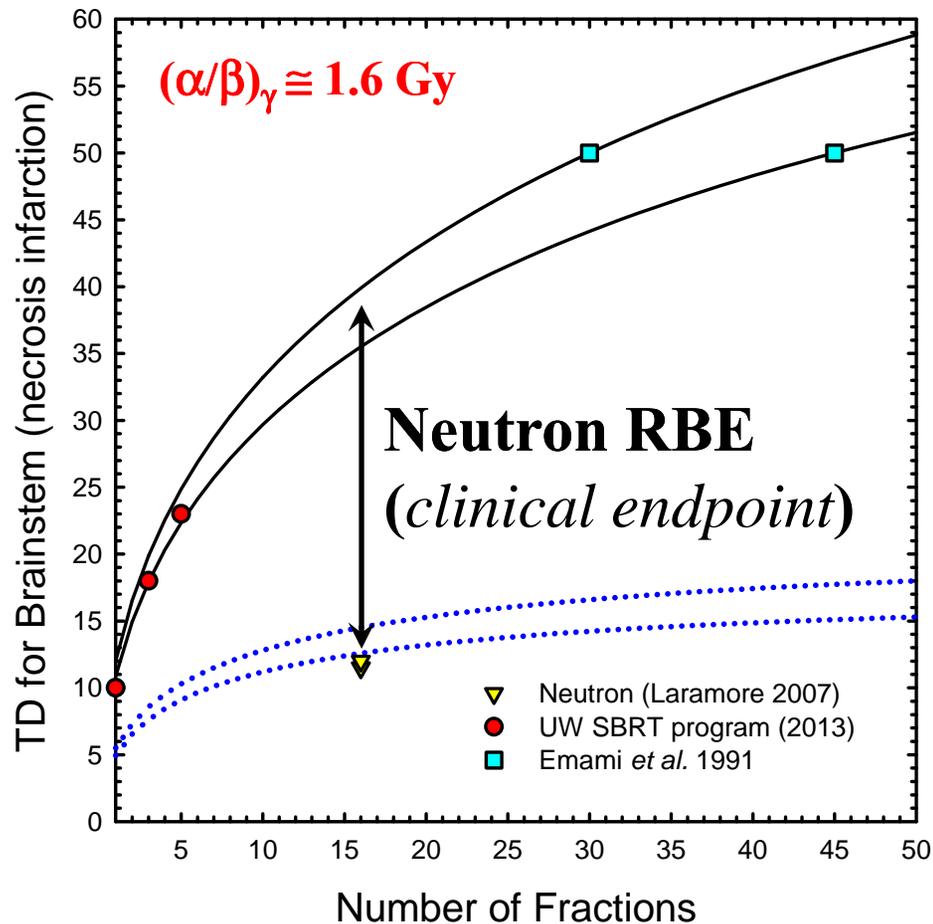
80-90% of absorbed dose to patient is from lower energy protons ($E_{\text{avg}} \cong 16 \text{ MeV}$)

