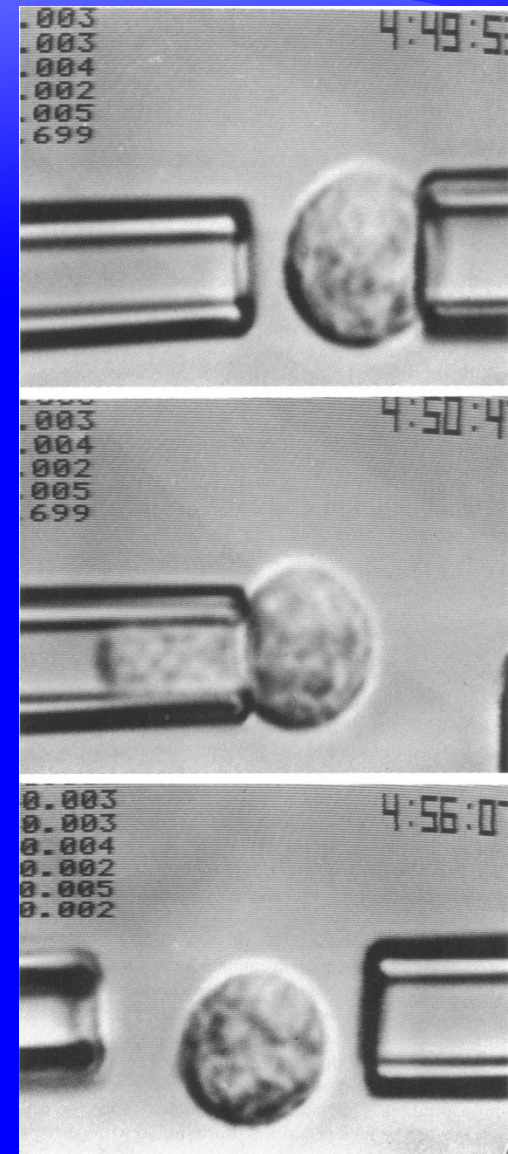


Session 13

# SIMPLE LIPID SYSTEMS

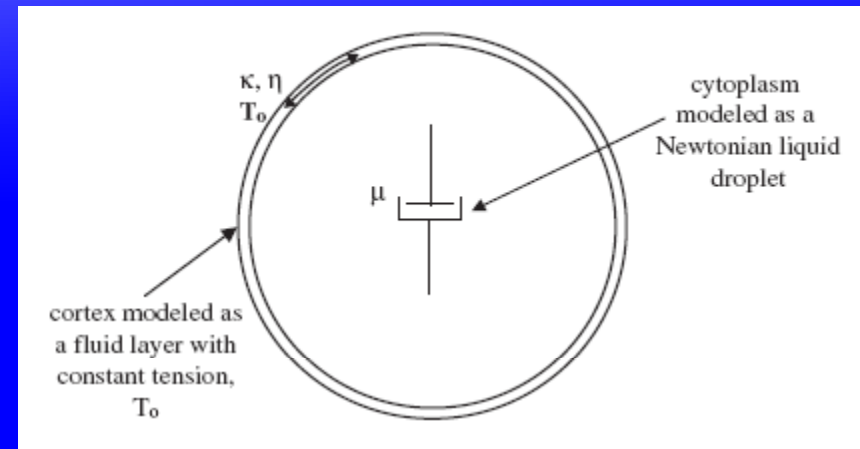
# Micropipette Aspiration

- ◆ Measure non-adherent cells
  - ◆ Exhibit liquid-like flow behavior
    - ◆ Rate of entry depends on pressure
  - ◆ Exhibit surface tension behavior
    - ◆ Recovers shape upon release
- ◆ Is a fluid droplet model appropriate?
  - ◆ What is cellular viscosity?
  - ◆ What is mechanical coupling to cortex?



