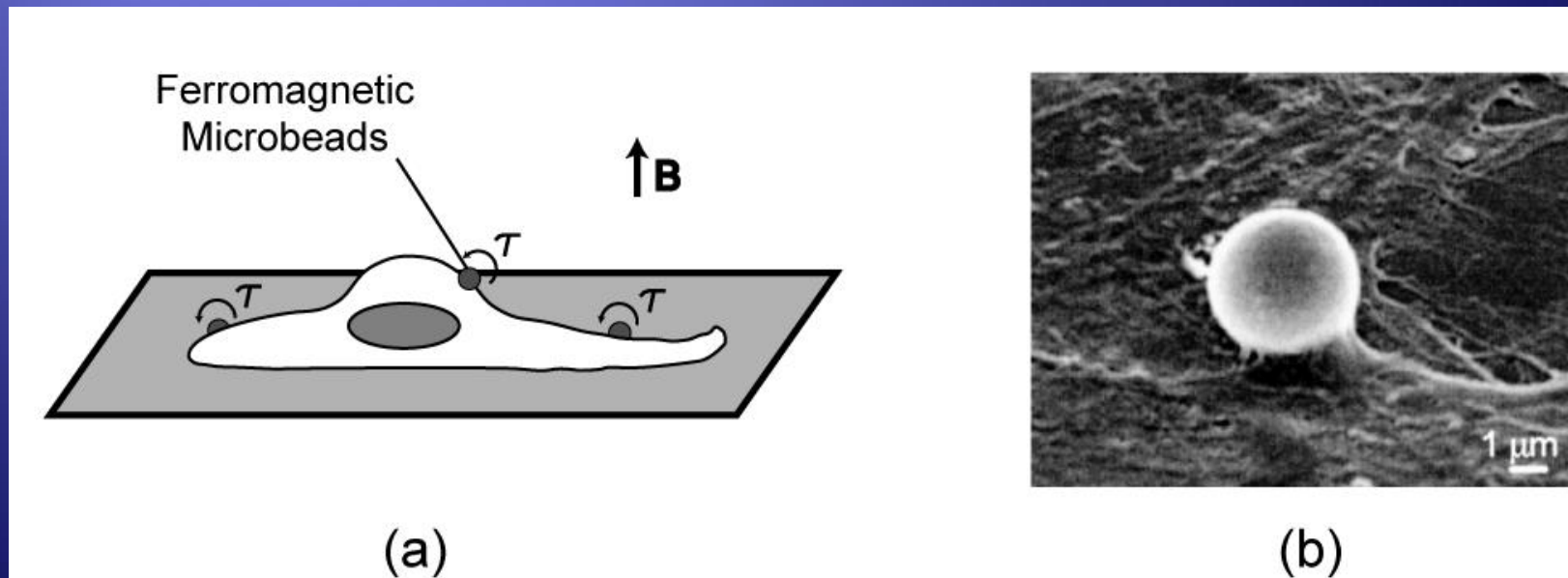


Session 17

# SOFT GLASSY RHEOLOGY

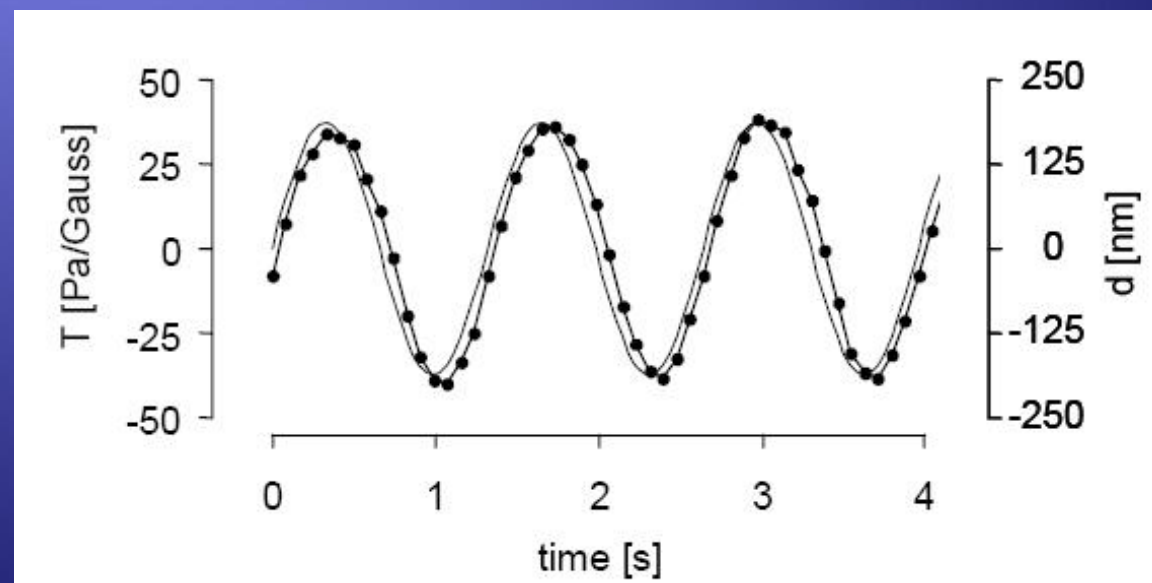
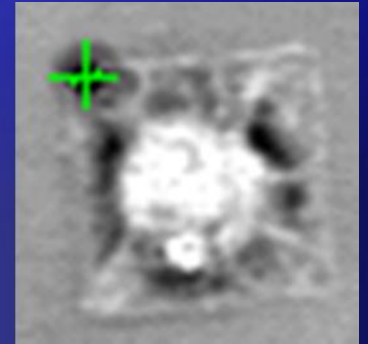
# Recall: Magnetic Twisting Cytometry