Tolerance doses derived from over 25+ years of clinical experience

Used as a guide for tolerance doses in carbon ion therapy

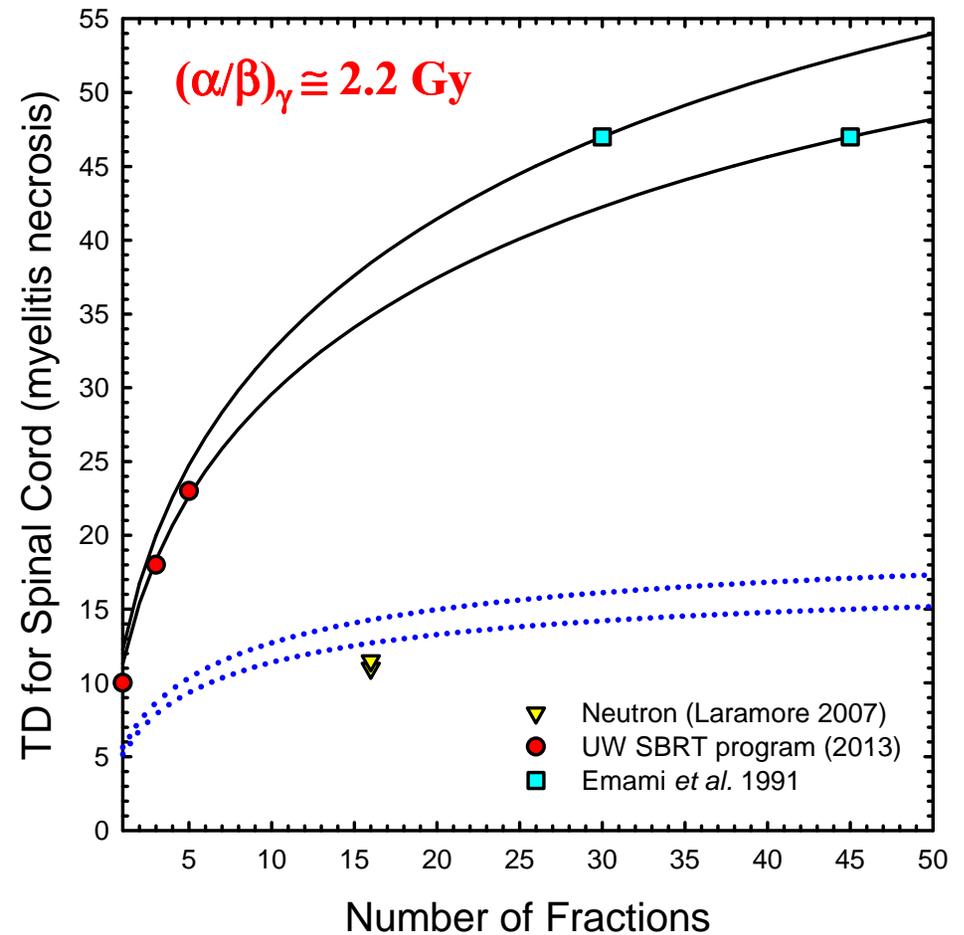
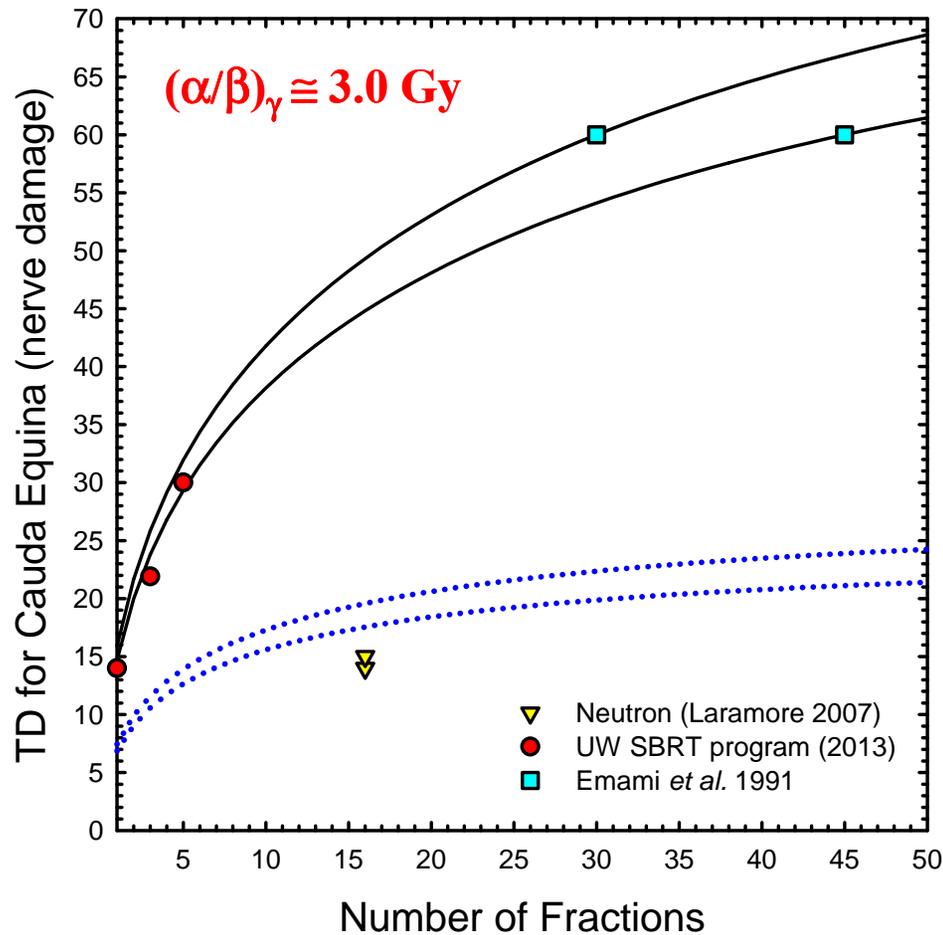
What can fast neutron therapy tell us about RBE effects in a proton Bragg peak?

Neutron TD5/5 Dose (*Brainstem and Lung*)