# Newtonian Liquid Drop Model

- ◆ Model:
  - ◆ Cortical layer enclosing a Newtonian liquid
- ◆ Core:
  - ◆ Cytoplasm viscosity:  $\mu$
  - ◆ Newtonian fluid: Stress ( $\tau$ ) vs. velocity gradient is linear:  
$$\tau = \mu (du/dy)$$
- ◆ Cortex:
  - ◆ Anisotropic viscous fluid layer
  - ◆ Negligible bending stiffness
  - ◆ Two viscosity terms
    - ◆  $\kappa$  is dilation viscosity
    - ◆  $\eta$  is shear viscosity



- ◆ Pipet:
  - ◆ Frictionless interaction
  - ◆ Reaction force at pipet orifice

# Approach

- ◆ Define constitutive relationship for liquid core
  - ◆ Equations of motion for Newtonian fluid with creeping flow
- ◆ Determine boundary conditions
  - ◆ Equations of motion for cortical shell (cortex)
  - ◆ Equations of viscous deformation for cortical shell
  - ◆ No slip condition at core-cortex interface

# Approach

- ◆ Not an easy task to obtain numerical solution to this problem
  - ◆ Discontinuities
  - ◆ Inversion difficulties
- ◆ Yeung & Evans' approach
  - ◆ Spherical solutions exist for cell exterior to pipet
  - ◆ Course approximation used for flow inside pipet
  - ◆ Coupling provided by pressure difference:

$$\Delta P = (p_o - p_{\text{orif}}) + (p_{\text{orif}} - p_i)$$

# Core: Creeping Flow

- ◆ Equations of motion

$$\sigma_{ij} = -p \cdot \delta_{ij} + \mu \left[ \frac{\partial v_i}{\partial x_j} + \frac{\partial v_j}{\partial x_i} \right], \quad (1)$$

- ◆ By means of indicial notation, this is

$$\sigma_{11} = -p + \mu \left( \frac{\partial u_1}{\partial x_1} + \frac{\partial u_1}{\partial x_1} \right) = -p + 2\mu \frac{\partial u_1}{\partial x_1}$$

$$\sigma_{22} = -p + 2\mu \frac{\partial u_2}{\partial x_2}$$

$$\sigma_{12} = \mu \left( \frac{\partial u_1}{\partial x_2} + \frac{\partial u_2}{\partial x_1} \right) = \sigma_{21}$$

$$\sigma_{23} = \mu \left( \frac{\partial u_2}{\partial x_3} + \frac{\partial u_3}{\partial x_2} \right) = \sigma_{32}$$

$$\sigma_{13} = \mu \left( \frac{\partial u_1}{\partial x_3} + \frac{\partial u_3}{\partial x_1} \right) = \sigma_{31}$$

$$\sigma_{33} = -p + 2\mu \frac{\partial u_3}{\partial x_3}$$

# Core

- ◆ In rectilinear coordinates

$$\sigma_{11} = -p + 2\mu \frac{\partial u_1}{\partial x_1}$$

$$\sigma_{12} = \mu \left( \frac{\partial u_1}{\partial x_2} + \frac{\partial u_2}{\partial x_1} \right) = \sigma_{21}$$

$$\sigma_{13} = \mu \left( \frac{\partial u_1}{\partial x_3} + \frac{\partial u_3}{\partial x_1} \right) = \sigma_{31}$$

$$\sigma_{22} = -p + 2\mu \frac{\partial u_2}{\partial x_2}$$

$$\sigma_{23} = \mu \left( \frac{\partial u_2}{\partial x_3} + \frac{\partial u_3}{\partial x_2} \right) = \sigma_{32}$$

$$\sigma_{33} = -p + 2\mu \frac{\partial u_3}{\partial x_3}$$



$$\sigma_x = -p + 2\mu \frac{\partial u}{\partial x}$$

$$\tau_{xy} = \mu \left( \frac{\partial u}{\partial y} + \frac{\partial v}{\partial x} \right) = \tau_{yx}$$

$$\tau_{xz} = \mu \left( \frac{\partial u}{\partial z} + \frac{\partial w}{\partial x} \right) = \tau_{zx}$$