- ◆ Torque applied at surface of cells with magbeads
- ◆ Used to determine cell mechanics
  - ◆ Cellular viscoelasticity (Fabry, Fredberg)
  - ◆ Mechanotransduction (Wang, Ingber)



# Particle Tracking Measurement

- ◆ Fast, real-time image analysis
  - ◆ 16 frames per twist
  - ◆ Stroboscopic technique for  $>1$  Hz twists
- ◆ Individual particle tracking using intensity-weighted centroid calculation.
- ◆ Small phase lag between twist frequency and displacement frequency



# Complex Modulus

- ◆ Complex modulus defined by ratio of complex applied torque and complex bead displacement

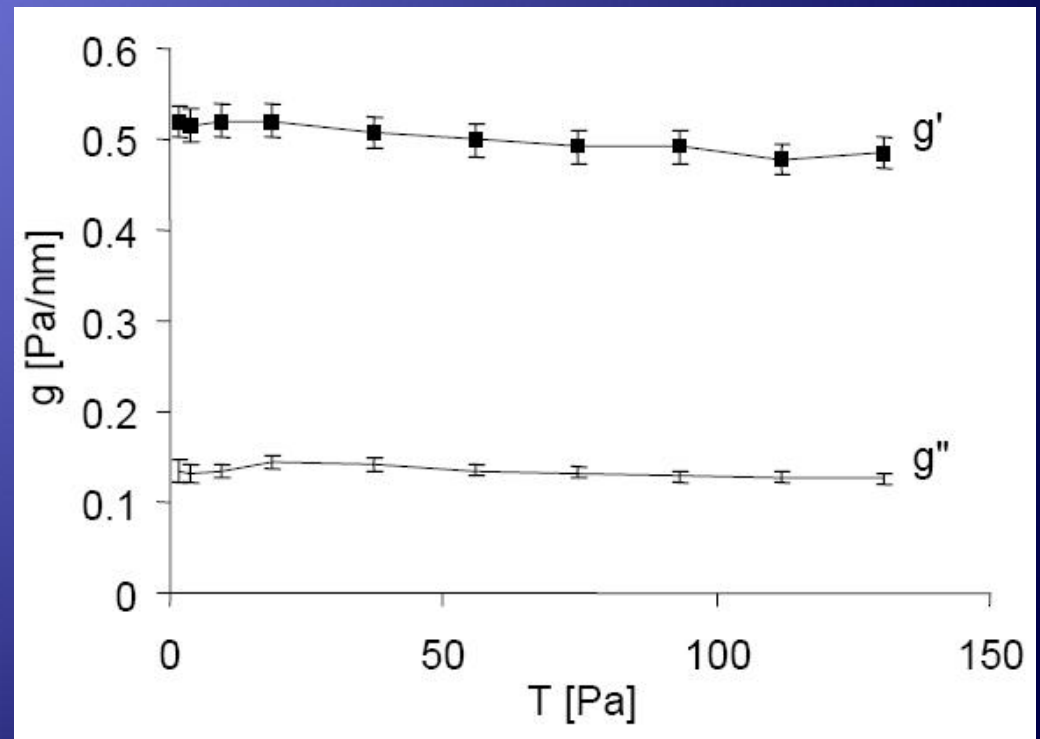
$$g = T/d$$

- ◆ Elastic (storage) modulus:  $g' = \text{Re}(\cdot)$
- ◆ Loss modulus:  $g'' = \text{Im}(\cdot)$
- ◆ Loss tangent:  $= g''/g'$
- ◆ Transform to storage modulus and loss modulus through geometric factor  $= 6.8 \mu\text{m}$