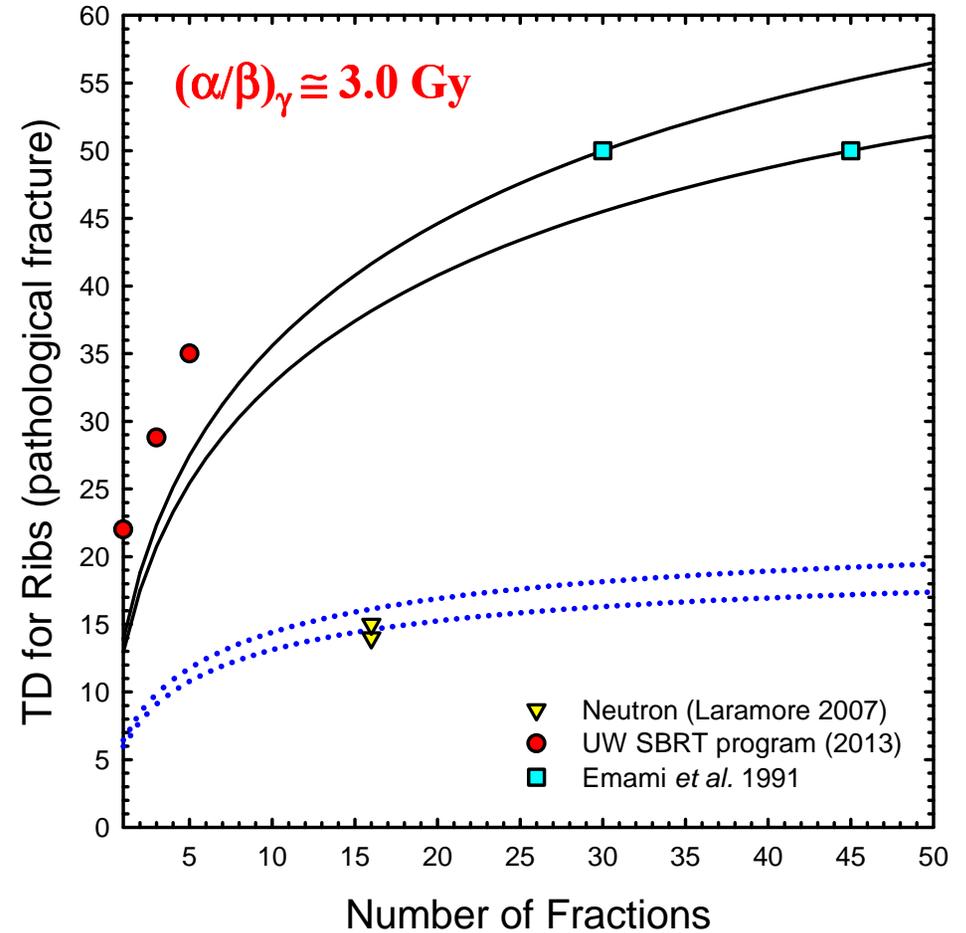
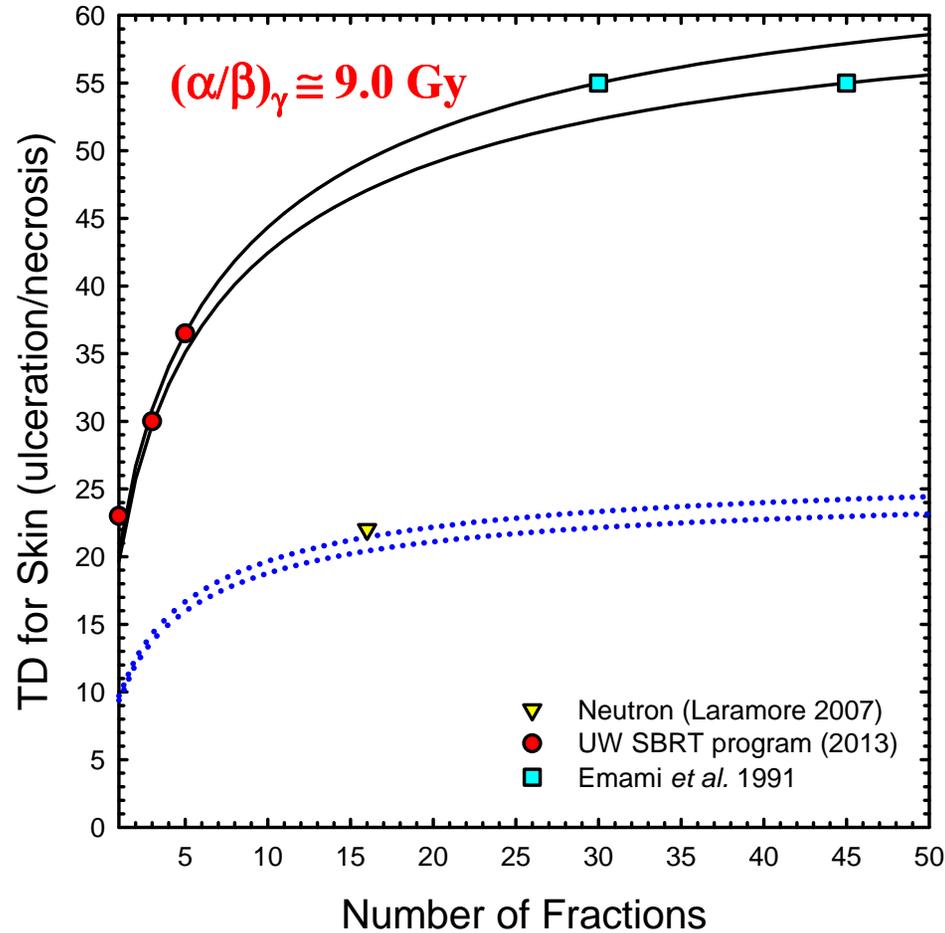