$$\sigma_y = -p + 2\mu \frac{\partial v}{\partial y}$$

$$\tau_{yz} = \mu \left( \frac{\partial v}{\partial z} + \frac{\partial w}{\partial y} \right) = \tau_{zy}$$

$$\sigma_z = -p + 2\mu \frac{\partial w}{\partial z}$$

# Core

- ◆ Incompressibility condition for a fluid

$$\sum_k \frac{\partial v_k}{\partial x_k} = 0. \quad (2)$$

- ◆ By means of indicial notation

$$\frac{\partial u_1}{\partial x_1} + \frac{\partial u_2}{\partial x_2} + \frac{\partial u_3}{\partial x_3} = 0$$

$$\left( \frac{\partial u}{\partial x} + \frac{\partial v}{\partial y} + \frac{\partial w}{\partial z} = 0 \right)$$

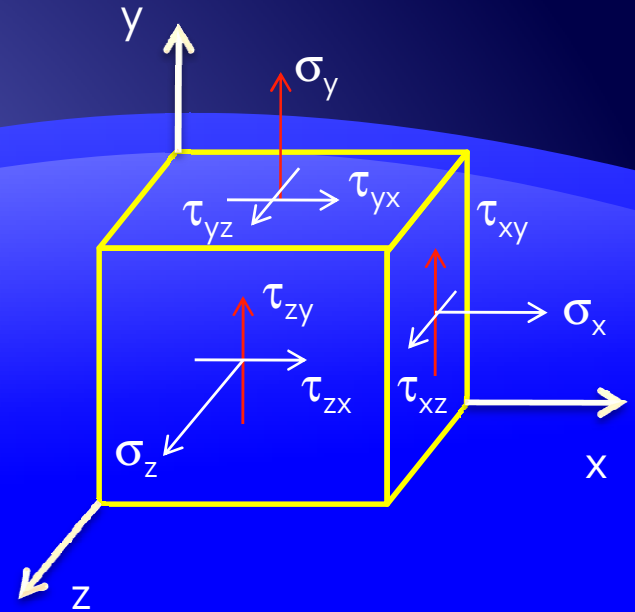
- ◆ Consider one-dimensional flow  $(x, u)$ . If gradient exists, then fluid density would have to expand or compress to satisfy.



# Core

- ◆ Mechanical equilibrium

$$\sum_k \frac{\partial \sigma_{ik}}{\partial x_k} = 0$$



- ◆ By means of indicial notation

$$\frac{\partial \sigma_{11}}{\partial x_1} + \frac{\partial \sigma_{12}}{\partial x_2} + \frac{\partial \sigma_{13}}{\partial x_3} = 0$$

$$\frac{\partial \sigma_{21}}{\partial x_1} + \frac{\partial \sigma_{22}}{\partial x_2} + \frac{\partial \sigma_{23}}{\partial x_3} = 0$$

$$\frac{\partial \sigma_{31}}{\partial x_1} + \frac{\partial \sigma_{32}}{\partial x_2} + \frac{\partial \sigma_{33}}{\partial x_3} = 0$$



$$\frac{\partial \sigma_x}{\partial x} + \frac{\partial \tau_{xy}}{\partial y} + \frac{\partial \tau_{xz}}{\partial z} = 0$$

$$\frac{\partial \tau_{yx}}{\partial x} + \frac{\partial \sigma_y}{\partial y} + \frac{\partial \tau_{yz}}{\partial z} = 0$$

$$\frac{\partial \tau_{zx}}{\partial x} + \frac{\partial \tau_{zy}}{\partial y} + \frac{\partial \sigma_z}{\partial z} = 0$$

# Core

- ◆ By taking derivative of each equation (1), e.g.

$$\frac{\partial \sigma_{11}}{\partial x_1} = -\frac{\partial p}{\partial x_1} + 2\mu \frac{\partial^2 u_1}{\partial x_1^2}$$

$$\frac{\partial \sigma_{12}}{\partial x_2} = \mu \left( \frac{\partial^2 u_1}{\partial x_2^2} + \frac{\partial^2 u_2}{\partial x_1 \partial x_2} \right)$$

$$\frac{\partial \sigma_{13}}{\partial x_3} = \mu \left( \frac{\partial^2 u_1}{\partial x_3^2} + \frac{\partial^2 u_3}{\partial x_1 \partial x_3} \right)$$