$$G = r g$$

# Shear Stress Response

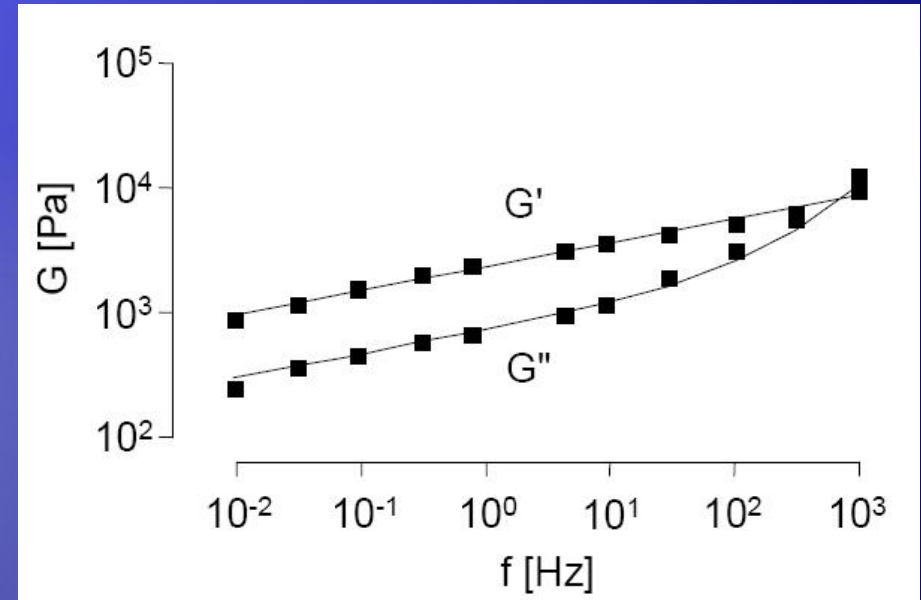
- ◆ Physiological range of stress
- ◆ Linear mechanical behavior observed
- ◆ No observation of nonlinear behavior as by others
  - ✗ Strain-hardening
  - ✗ Shear-thinning



# Frequency Response

- ◆ Storage modulus
  - ◆ Increased with frequency
  - ◆ Weak power law observed on log-log plot

$$G' \propto f^{x-1}$$



- ◆ Loss modulus
  - ◆ Smaller than G' except at 1 kHz
  - ◆ Weak power law observed for < 10 Hz
  - ◆ Newton viscosity characteristics observed > 10 Hz
    - ◆ Slope approaches 1 ( $x = 2$ )

# Structural Damping Law

- ◆ In angular frequency domain ( $\omega = 2\pi f$ )

$$g = g_0 \left( \frac{\check{S}}{\Phi_0} \right)^{x-1} (1 - i\bar{y}) \Gamma(2-x) \cos \frac{f}{2}(x-1) + i\check{S} \sim$$

$$\bar{y} = \tan \frac{f}{2}(x-1)$$

- ◆ Scale factor for stiffness:  $g_0$
- ◆ Scale factor for frequency:  $\Phi_0$
- ◆ Gamma Function:  $\Gamma$
- ◆ Newtonian viscosity:  $\mu$

# Structural Damping Law

$$g = g_0 \left( \frac{\check{S}}{\Phi_0} \right)^{x-1} (1 - i\bar{y}) \Gamma(2-x) \cos \frac{f}{2}(x-1) + i\check{S} \sim$$

$$\bar{y} = \tan \frac{f}{2}(x-1)$$

- ◆ Storage modulus is real part of equation
- ◆ Loss modulus is imaginary part of equation
  - ◆ Newton viscous term  $i \mu$  relevant at hi frequency only
  - ◆ As  $x \rightarrow 1$ ,  $\tan(0) \rightarrow 0$ ,  $\bar{y} \rightarrow 0$ ,  $g' \rightarrow g_0$  (Solid-like)
  - ◆ As  $x \rightarrow 2$ ,  $\cos(\pi/2) \rightarrow 0$ ,  $g'' \rightarrow \mu$  (Fluid-like)