Usual caveats apply about accuracy of tolerance dose estimates

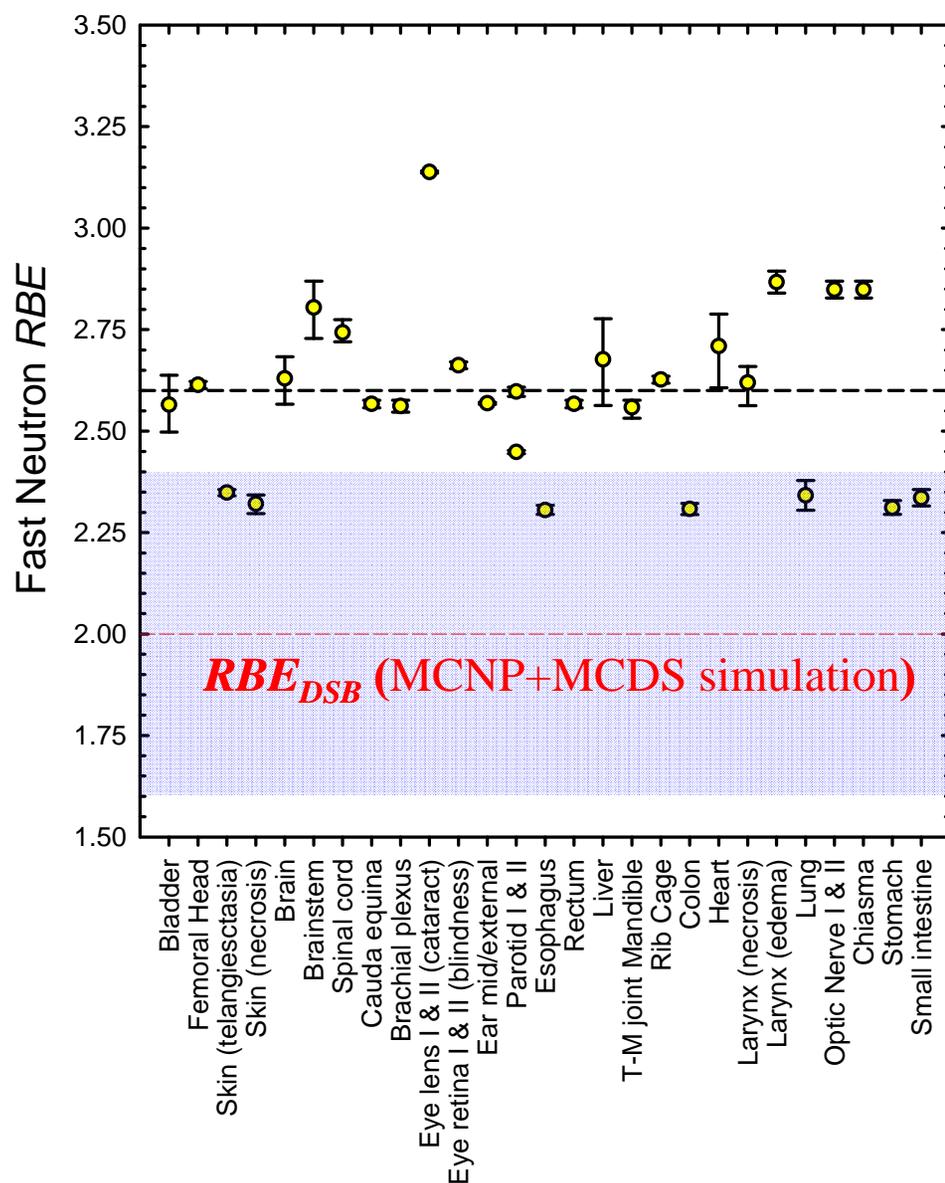
Neutron TD5/5 Dose (*Cauda Equina and Cord*)



Neutron TD5/5 Dose (*Skin and Ribs*)



Fast Neutron RBE for Selected Tissue



Filled circles: $RBE(n = 16) = TD_{\gamma}/TD_n$

Avg RBE = 2.6 ± 0.3

27 tissues/endpoints

Red Dashed line: Monte Carlo (“*first principles*”) simulation of neutron RBE for DSB induction.

Blue Shaded Region: Estimate of RBE for DSB induction derived from analysis of *in vitro* cell survival data for 30 human tumor cell lines (Warenius *et al.* IJROBP 1994).

Clinical RBE $\geq RBE_{DSB}$, as predicted by the RMF model

Summary and Conclusions

- **Much of the uncertainty in proton RBE due to**
 - Uncertainty in dosimetry of the reference radiation and proton beam
 - Need for mechanistic dose-response models to guide the interpretation and analysis of measured data
- **RBE_{DSB} (RBE_{min}) and low dose RBE_{SF} (RBE_{max}) are relevant biological endpoints for (1) local tumor control and (2) tolerance doses for healthy organs and tissues**
- **Ample (*very strong*) evidence that spatial\LET variations in proton RBE are real and clinically relevant (*exploitable*)**
 - **Sticking with a constant $RBE = 1.1$ is a missed opportunity to enhance the therapeutic ratio!**

Thank You!