- ◆ Can sum together to get

$$\frac{\partial \sigma_{11}}{\partial x_1} + \frac{\partial \sigma_{12}}{\partial x_2} + \frac{\partial \sigma_{13}}{\partial x_3} = -\frac{\partial p}{\partial x_1} + \mu \left( \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_2^2} + \frac{\partial^2 u_2}{\partial x_1 \partial x_2} + \frac{\partial^2 u_1}{\partial x_3^2} + \frac{\partial^2 u_3}{\partial x_1 \partial x_3} \right)$$

# Core

- ◆ Simplifying by mechanical equilibrium

$$\frac{\partial \sigma_{11}}{\partial x_1} + \frac{\partial \sigma_{12}}{\partial x_2} + \frac{\partial \sigma_{13}}{\partial x_3} = -\frac{\partial p}{\partial x_1} + \mu \left( \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_2^2} + \frac{\partial^2 u_2}{\partial x_1 \partial x_2} + \frac{\partial^2 u_1}{\partial x_3^2} + \frac{\partial^2 u_3}{\partial x_1 \partial x_3} \right)$$
$$0 = -\frac{\partial p}{\partial x_1} + \mu \left( \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_2^2} + \frac{\partial^2 u_2}{\partial x_1 \partial x_2} + \frac{\partial^2 u_1}{\partial x_3^2} + \frac{\partial^2 u_3}{\partial x_1 \partial x_3} \right)$$

- ◆ Simplifying by incompressibility condition

$$0 = -\frac{\partial p}{\partial x_1} + \mu \left( \frac{\partial}{\partial x_1} \left( \frac{\partial u_1}{\partial x_1} + \frac{\partial u_2}{\partial x_2} + \frac{\partial u_3}{\partial x_3} \right) + \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_2^2} + \frac{\partial^2 u_1}{\partial x_3^2} \right)$$
$$0 = -\frac{\partial p}{\partial x_1} + \mu \left( \frac{\partial^2 u_1}{\partial x_1^2} + \frac{\partial^2 u_1}{\partial x_2^2} + \frac{\partial^2 u_1}{\partial x_3^2} \right)$$

- ◆ Have creeping flow eqs.

$$\frac{\partial p}{\partial x_i} = \mu \cdot \sum_k \frac{\partial^2 v_i}{\partial x_k^2}, \quad (3)$$

# Cortex

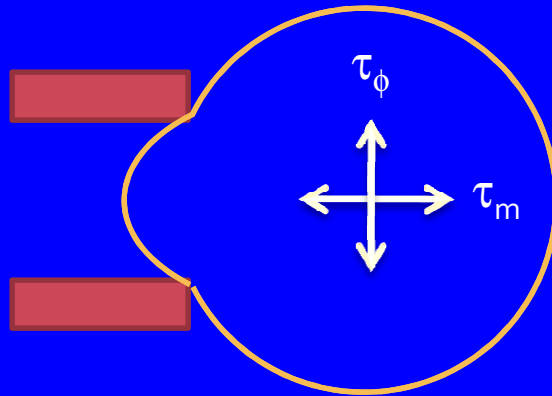
- ◆ Stress Resultants ( $\tau_m, \tau_\phi$ )
  - ◆ For thin shell, stresses integrated by thickness

$$\tau = \int \sigma_{ij} d\delta$$

- ◆ Units [N/m]
- ◆ Types: lateral, bending, torque, transverse

# Cortex

- ◆ Coordinate system:  $(s, \theta)$
- ◆ Axisymmetry yields in-plane stress resultants
  - ◆ Meridional  $\tau_m$  :  $\tau_m \approx \sigma_m \delta$
  - ◆ Circumferential  $\tau_\phi$  :  $\tau_\phi \approx \sigma_\phi \delta$