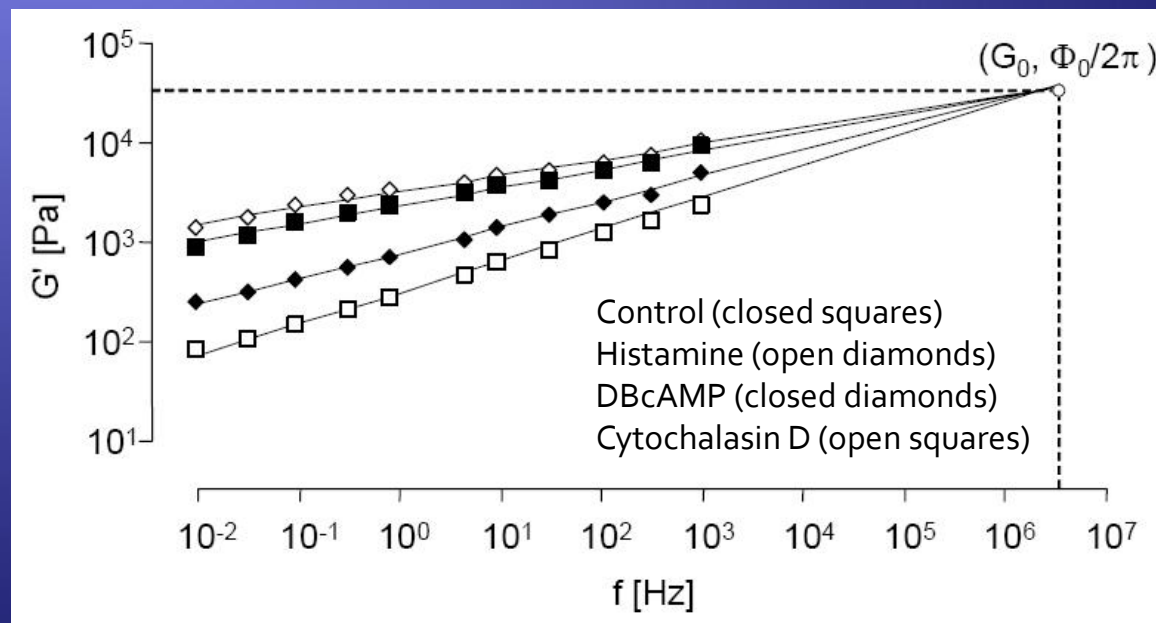


# Independence of Parameters

- ◆ Structural damping described by parameters:
  - ◆ Scale factor for stiffness:  $g_0$
  - ◆ Scale factor for frequency:  $\Phi_0$
  - ◆ Newtonian viscosity:  $\mu$
  - ◆ Power law exponent:  $x$
- ◆ Noise temperature ( $x$ ) is master parameter
  - ◆ Shown in following slides