Supplemental Slides...

- Acknowledgements
- Example of an easy way to setup dose-weighted RBE calculations in MCNP and MCNPX (*DE DF modified F6 tally*)
- Is dose-averaged LET a could surrogate for RBE_{DSB} and/or the RBE_{SF} ?
- Approximate formula linear and linear-quadratic formulas to estimate RBE_{DSB} as a function of proton LET
- Why does RBE_{DSB} increase with increasing LET and the RBE for SSB and base damage decrease with increasing LET?
- Why are some DSB more lethal than others?

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NOTE: “trawets” = “stewart” spelled backwards.

Acknowledgements

***Entire UW physics group* but especially D. Argento, G. Sandison, C. Bloch, E. Ford, F. Yang; other UW faculty: J. Schwartz, G. Laramore, U. Parvatheni**

Many Other (non-UW) Collaborators, especially V. Semenenko, D. Carlson, C. Kirkby, N. Cao, G. Moffitt, S. Streitmatter, T. Jevremovic, Y. Hsaio, V.K. Yu, J.H. Park, M. Frese, R. Rockne, K. Swanson

Example of $D \times RBE$ tally in MCNP

FC1026 RBE-weighted proton (1H+) dose; DSB induction (aerobic)

F1026:H 3

FM1026 0.1602

DE1026 1.000E-03 2.000E-03 3.000E-03 4.000E-03 5.000E-03 6.470E-03
 7.500E-03 1.000E-02 2.000E-02 3.000E-02 4.000E-02 5.000E-02
 6.000E-02 7.000E-02 8.000E-02 9.000E-02 1.000E-01 2.000E-01
 3.000E-01 5.000E-01 9.000E-01 1.000E+00 1.100E+00 1.300E+00
 1.500E+00 2.000E+00 2.500E+00 3.000E+00 3.500E+00 4.000E+00
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DF1026 3.375E+00 3.367E+00 3.368E+00 3.363E+00 3.359E+00 3.352E+00
 3.348E+00 3.340E+00 3.317E+00 3.290E+00 3.264E+00 3.242E+00
 3.216E+00 3.193E+00 3.168E+00 3.143E+00 3.122E+00 2.889E+00
 2.687E+00 2.370E+00 1.986E+00 1.916E+00 1.860E+00 1.760E+00
 1.685E+00 1.542E+00 1.451E+00 1.386E+00 1.336E+00 1.297E+00
 1.244E+00 1.204E+00 1.164E+00 1.123E+00 1.083E+00 1.051E+00
 1.026E+00 1.016E+00 1.012E+00 1.004E+00 1.004E+00 1.003E+00
 1.001E+00 9.995E-01

KE of proton



RBE_{DSB} from
MCDS 3.10A



Above tally will record $D \times RBE_{DSB}$. Divide by dose (*separate tally*) to get dose-averaged RBE.

See <http://faculty.washington.edu/trawets/> for additional (*downloadable*) examples for protons and other particles

Analytic way to estimate an approximate $RBE_{DSB} \times \text{Dose}$ for proton beams?

Recall

$$\frac{D(x)}{\Phi(x)} = \frac{S(x)}{\rho} = \frac{LET_{\infty}(x)}{\rho} \quad \therefore \frac{D(x) / \Phi(x)}{D(x_r) / \Phi(x_r)} = \frac{LET_{\infty}(x) / \rho}{LET_{\infty}(x_r) / \rho}$$

If we know the LET and dose per unit fluence at a reference location x_r , LET at other locations along depth-dose curve computed from