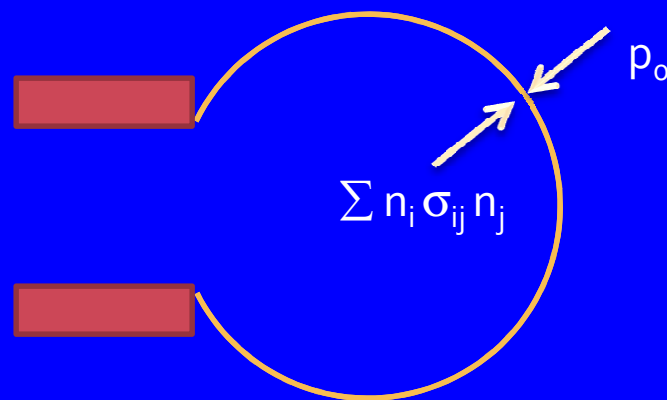


# Cortex

- ◆ Balance of forces in normal direction

$$\Delta\sigma_n \equiv \sigma_n - \sum_{i,j} n_i \cdot \sigma_{ij} \cdot n_j = \tau_m \cdot \frac{d\theta}{ds} + \tau_\phi \cdot \frac{\sin \theta}{r}, \quad (4)$$

where  $\sigma_n = p_o$  the outside pressure,  $n_i$  are unit vectors normal to the surface, and  $\sum n_i \sigma_{ij} n_j$  are normal tractions on the interior surface by the liquid core

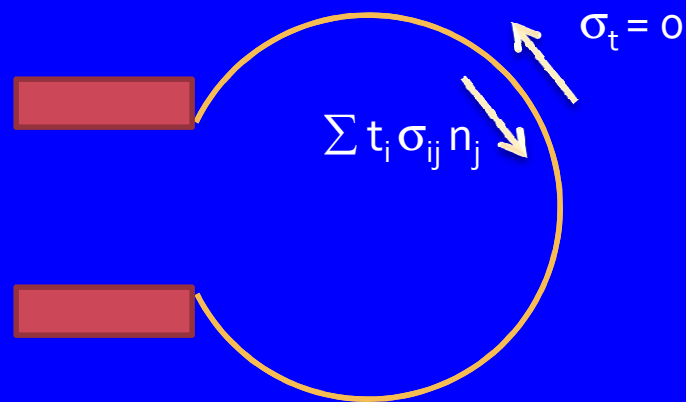


# Cortex

- ◆ Balance of forces in tangential direction

$$\Delta\sigma_t \equiv -\sigma_t + \sum_{i,j} t_i \cdot \sigma_{ij} \cdot n_j = \frac{d\tau_m}{ds} + \left[ \frac{\tau_m - \tau_\phi}{r} \right] \cos\theta. \quad (5)$$

where  $\sigma_t = 0$  on the outside,  $t_i$  are unit vectors tangential to the surface, and  $\sum t_i \sigma_{ij} n_j$  are tangential tractions on the interior surface by the liquid core



# Cortex

- ◆ For BCs, we need constitutive relationships
- ◆ Cortex deforms by planar dilation and shear
  - ◆  $\kappa$  is viscosity for surface area dilation
  - ◆  $\eta$  is viscosity for shear shear
  - ◆ Units:  $[\text{dyne}\cdot\text{s}/\text{cm}^2]*[\text{cm}] = [\text{dyne}\cdot\text{s}/\text{cm}]$