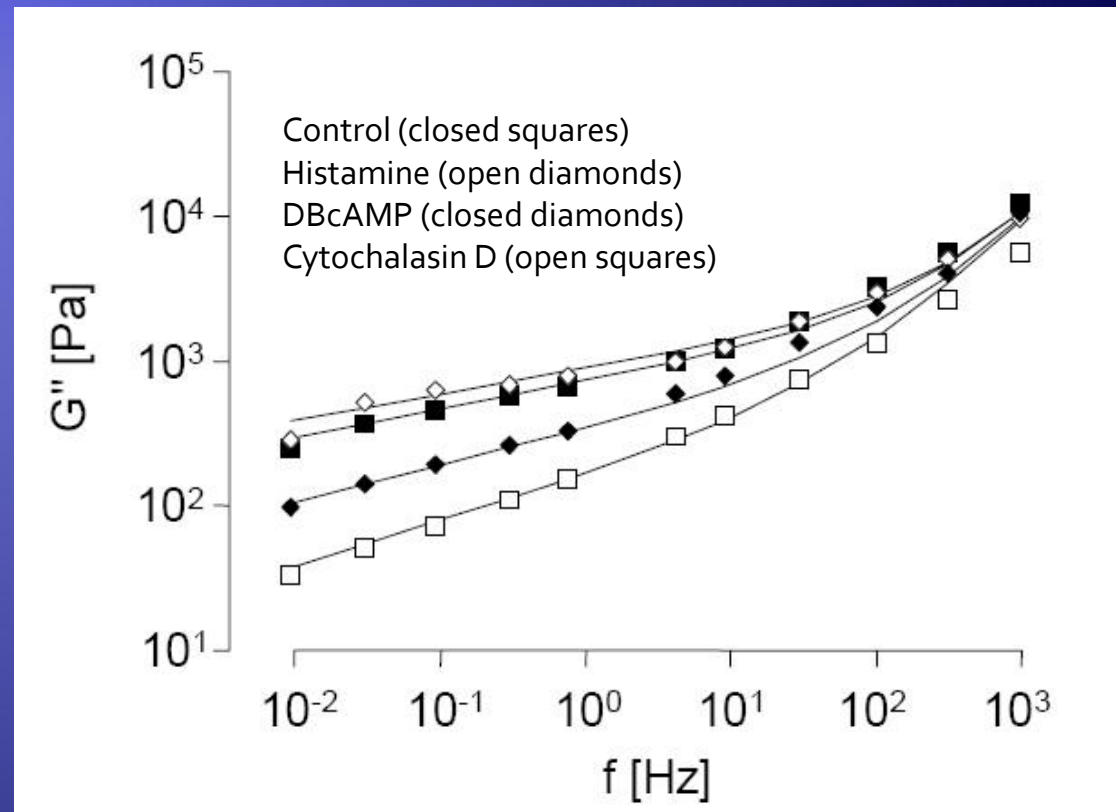
# Contractility & CSK Disruption

- ◆ Common intersection exists for  $G'$  vs.  $f$  curves
  - ◆ Lines represent structural damping equation
  - ◆ Parameters  $g_0, \Phi_0$  appear invariant with drugs
- ◆ Statistical analysis
  - ◆ 3 parameter fit ( $g_0, \Phi_0, x$ ) is not statistically different than 1 parameter fit ( $x$  and  $g_0, \Phi_0$  fixed)



# Contractility & CSK Disruption

- ◆ Loss moduli merge onto single curve at high  $f$
- ◆ Fixed  $\mu$  can match the data
- ◆ However, varied  $\mu$  can slightly improve statistical fit
- ◆ This plus  $g_0$ ,  $\Phi_0$  argument indicates  $x$  as single cell mechanics parameter