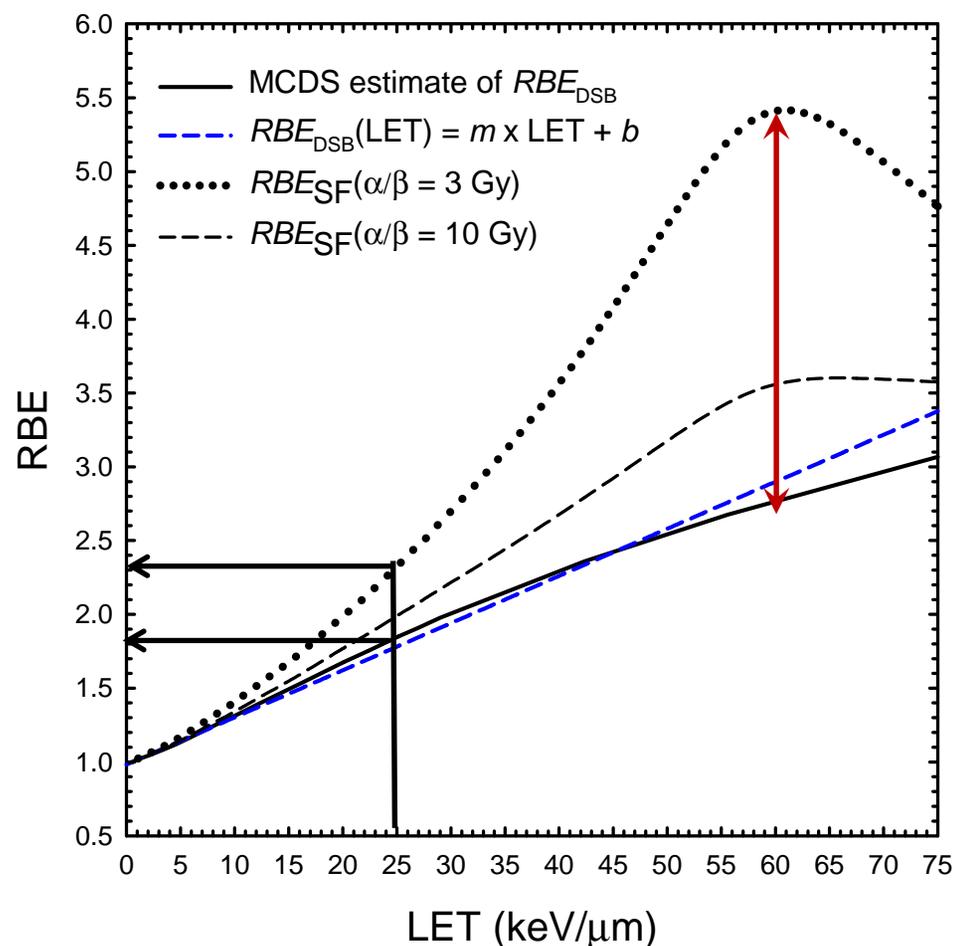
$$LET_{\infty}(x) = LET_{\infty}(x_r) \frac{D(x) / \Phi(x)}{D(x_r) / \Phi(x_r)}$$

$$RBE_{DSB}(x)D(x) = (mLET_{\infty}(x) + b)D(x)$$

$$m = 0.03193 \mu\text{m/keV} \quad \text{and} \quad b = 0.98274$$

Simple formulism to connect patient-specific QA measurements of dose-average LET to RBE_{DSB} and (hence) the RBE_{SF} (via RMF model)?

LET_D instead of RBE_{DSB} or RBE_{SF} ?



For a clinically relevant* range of proton energies (LET < 25 keV/ μm), dose-averaged LET is a good surrogate for RBE_{DSB} and the low dose RBE_{SF} .

$$m = 0.03193 \text{ RBE}/(\text{keV}/\mu\text{m})$$

$$b = 0.98274$$

For tumors and/or tissues with a low α/β , RBE_{SF} may be larger than RBE_{DSB} by 25-30% larger at 25 keV/ μm .

* **Caveat:** ± 2 mm of the Bragg peak really low energy protons (< 1-5 MeV) contribute in a substantial way to dose and RBE.

LQ fit to proton RBE_{DSB} as function of LET

To better capture trends in the RBE for DSB induction as a function of LET, a linear-quadratic (LQ) fit is highly recommended.

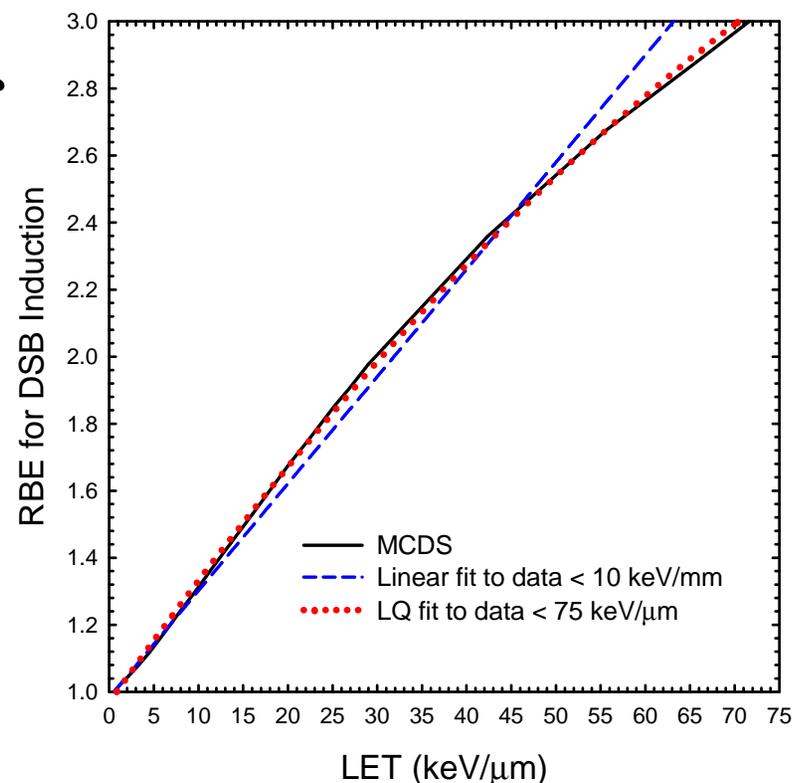
$$RBE_{DSB} = a \cdot LET^2 + b \cdot LET + c$$