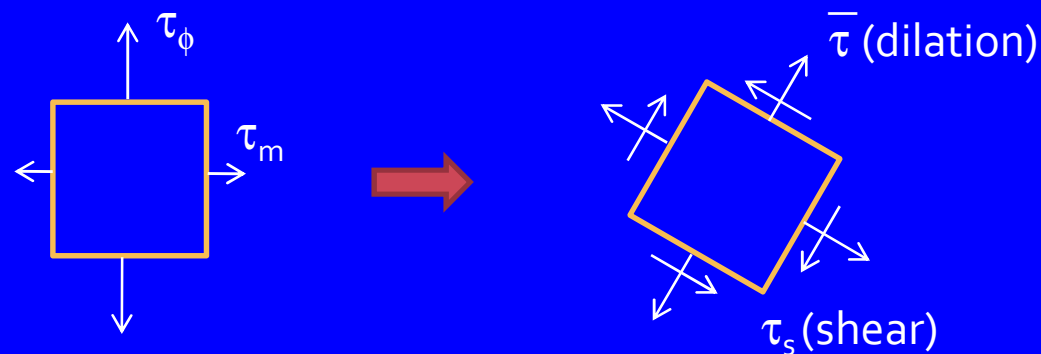
# Cortex

- ◆ First order model: stress resultants are proportional to rate of dilation and shear

$$\begin{aligned}\bar{\tau} &\equiv (\tau_m + \tau_\phi)/2 = \bar{\tau}_0 + \kappa \cdot V_\alpha \\ \tau_s &\equiv (\tau_m - \tau_\phi)/2 = 2\eta \cdot V_s\end{aligned}\quad (6)$$

where  $\bar{\tau}_0$  is static in-plane tension corresponding to zero rate of shearing and dilation

- ◆ Rotation of c.s. for principal shear stresses



# Cortex

- ◆ Kinematics of flow in the shell (curved surface)

$$\begin{aligned}V_{\alpha} &= \frac{dv_s}{ds} + \frac{v_s}{r} \cdot \cos \theta + v_n \left( \frac{d\theta}{ds} + \frac{\sin \theta}{r} \right) \\2V_s &= \frac{dv_s}{ds} - \frac{v_s}{r} \cdot \cos \theta + v_n \left( \frac{d\theta}{ds} - \frac{\sin \theta}{r} \right).\end{aligned}\quad (7)$$

where  $v_s, v_n$  are velocity fields derived from normal and tangential projections of fluid core velocities at the interface

$$\begin{aligned}v_n &= \sum_k n_k \cdot v_k \\v_s &= \sum_k t_k \cdot v_k.\end{aligned}\quad (8)$$

i.e., motion of cortical layer specified by liquid core's fluid velocities at the interface with a no-slip assumption

# Solution Approach

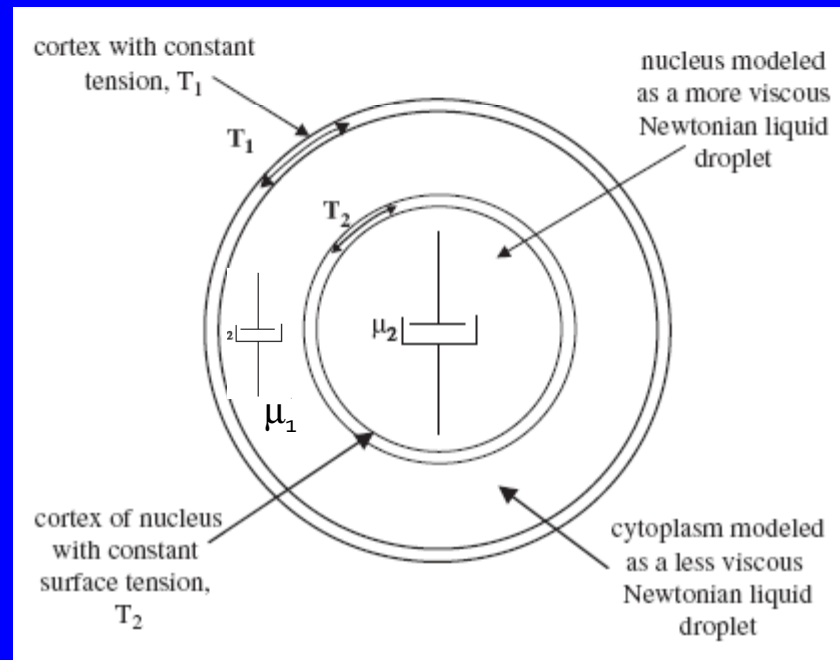
- ◆ Yeung and Evan use a general solution for axisymmetric creeping flow for exterior region