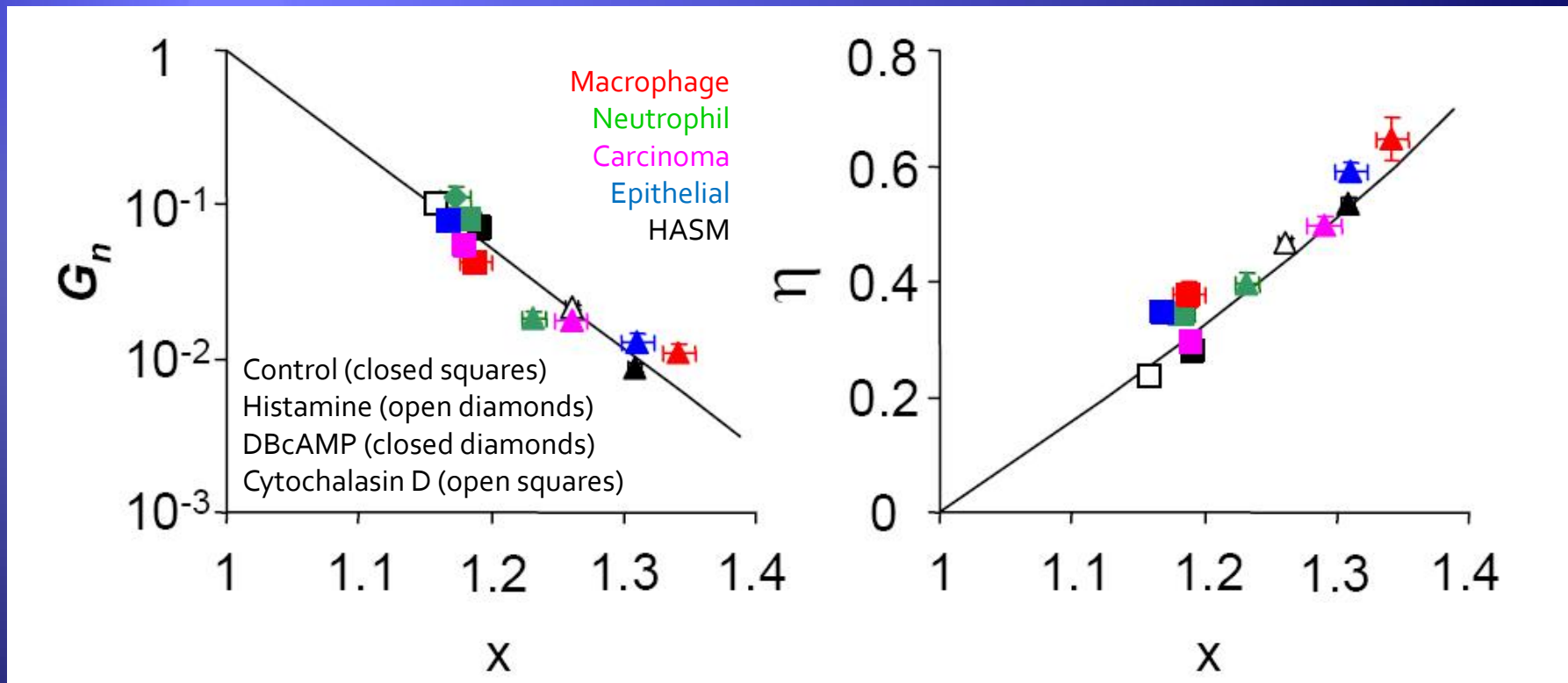


# Universality

- ◆ Common structural damping behavior
  - ◆ Power-law for  $G'$  and  $G''$  vs.  $f$
  - ◆ Common extrapolated intersection of  $G'$  vs.  $f$  with drug treatment
  - ◆ Merging of  $G''$  vs.  $f$  curves to single line at high freq
- ◆ Observed in
  - ◆ Cell types: macrophages, neutrophils, endothelial, epithelial, fibroblasts, cancer cells
  - ◆ CSK drugs: Myosin inhibitors (BDM), MLCK inhibitors (ML-7, ML-9), ROCK inhibitors, actin polymerizing inhibitors (Latrunculin), actin stabilizers (jasplakinolide)
  - ◆ Ligand types: RGD-peptide, collagen, vitronectin, fibronectin, urokinase, acetylated-LDL, adhesion receptor antibodies
  - ◆ Testing systems: AFM, mag-tweezers, rotating disk rheometers

# Master Curves

- Normalized stiffness  $G_n = G'_{0.75 \text{ Hz}} / G_0$



$$G_n = \frac{G'}{G_0} = \frac{\text{Re}(G)}{G_0} \Rightarrow \ln G_n = (x-1) \ln \left( \frac{2f f}{\Phi_0} \right) \quad y = \tan \frac{f}{2} (x-1)$$

# Soft Glassy Rheology

- ◆ Material types include foams, pastes, colloids, emulsions, slurries, (and cells)
- ◆ Common behavior
  - ◆ Small elasticity (Pa to 1 kPa)
  - ◆ Weak power-law for  $G'$  and  $G''$  vs.  $f$
  - ◆ Loss tangent  $\eta$  is frequency independent and order 0.1
- ◆ Shared generic properties
  - ◆ Composed of elements that are discrete, numerous, aggregate with one another via weak interactions
  - ◆ Geometric arrangement that is structurally disordered and metastable

# Soft Glassy Rheology Theory

- ◆ Elements (particles, proteins, beads, etc.) contained in an energy landscape that contains deep energy wells
  - ◆ Energy wells defined from interactions with other elements
  - ◆ Individual elements unable to escape wells by thermal energy alone but by agitation
- ◆ Parameter  $x$  is measure of agitation
  - ◆ “Effective Temperature” or “Noise Level”
  - ◆ When  $x = 1$ , materials is in a frozen state has ordered structure and elasticity
  - ◆ When  $x > 1$ , sufficient “noise” that elements can hop between wells. and system can flow and become more disordered

# Soft Glass Rheology for Cells

- ◆ Cellular energy wells from CSK binding energies
  - ◆ Actin filament cross-linking
  - ◆ Actin-myosin cross-bridges
  - ◆ Hydrophobic interactions
  - ◆ Ionic charge or size exclusion
- ◆ Drug effects
  - ◆ Agents that inactivate contractile apparatus or cytoskeletal disruption move cell away from frozen state (glass transition)
  - ◆ Decreasing noise temperature is formation of ordered structure
  - ◆ Increasing noise temperature is disordered and fluid state