$$a = 6.771 \times 10^{-3}$$

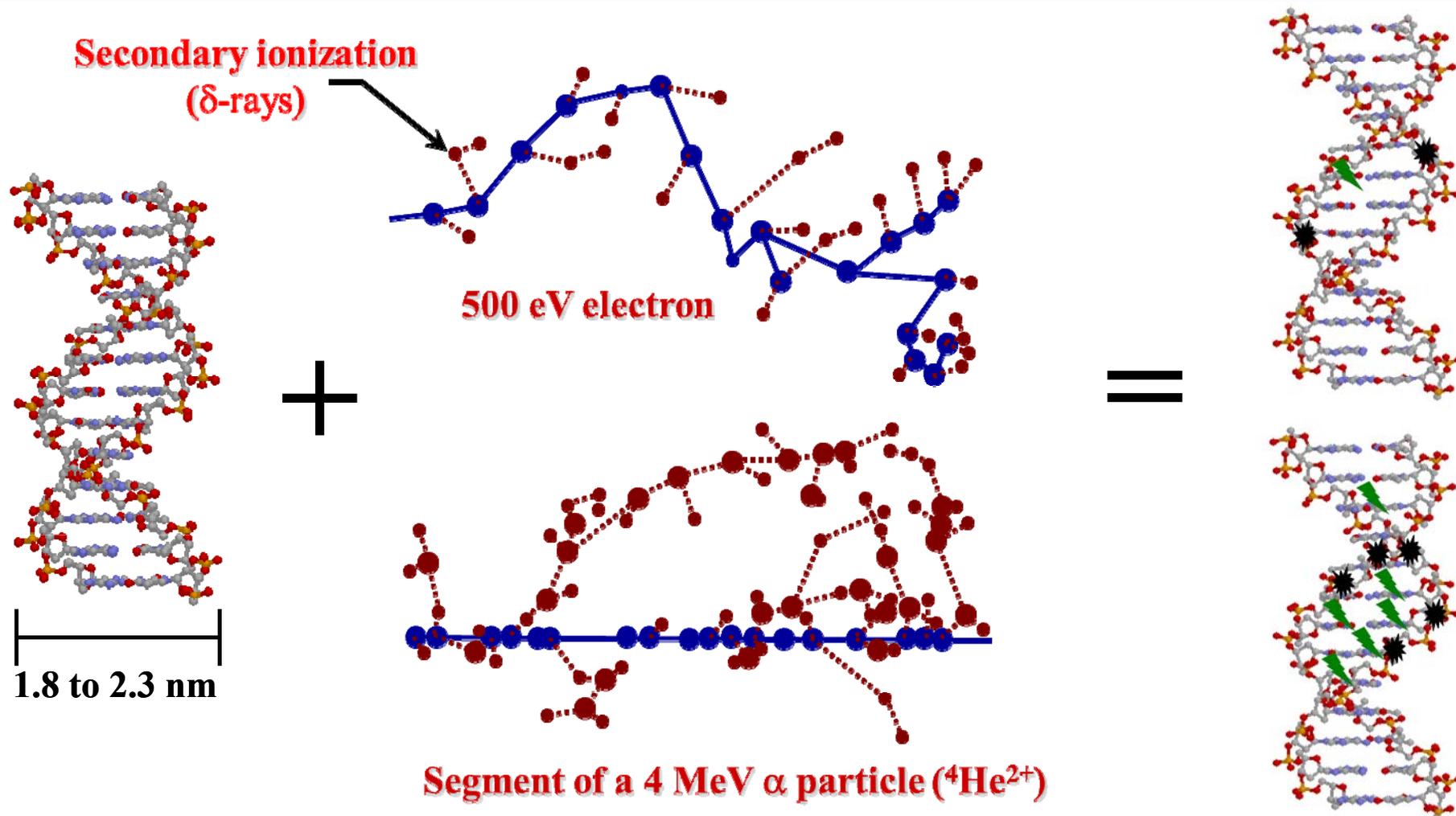
$$b = 2.553 \times 10^{-2}$$

$$c = 9.969 \times 10^{-1}$$

*** Coefficients for fit may need to be adjusted slightly to correct for uncertainties in proton LET.**



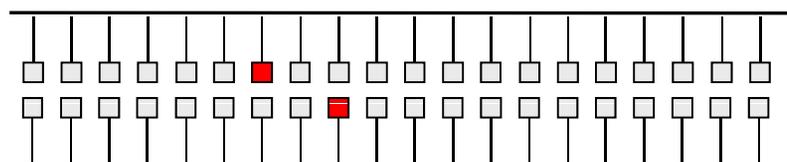
Ionization Density and Cluster Complexity



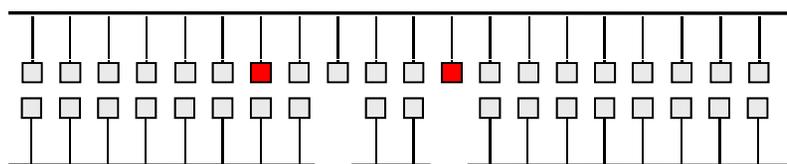
Number of DNA lesions per cluster tends to increase with increasing particle LET.