$$\begin{aligned}v_R(R, \theta) &= - \sum_{n=2}^{\infty} (A_n \cdot R^{n-2} + C_n \cdot R^n) P_{n-1}(\cos \theta) \\v_\theta(R, \theta) &= \sum_{n=2}^{\infty} (nA_n R^{n-2} + (n+2)C_n R^n) \frac{I_n(\cos \theta)}{\sin \theta} \\p(R, \theta) &= \Pi - \mu \sum_{n=2}^{\infty} \frac{2(2n+1)}{(n-1)} C_n R^{n-1} P_{n-1}(\cos \theta), \quad (9)\end{aligned}$$

- ◆ Course approximation used for inside the pipet

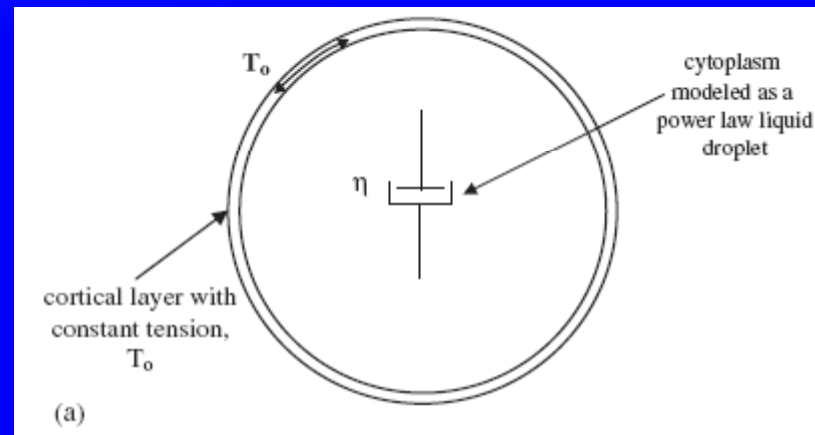
# Additional models

- ◆ Compound liquid drop model
  - ◆ Incorporates the higher viscosity and stiffness of the smaller nucleus



# Additional Models

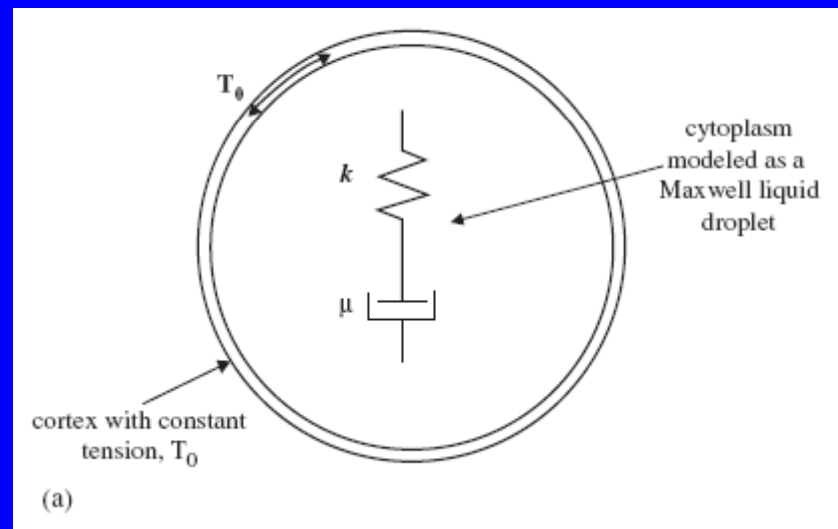
- ◆ Shear thinning liquid drop model
  - ◆ Approximates the apparent viscosity decrease with aspiration pressure



- ◆ Positive feedback: increase in shear rate leads to decreased viscosity, which in turn further increases shear rate...

# Additional Models

- ◆ Maxwell Liquid Drop
  - ◆ Large deformations satisfied by Newton liquid drop model but not for small deformations



- ◆ Accounts for initial elastic-like entry during aspiration