Why does $RBE_{DSB} \uparrow$ and RBE_{SSB} and $RBE_{Bd} \downarrow$

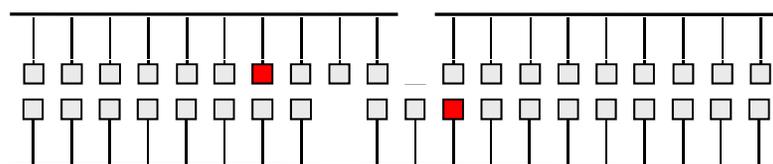
A cluster categorized as a DSB cannot also be categorized as a (simple or complex) SSB or as a (simple or complex) cluster of nucleotides with base damage – *mutually exclusive categories of DNA damage*



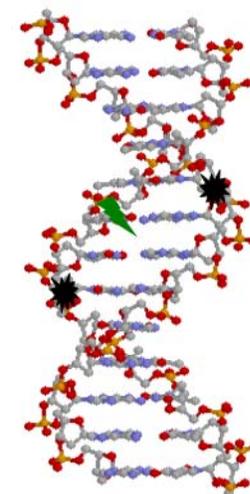
Cluster = 2 nucleotides with base damage



Cluster = complex SSB



Cluster = complex DSB



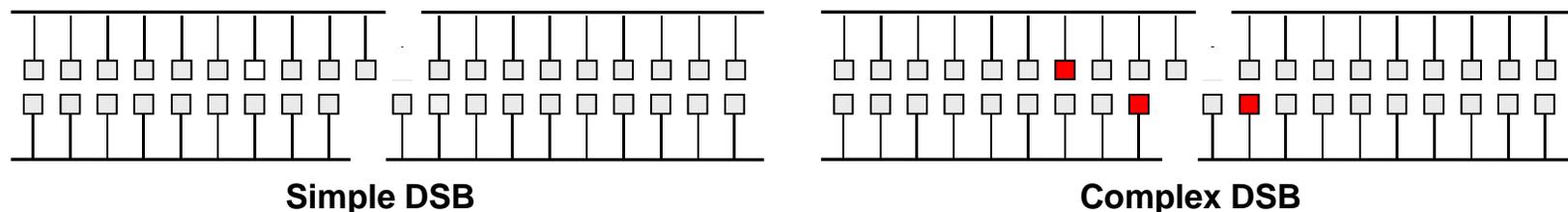
Chance a cluster will contain a pair of opposed strand breaks within about 10 bp increases (*i.e.*, be a simple or complex DSB) as LET and the number of DNA lesions per cluster increases.

Why are some DSB (*more*) lethal and others not?

Answer: *we don't know for sure...*

Hypotheses:

(1) Some DSB are unrepairable (*unrejoinable*) or more slowly rejoined than others because of the local (*spatial*) complexity of DNA lesions



(2) DSB formed in close spatial and temporal proximity to other DSB are more often mis-rejoined to form chromosome aberrations than DSB separated in time and/or space (*breakage and reunion theory*)

(3) Combination of mechanisms **(1)** and **(2)**

RMF model (Carlson *et al.* 2008) tends to emphasize mechanism 2

Critical MCDS and RMF Literature Citations

- V.A. Semenenko and R.D. Stewart. A fast Monte Carlo algorithm to simulate the spectrum of DNA damages formed by ionizing radiation. *Radiat Res.* **161**(4), 451-457 (2004)
- V.A. Semenenko and R.D. Stewart. Fast Monte Carlo simulation of DNA damage formed by electrons and light ions. *Phys. Med. Biol.* **51**(7), 1693-1706 (2006)
- D.J. Carlson, R.D. Stewart, V.A. Semenenko and G.A. Sandison, Combined use of Monte Carlo DNA damage simulations and deterministic repair models to examine putative mechanisms of cell killing. *Rad. Res.* **169**, 447-459 (2008)
- R.D. Stewart, V.K. Yu, A.G. Georgakilas, C. Koumenise, J.H. Park, D.J. Carlson, Effects of Radiation Quality and Oxygen on Clustered DNA Lesions and Cell Death, *Radiat. Res.* **176**, 587-602 (2011). **MCDS Version 3.10A developed and tested in this one.**
- M.C. Frese, V.K. Yu, R.D. Stewart, D.J. Carlson, A Mechanism-Based Approach to Predict the Relative Biological Effectiveness of Protons and Carbon Ions in Radiation Therapy, *Int. J. Radiat. Oncol. Biol. Phys.*, **83**, 442-450 (2012).
- • C Kirkby, E Ghasroddashti, Y Poirier, M Tambasco, RD Stewart, Monte Carlo Simulations of Relative DNA Damage From KV CBCT Radiation. *Phys. Med. Biol.* **58**, 5693-5704 (2013)
- A.G. Georgakilas, P.O'Neill, R.D. Stewart, Induction and Repair of Clustered DNA Lesions: What Do We Know So Far? *Radiat. Res.* **180**,100-109 (2013)